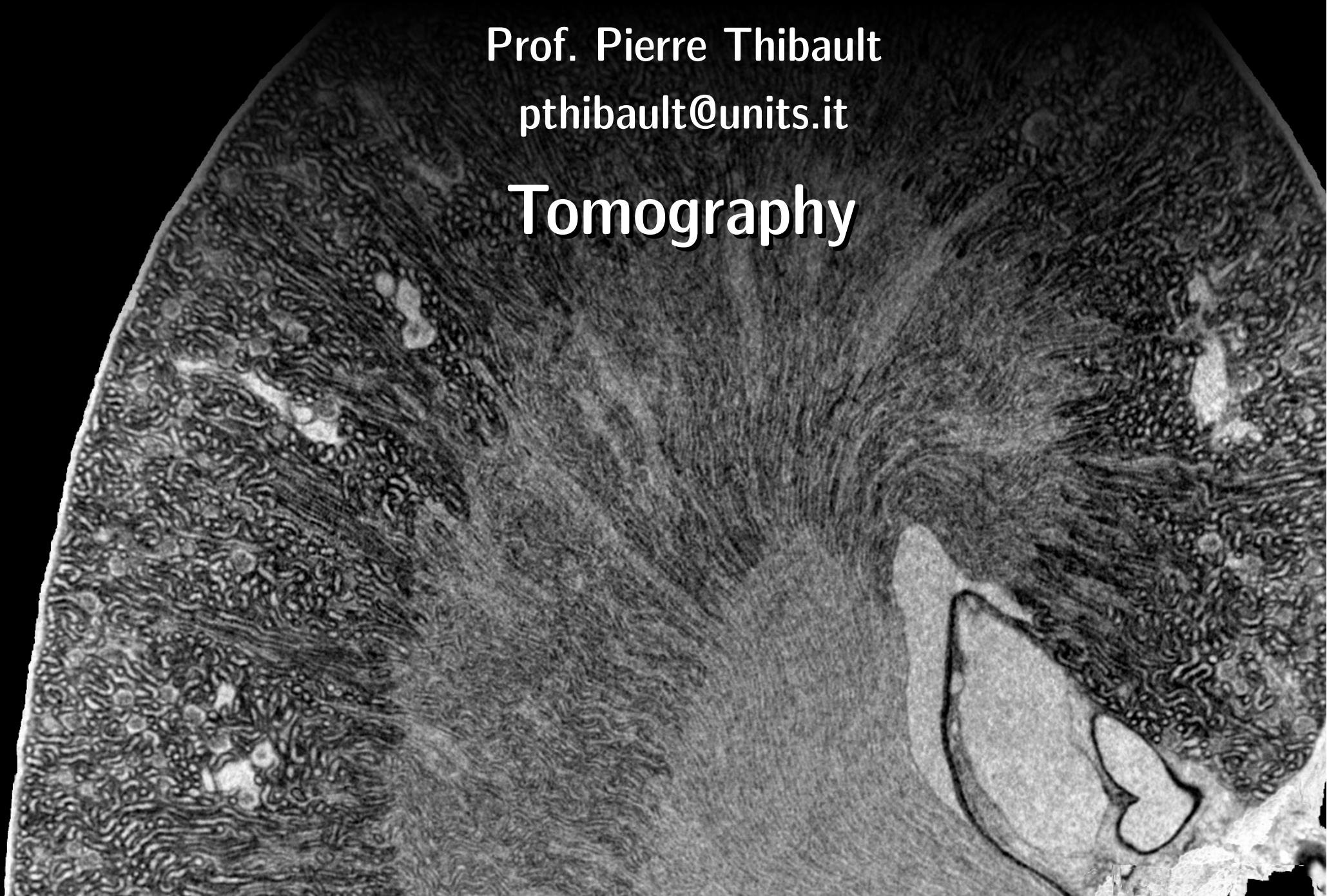


Image Processing for Physicists

Prof. Pierre Thibault

pthibault@units.it

Tomography

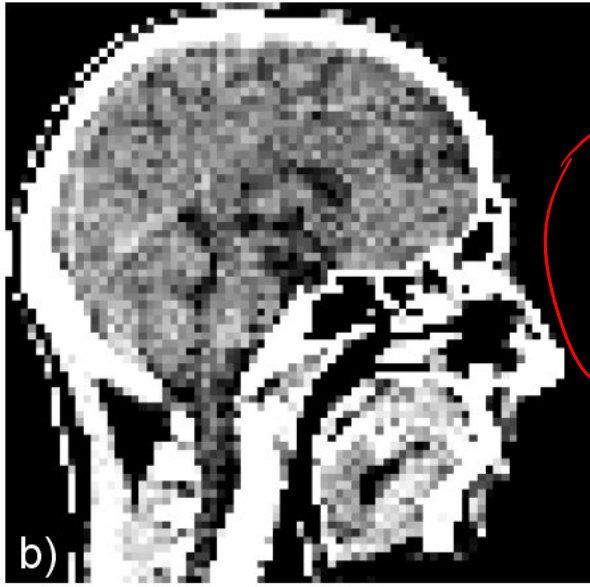
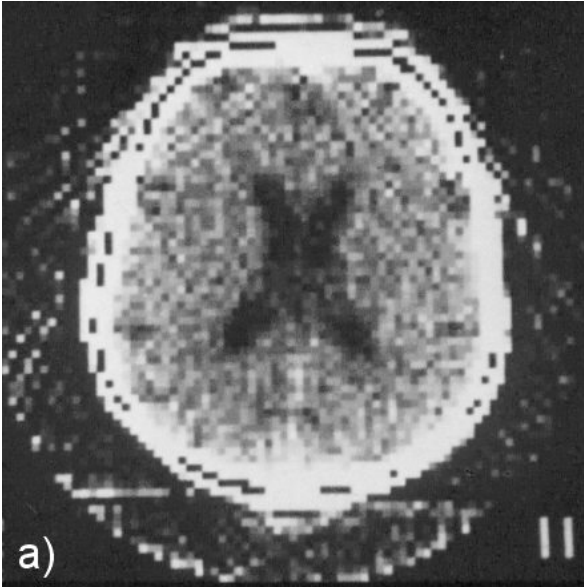
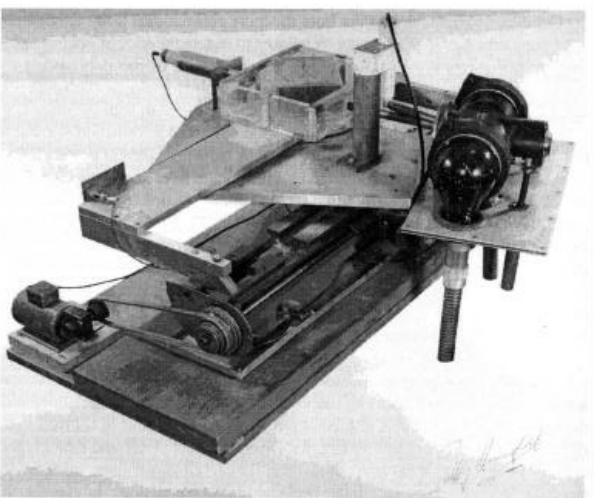


Overview

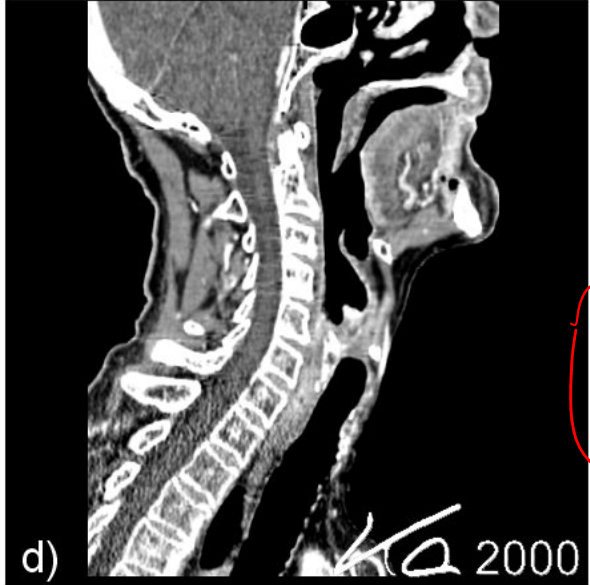
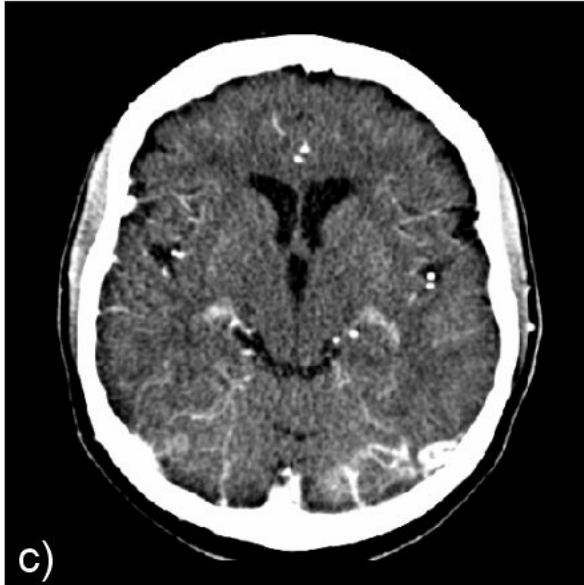
- Fundamentals of tomography
 - Physics & geometry
- Analytic formulation
 - Radon transform
 - Filtered back-projection
- Algebraic formulation

Examples of tomographic imaging

Computed (X-ray) Tomography (CT)



1974, 80x80 pixels

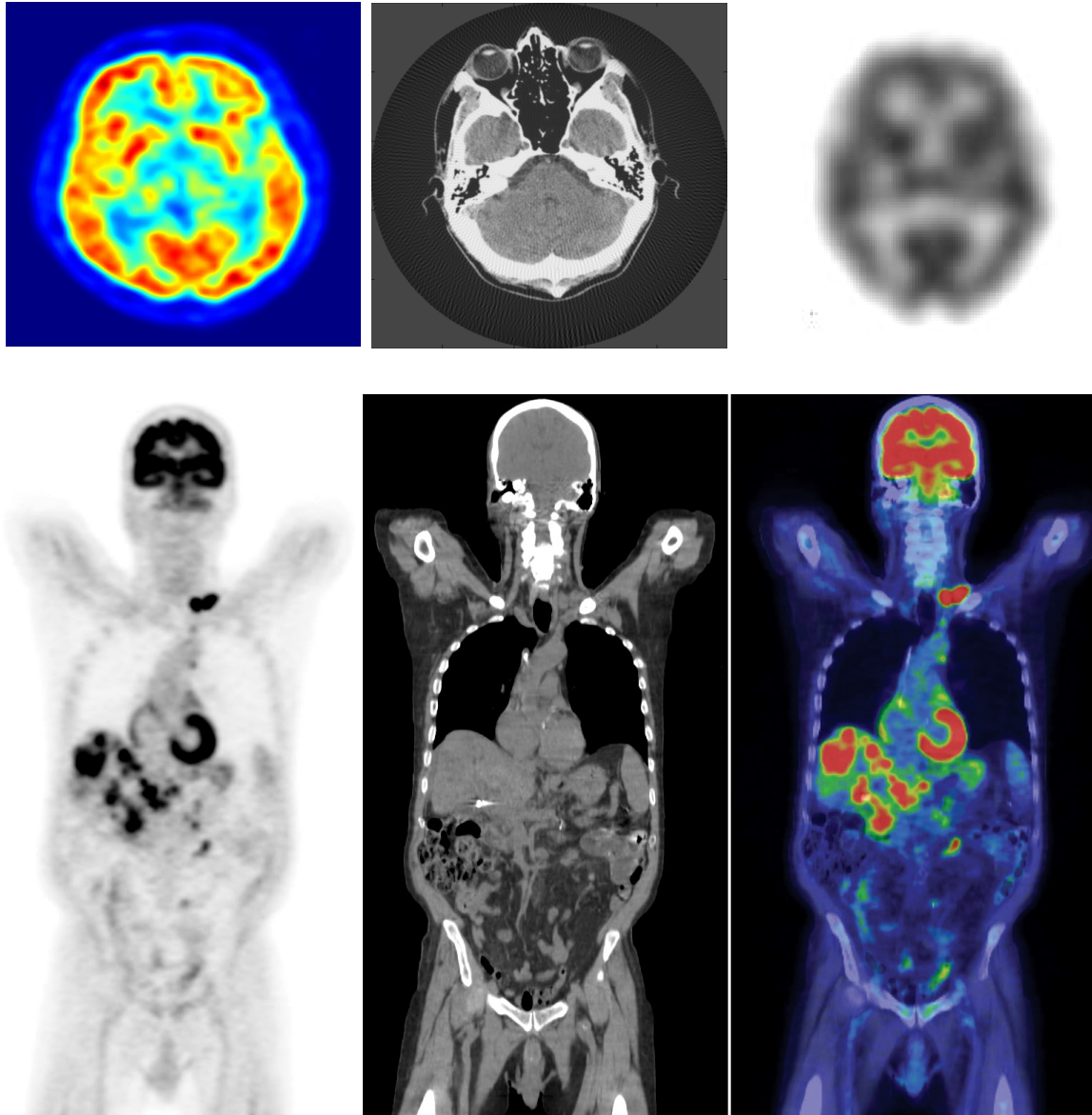


2000, 512x512 pixels, spiral CT

source: W. Kalender, Publicis, 3rd ed. 2011

Examples of tomographic imaging

Positron emission tomography (PET) + CT

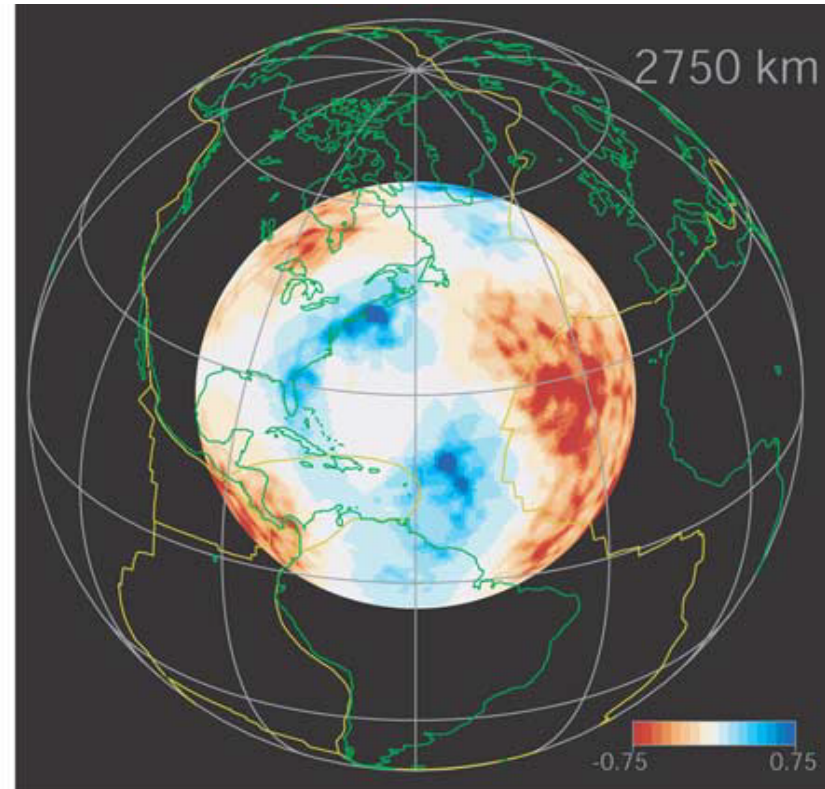
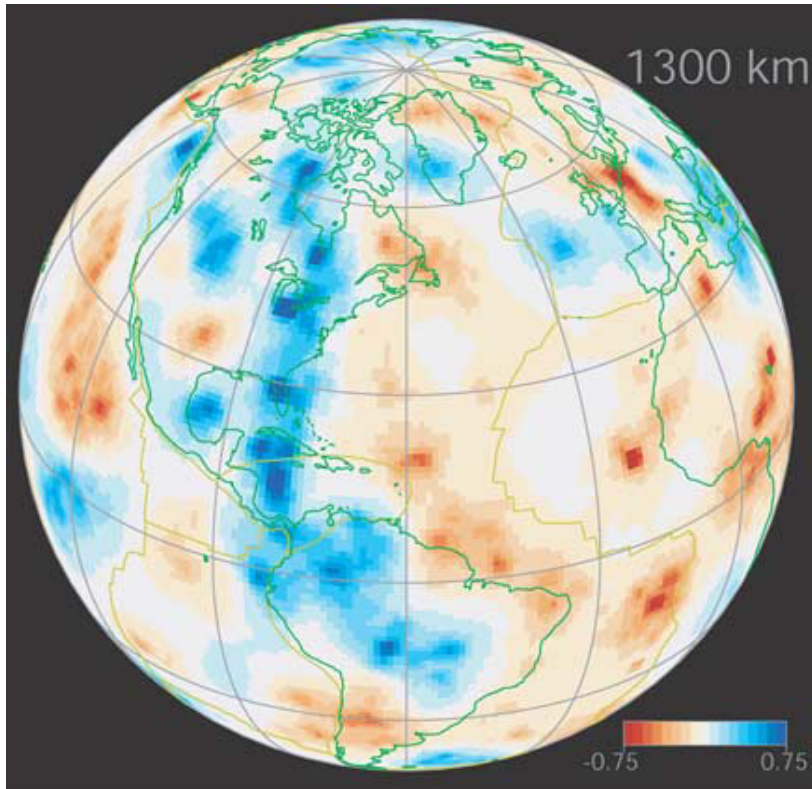


Single-Photon Emission
Computed Tomography (SPECT)



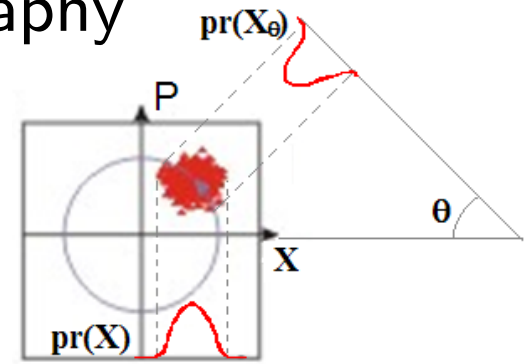
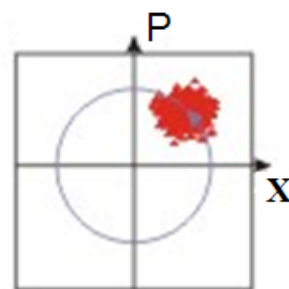
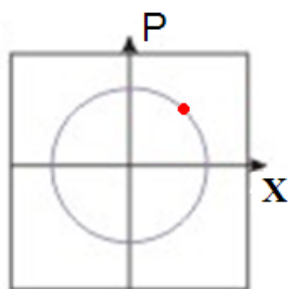
Examples of tomographic imaging

Seismic tomography



source: Sambridge et al. G3 Vol.4 Nr.3 (2003)

Quantum state tomography

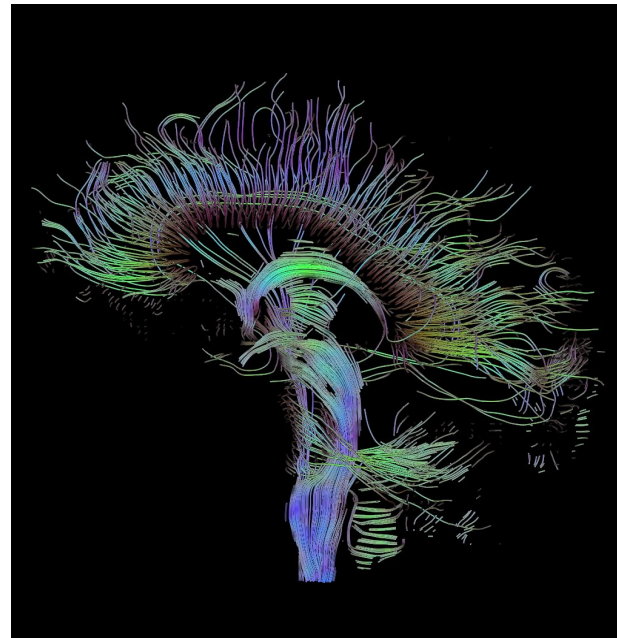
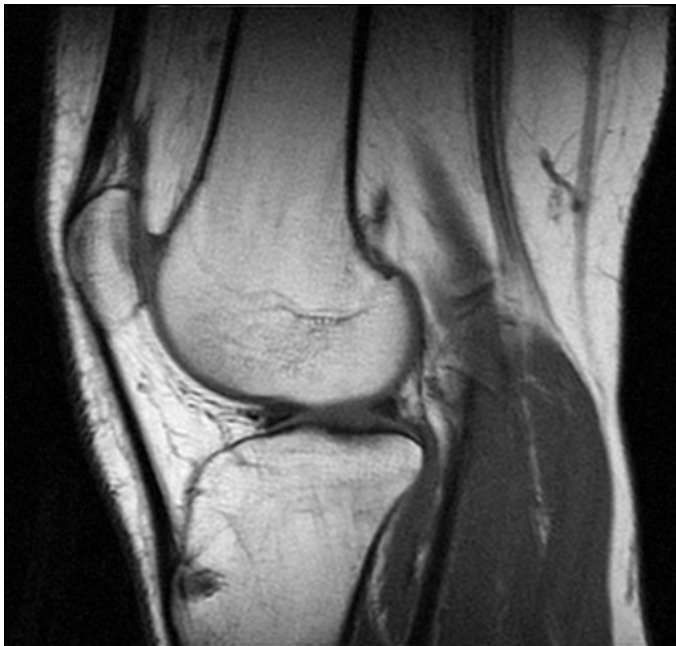


Examples of tomographic imaging

Ultrasonography/tomography (US/UST)

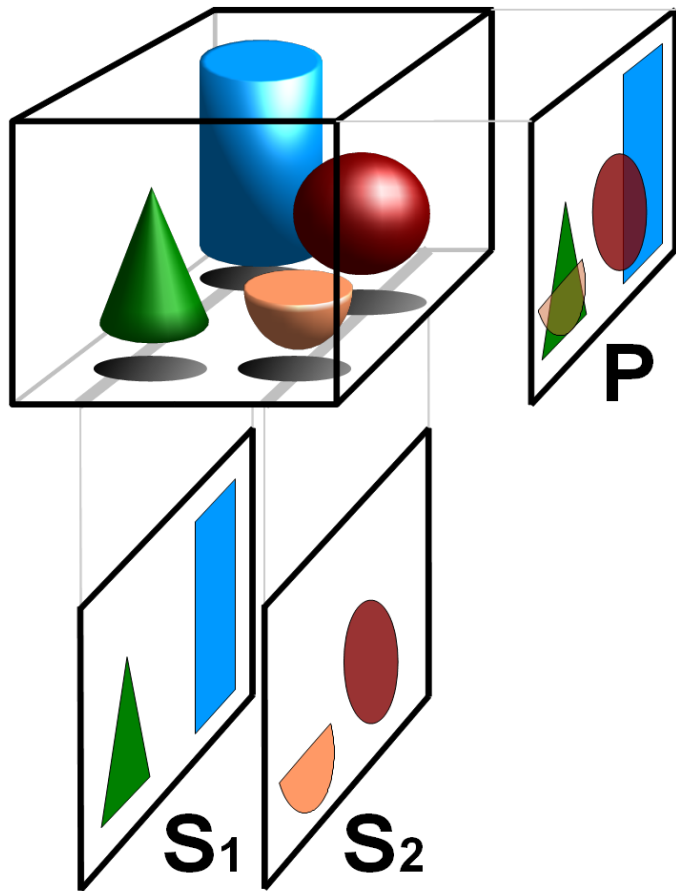


Magnetic resonance imaging/tomography (MRI/MRT)

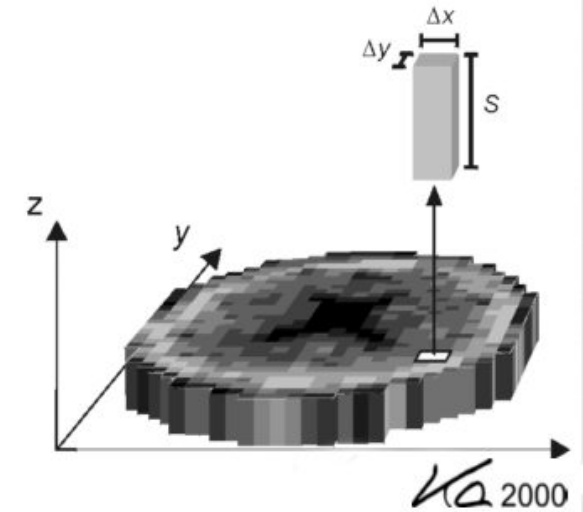
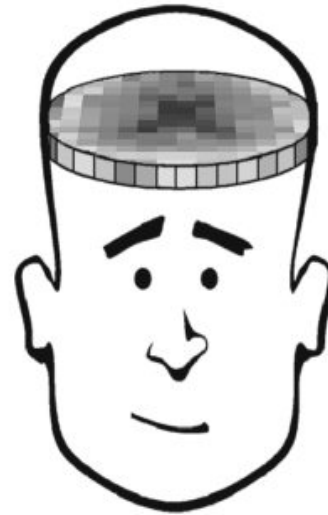


Reconstructions from projections

Reconstruction of volume
from projections

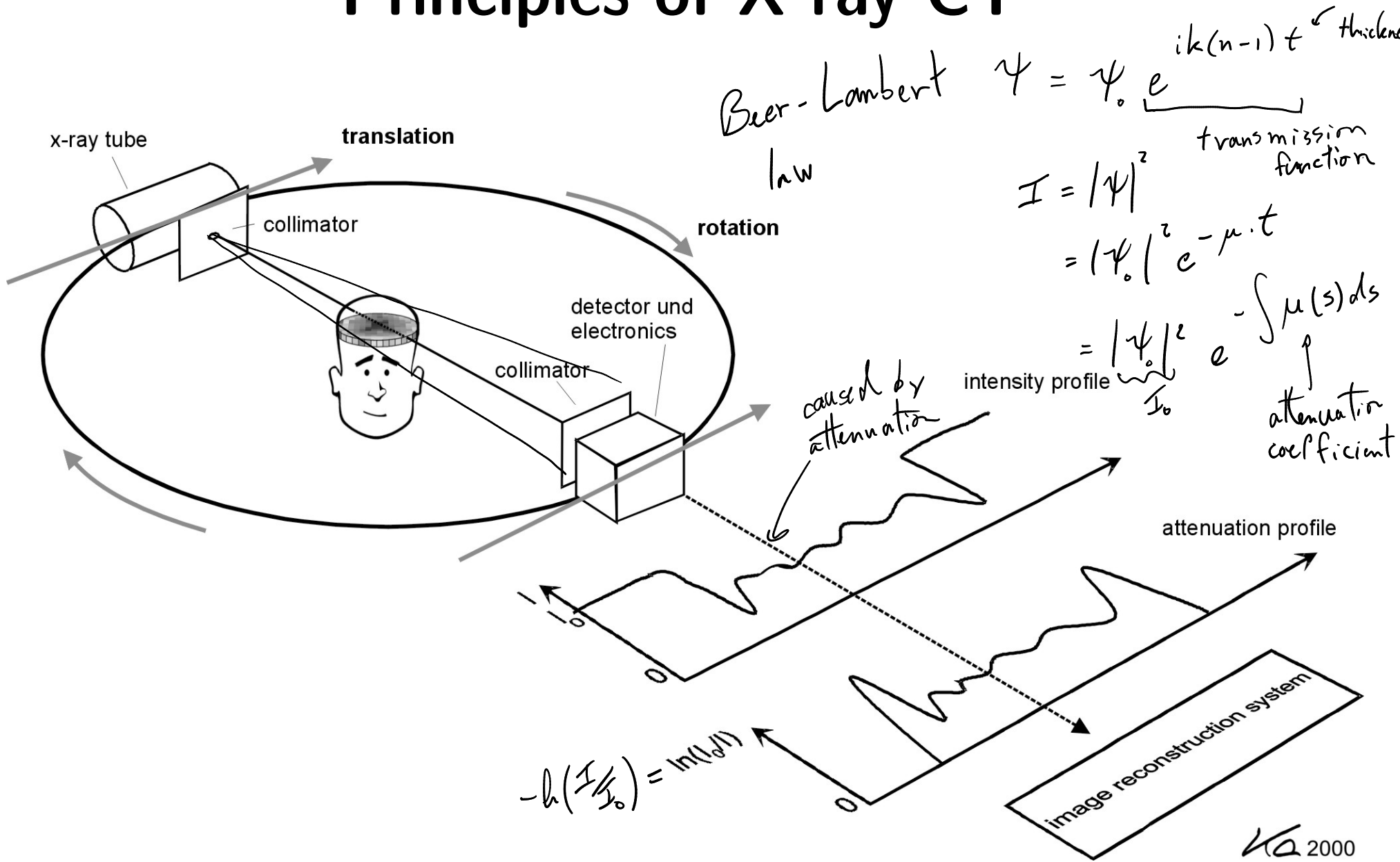


Digitization into voxels



source: W. Kalender, Publicis, 3rd ed. 2011

Principles of X-ray CT



source: W. Kalender, Publicis, 3rd ed. 2011

Radon transform

Rotated coordinate system

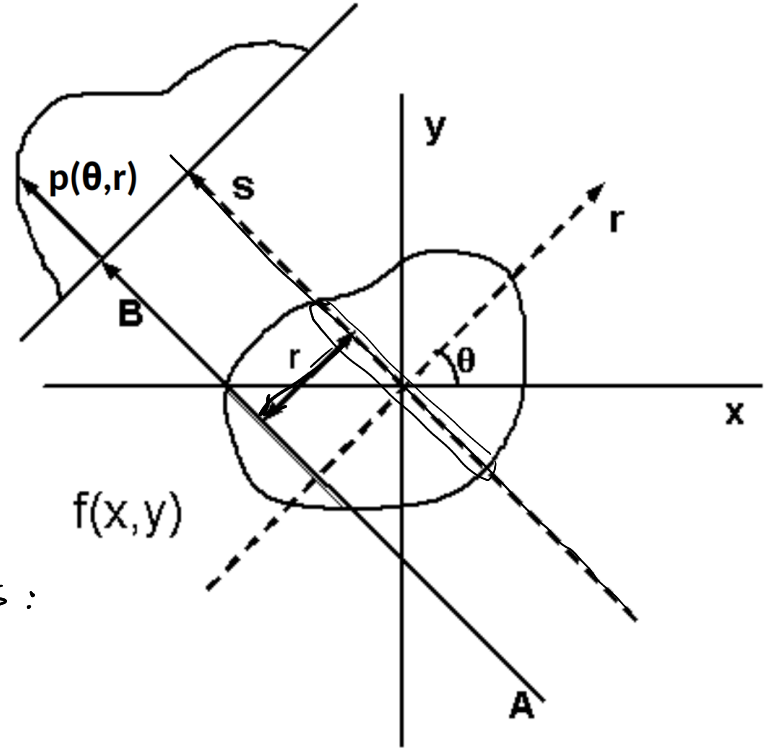
Radon transform

$$p(r, \theta) = \iint f(x, y) \delta(r - (x \cos \theta + y \sin \theta)) dx dy$$

r not as in polar coordinates:
can be negative

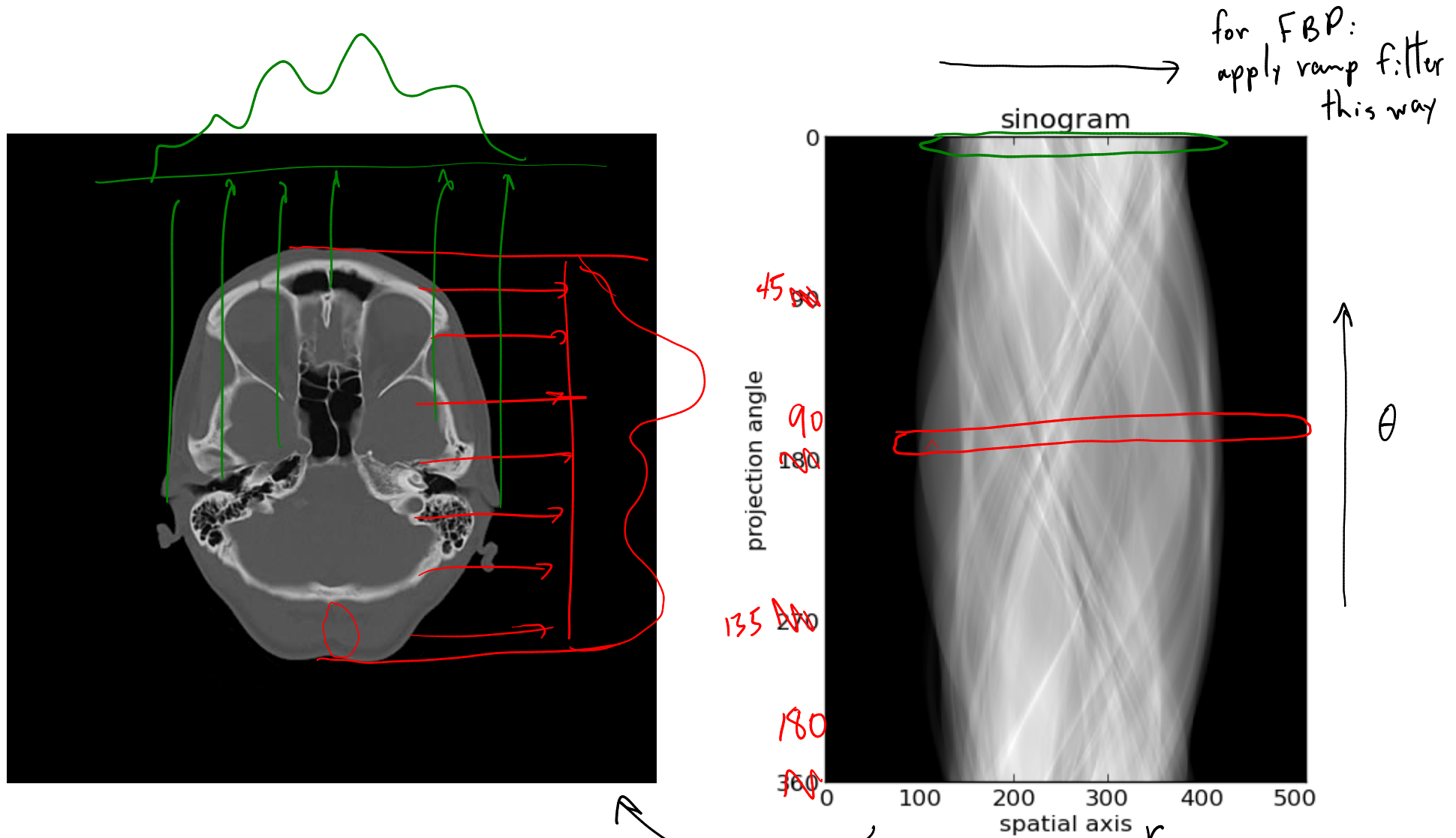
$$f(x, y) = \dots (p(r, \theta))$$

inverse Radon transform



Sinogram

Representation of projection measured by a single detector line as a function of angle



The Fourier slice theorem

"DC term"

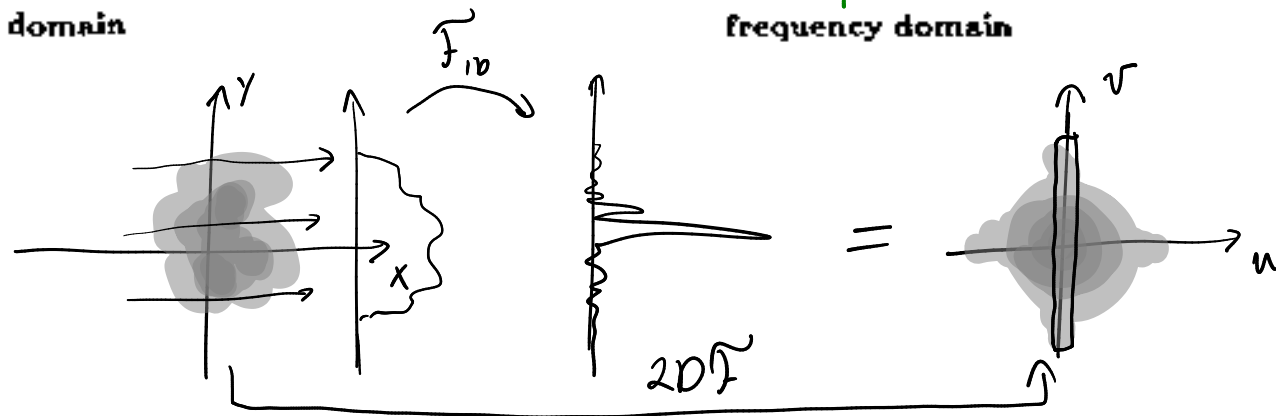
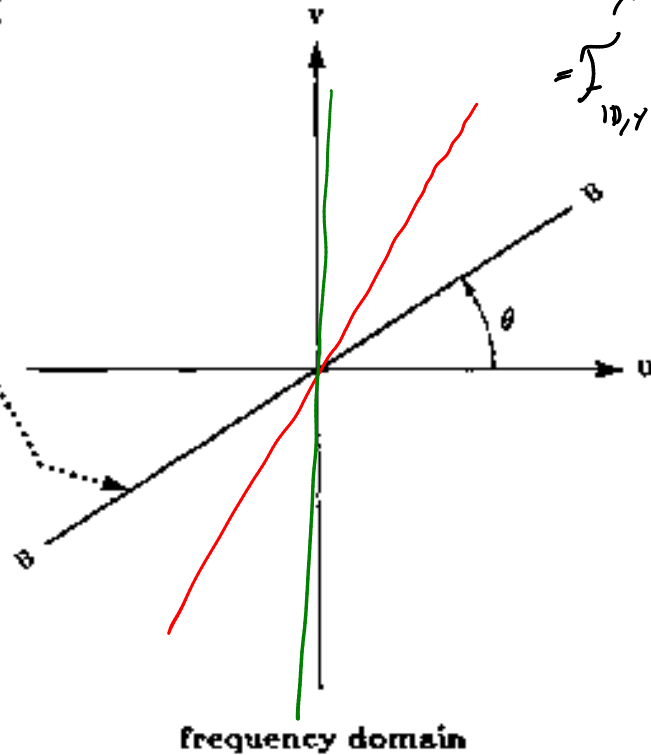
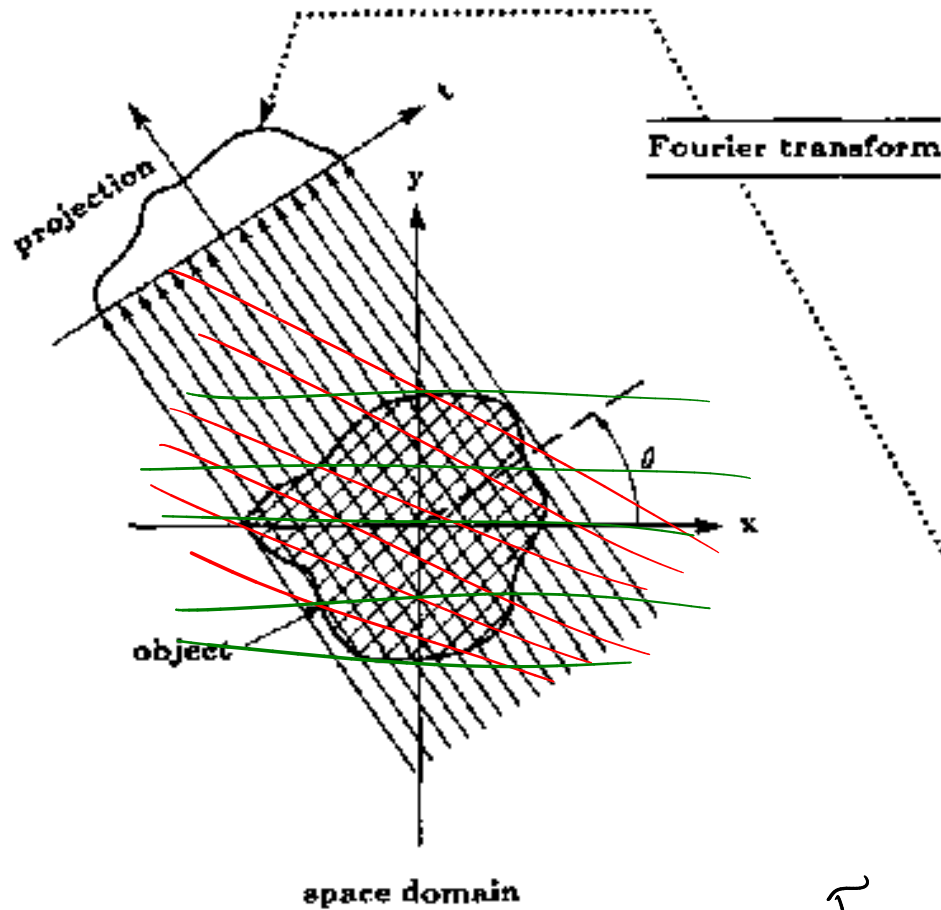
$$F(u=0) = \int f(x) dx$$

$$F(u=0, v) = \int_{2D} \{f\}(u=0, v) = \int f(x, y) e^{-iv y} dx dy$$

$$= F_{1D, y} \{ F_{1D, x} \{ f \} \}$$

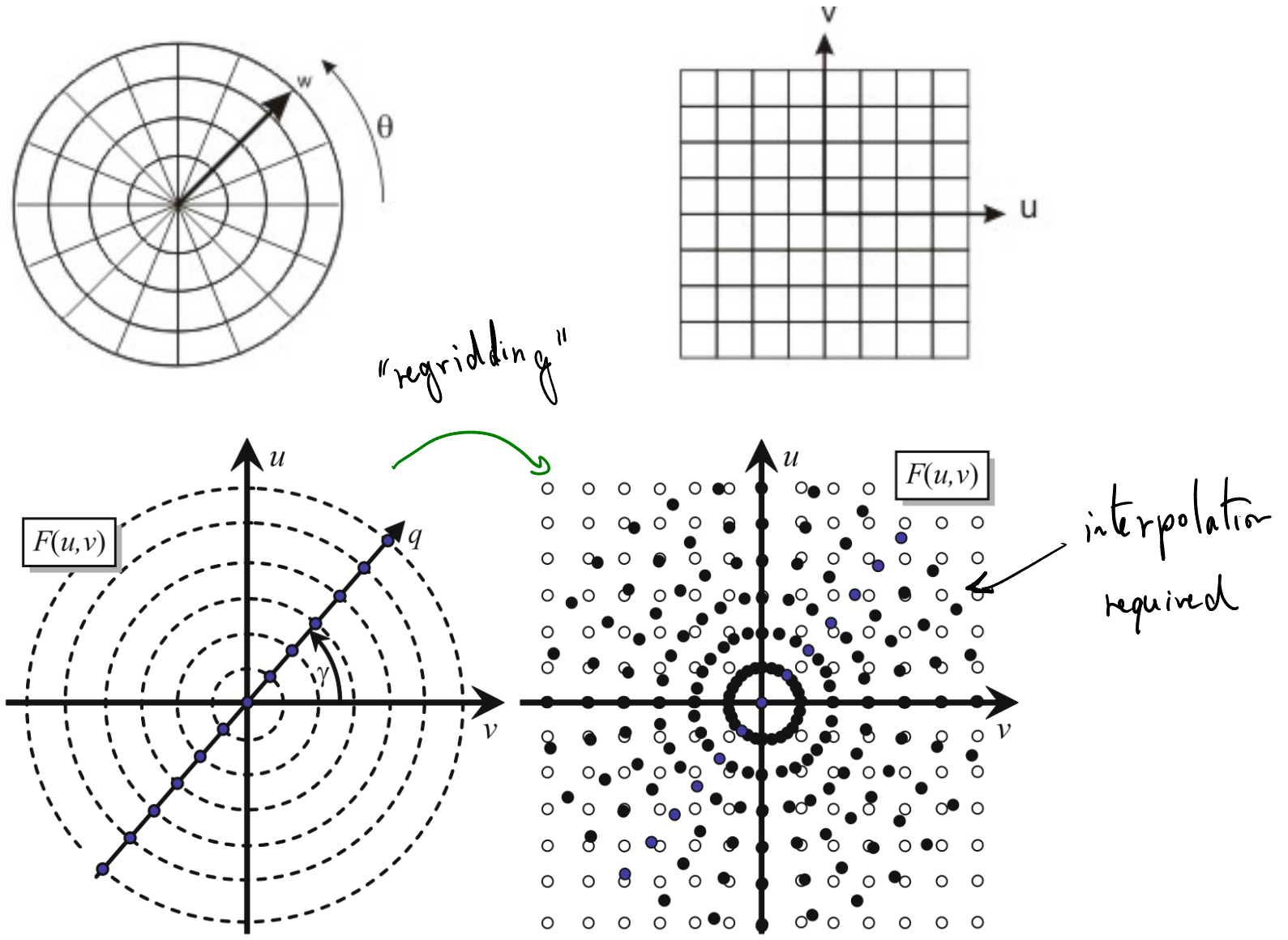
$$= \int_{1D, y} \left\{ \int f(x, y) dx \right\}$$

projection
along x



Frequency space sampling

Change of sampling grid from polar to rectangular requires interpolation



a

b

Filtered back-projection

$$f(x,y) = \mathcal{F}^{-1} \{ F(u,v) \}$$

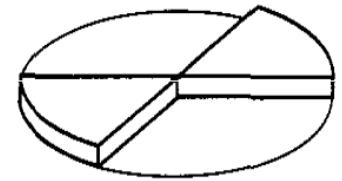
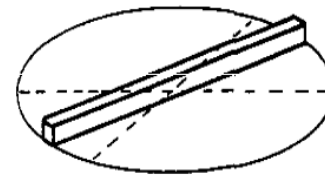
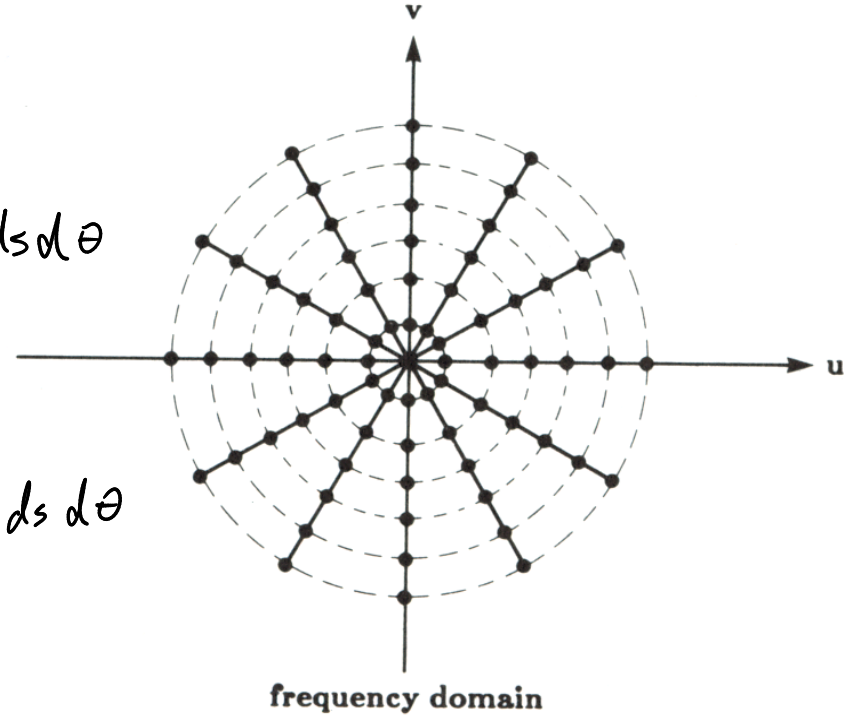
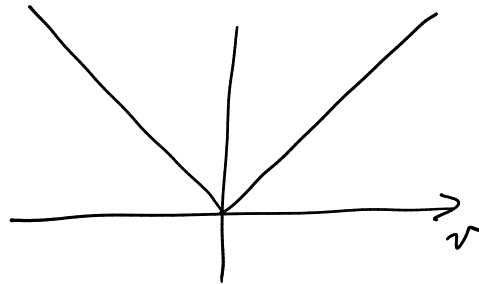
$$= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} F(u,v) e^{2\pi i(ux+vy)} du dv$$

Polar coordinates: $u = s \cos \theta$ $du dv = s ds d\theta$
 $v = s \sin \theta$

$$f(x,y) = \int_0^{\pi} \int_0^{\infty} F(s \cos \theta, s \sin \theta) e^{2\pi i s(x \cos \theta + y \sin \theta)} s ds d\theta$$

e.g. $\theta = 90^\circ$: $\int F(u=0, v) e^{2\pi i v y} v dv$

ramp filter



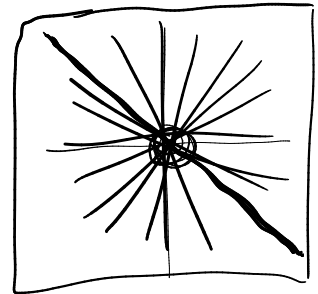
Filtered back-projection

Radon transform $\rightarrow \mathcal{F}$ along r

$$\mathcal{F}_r \{p(r, \theta)\} = F(w \cos \theta, w \sin \theta)$$

\uparrow $F(u, v) = 2d$ F.T. of $f(x, y)$
 filtered

$$FBP = \int d\theta \underbrace{\tilde{p}(x \cos \theta + y \sin \theta, \theta)}$$



$$\tilde{p}(r, \theta) = \int_{-\infty}^{\infty} F(w \cos \theta, w \sin \theta) e^{2\pi i r w} w dw$$

Filter

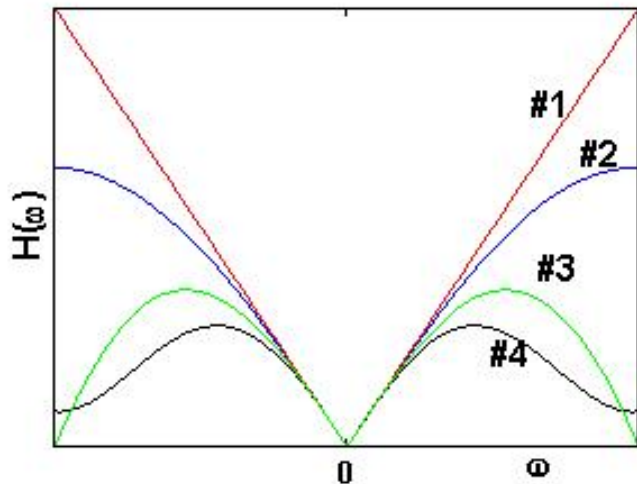
$$\tilde{p}(x \cos \theta + y \sin \theta, \theta) = \int_{-\infty}^{\infty} F(w \cos \theta, w \sin \theta) e^{2\pi i (x \cos \theta + y \sin \theta) w} w dw$$

$$\int d\theta \tilde{p}(x \cos \theta + y \sin \theta, \theta) = \iint F(w \cos \theta, w \sin \theta) e^{2\pi i (x w \cos \theta + y w \sin \theta)} w dw d\theta$$

\mathcal{F}^{-1} in polar coordinates
 $= f(x, y)$

Filtered back-projection

- Filter can be tuned to achieve image enhancement
- Trade-off between noise and sharpness

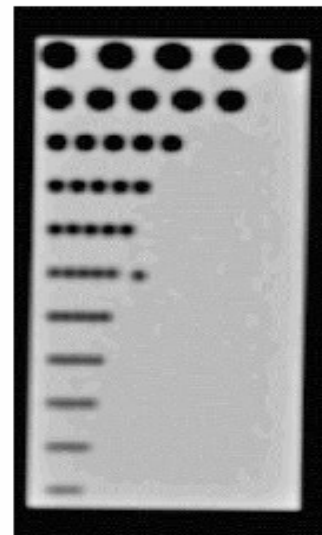
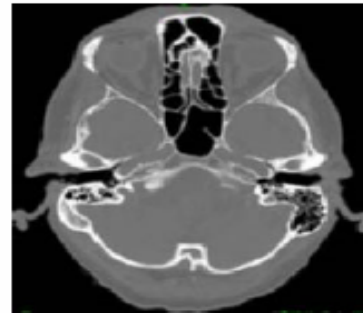


#1 ram-lak (ramp)

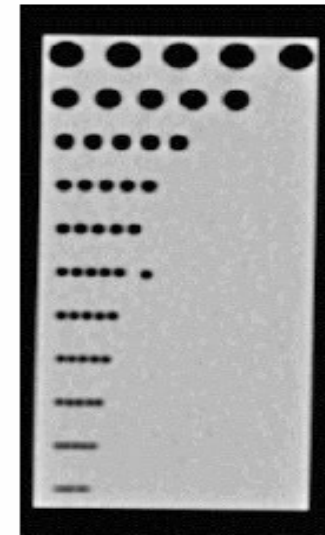
#2 Shepp-Logan

#3 cosine

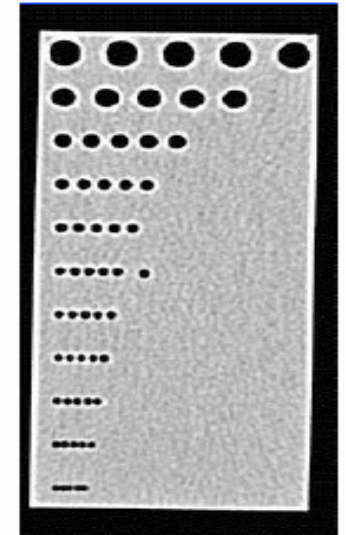
#4 Hamming



smoothing



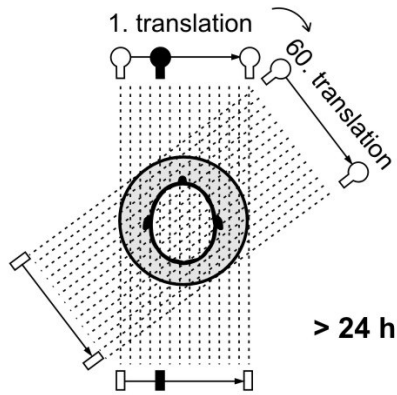
standard



edge enhanced

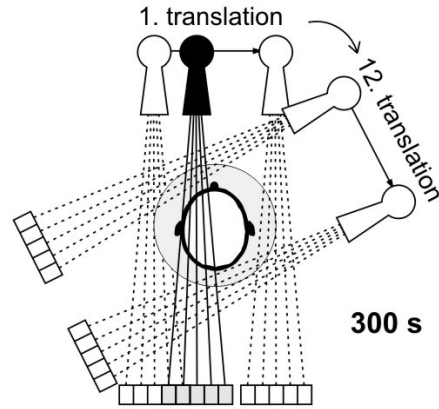
Geometries

pencil beam (1970)

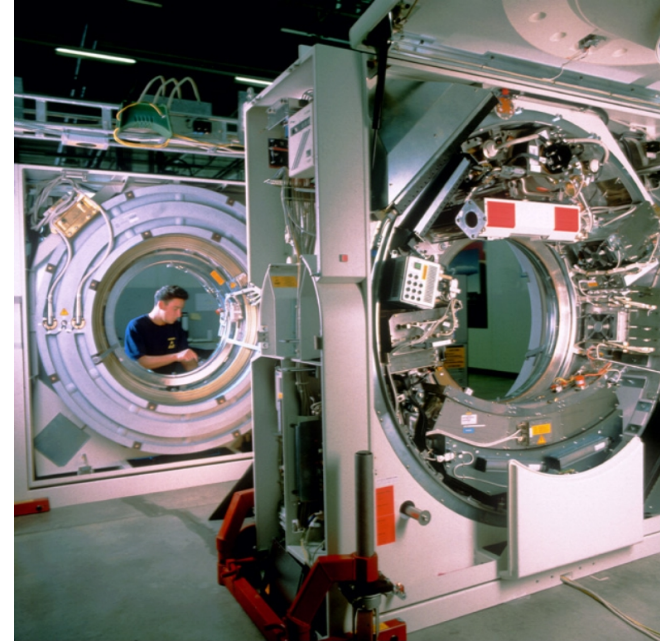


1st generation: translation / rotation

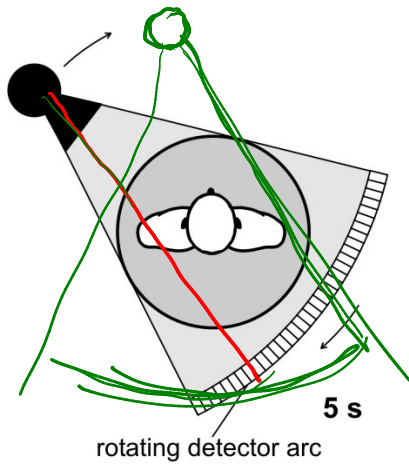
partial fan beam (1972)



2nd generation: translation / rotation

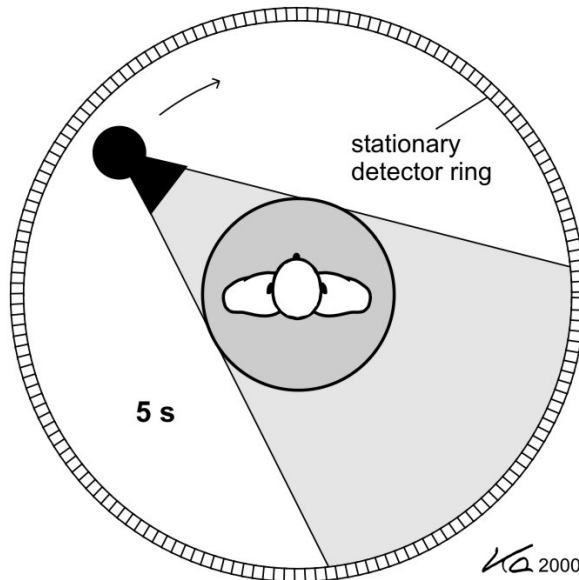


fan beam (1976)

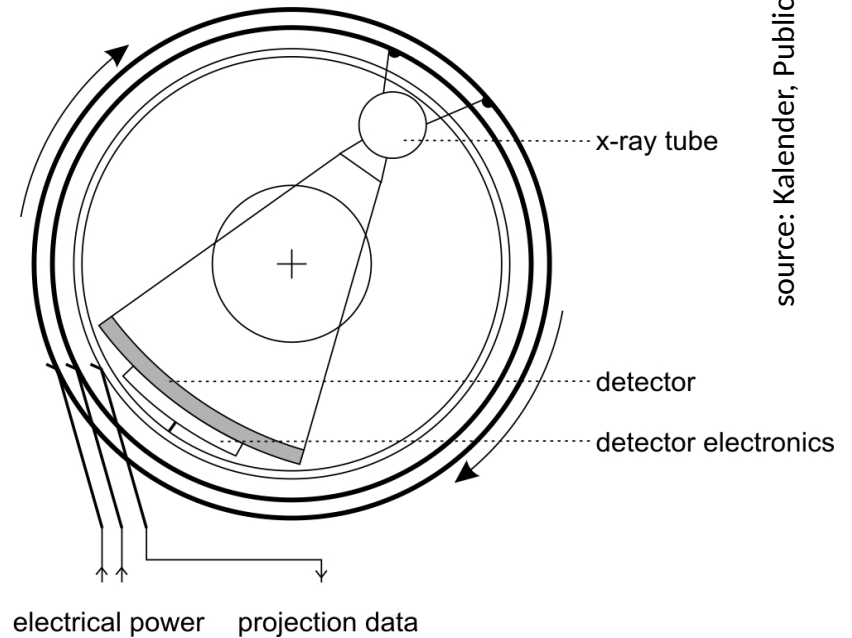


3rd generation: continuous rotation

fan beam (1978)



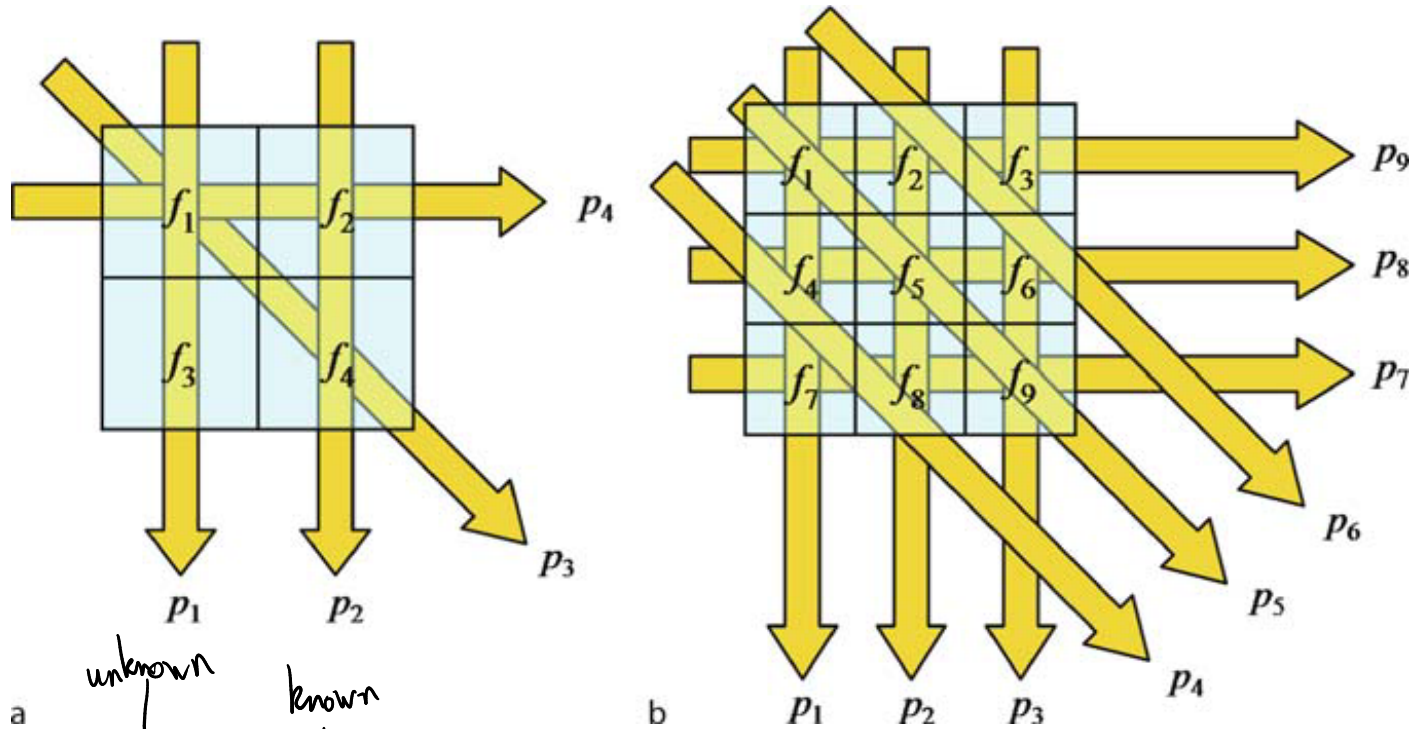
4th generation: continuous rotation



source: Kalender, Publicis, 3rd ed. 2011

Algebraic formulation

Tomography can be formulated as a set of linear equations



unknown
↓
known
↓

$$f_1 + f_2 = p_4$$
$$f_1 + f_3 = p_1$$

⋮

source: Buzug, Springer, 1st ed. 2008

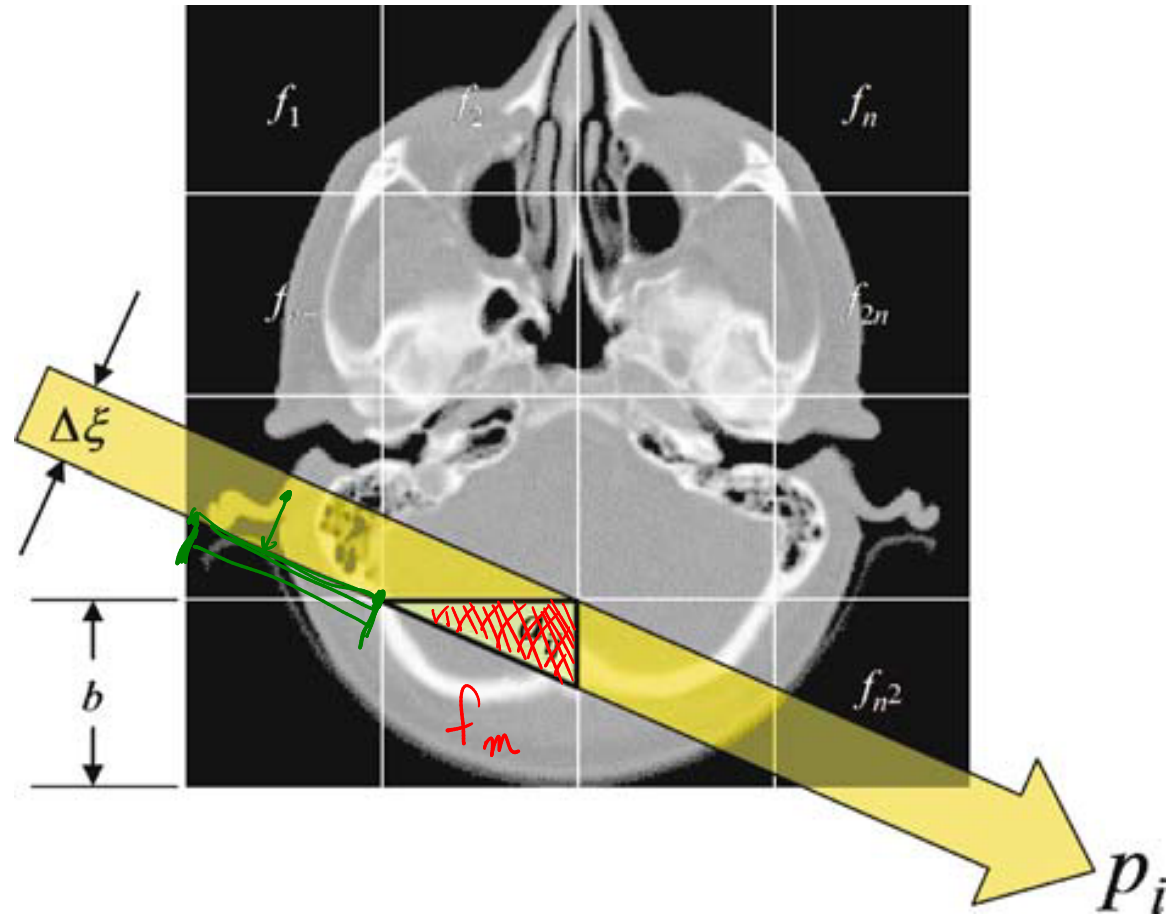
Weighting coefficients

Weighting measures:

- Logic
- Area
- Path length
- Distance to pixel center

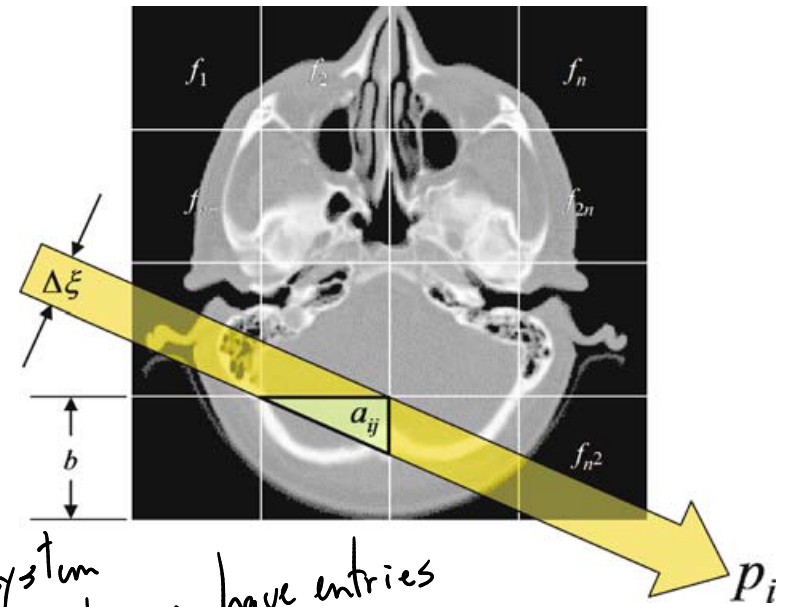
$$p_i = \dots + \alpha_i f_m$$

weight

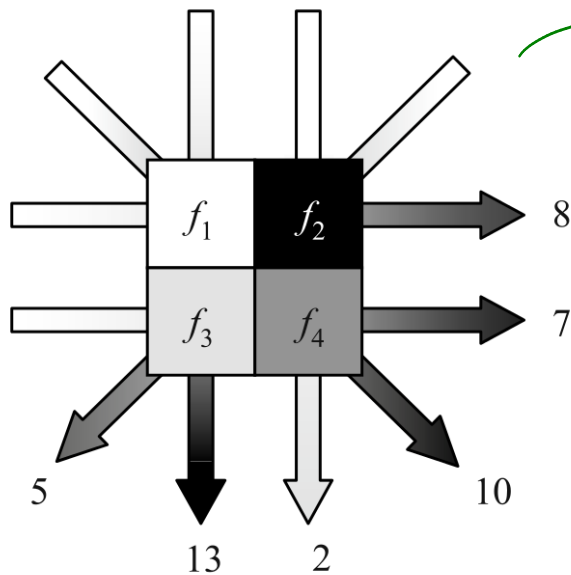


Differences in calculation effort, smoothness, noise sensitivity, ...

System Matrix



real system matrices have entries between 0 and 1

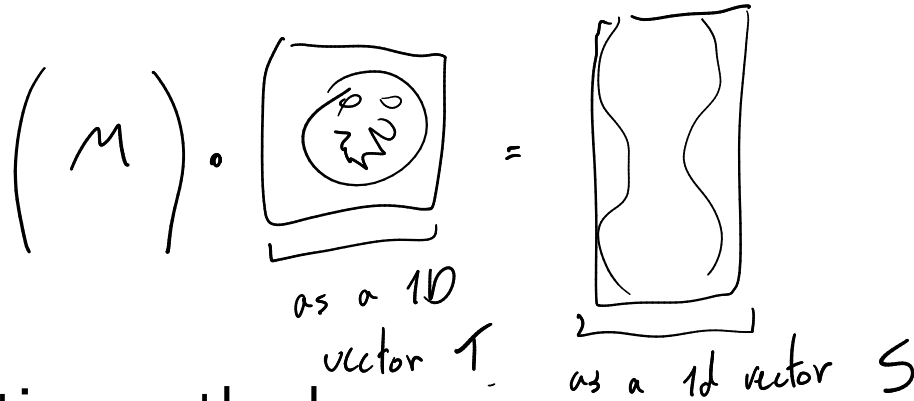


$$\begin{pmatrix} 0 & 1 & 1 & 0 \\ 1 & 0 & 1 & 0 \\ 0 & 1 & 0 & 1 \\ 1 & 0 & 0 & 1 \\ 0 & 0 & 1 & 1 \\ 1 & 1 & 0 & 0 \end{pmatrix} \begin{pmatrix} f_1 \\ f_2 \\ f_3 \\ f_4 \end{pmatrix} = \begin{pmatrix} 5 \\ 13 \\ 2 \\ 10 \\ 7 \\ 8 \end{pmatrix}$$

source: Buzug, Springer, 1st ed. 2008

Matrix (pseudo)-inversion

Tomographic reconstruction = linear system inversion



$$M^{-1} = (M^T M)^{-1} M^T$$

pseudo inverse
"best" solution in
the least square
sense

$$M \cdot T = S$$

$$T \sim 1000 \times 1000 = 10^6$$

$$S \sim 1060 \times 1000 = 10^6$$

$$M : 1000000 \times 1000000 \text{ matrix}$$

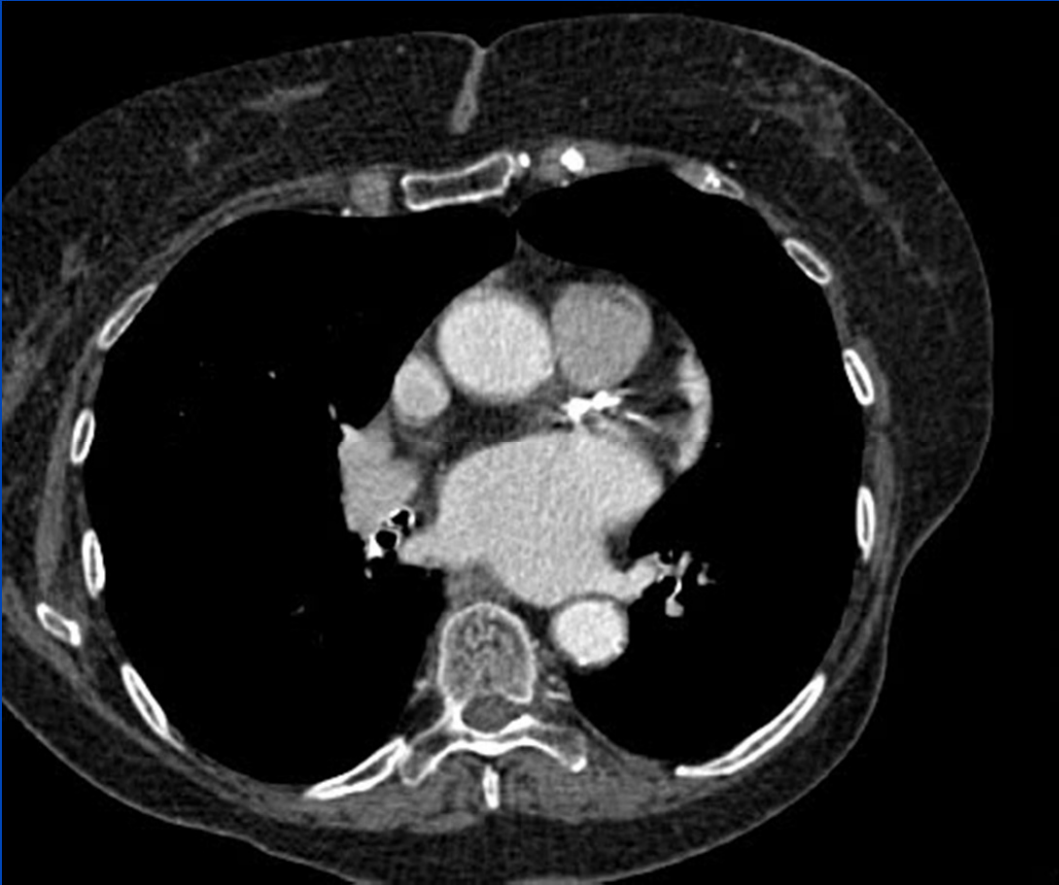
Iterative methods:

- ART Algebraic reconstruction technique
- SART Simultaneous algebraic reconstruction technique
- SIRT Simultaneous iterative reconstruction technique
- MART Multiplicative algebraic reconstruction technique
- MLEM Maximum likelihood expectation maximization
- OSEM Ordered subset expectation maximization
- ... and many, many more

FBP vs algebraic methods

FBP

Filtered backprojection 100% dose



ART (or SART)

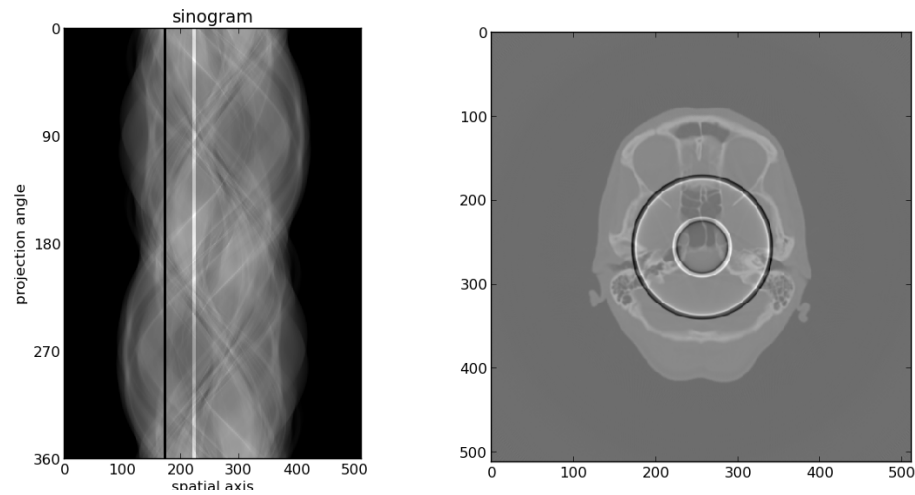
iterative 40% dose



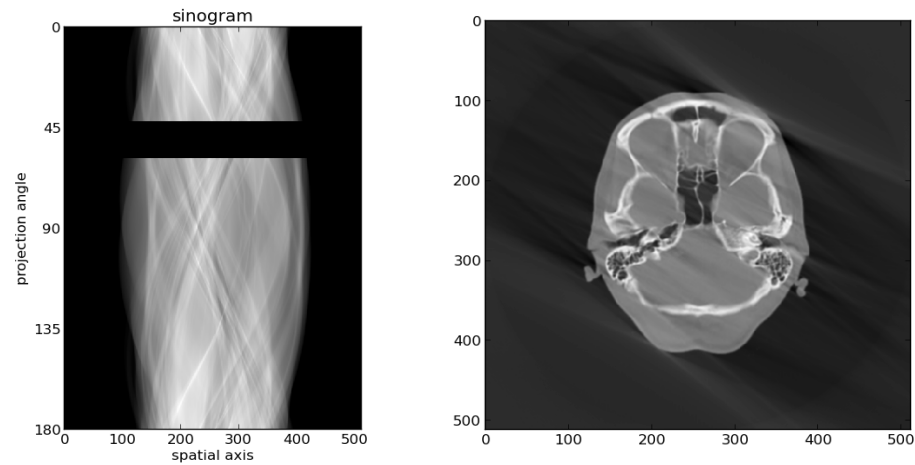
source: Kachelries, http://www.dkfz.de/en/medphysrad/workinggroups/ct/ct_conference_contributions/BasicsOfCTImageReconstruction_Part2.pdf

Artifacts

Detector imperfections → ring artifacts

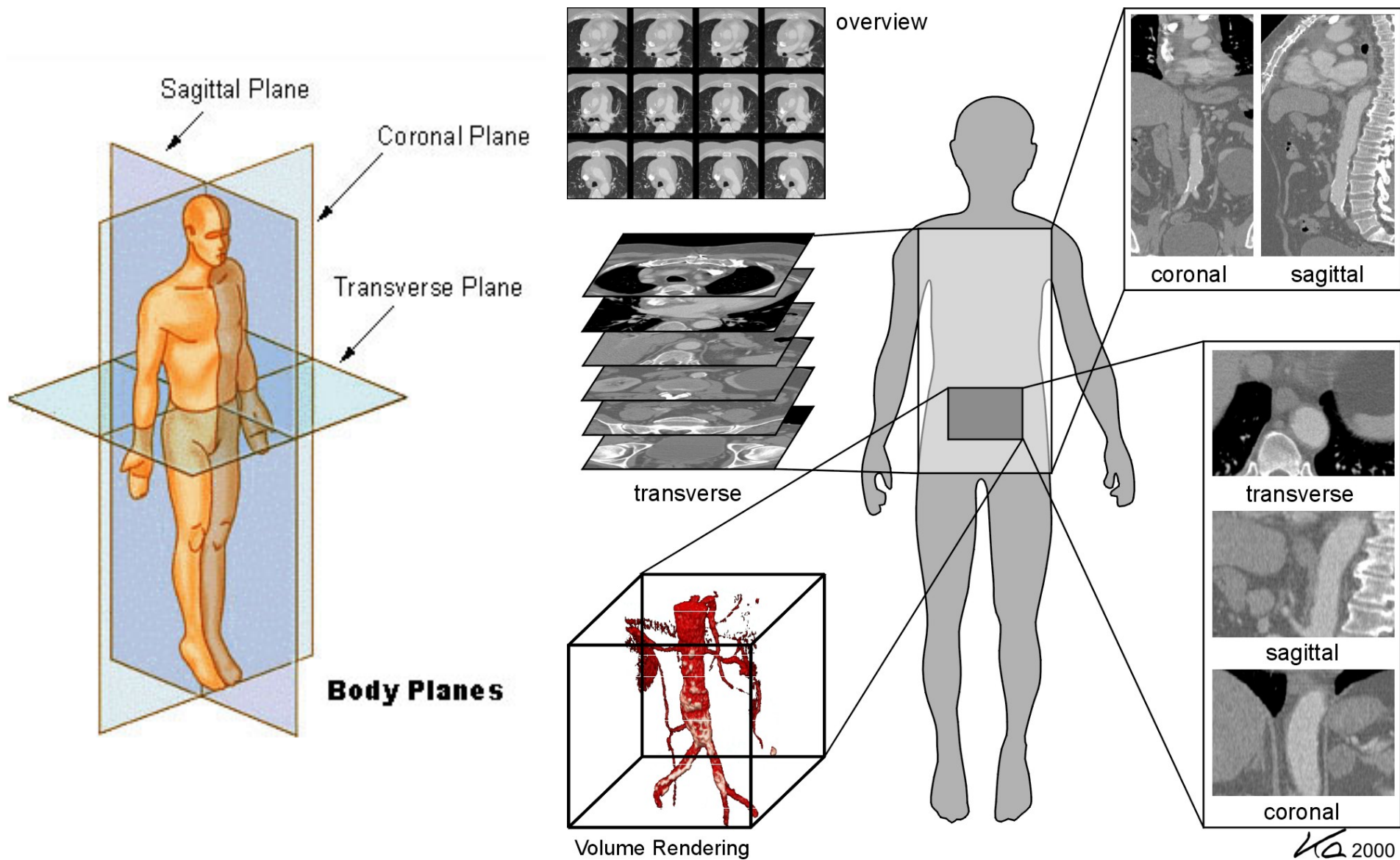


Missing projections → “streak” artifacts



Also: sample motion, beam hardening, ...

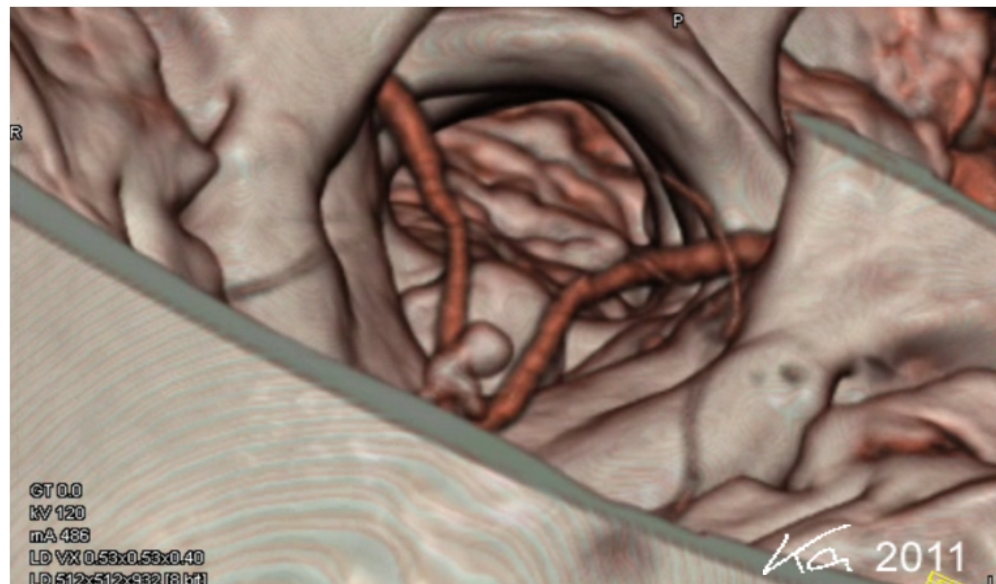
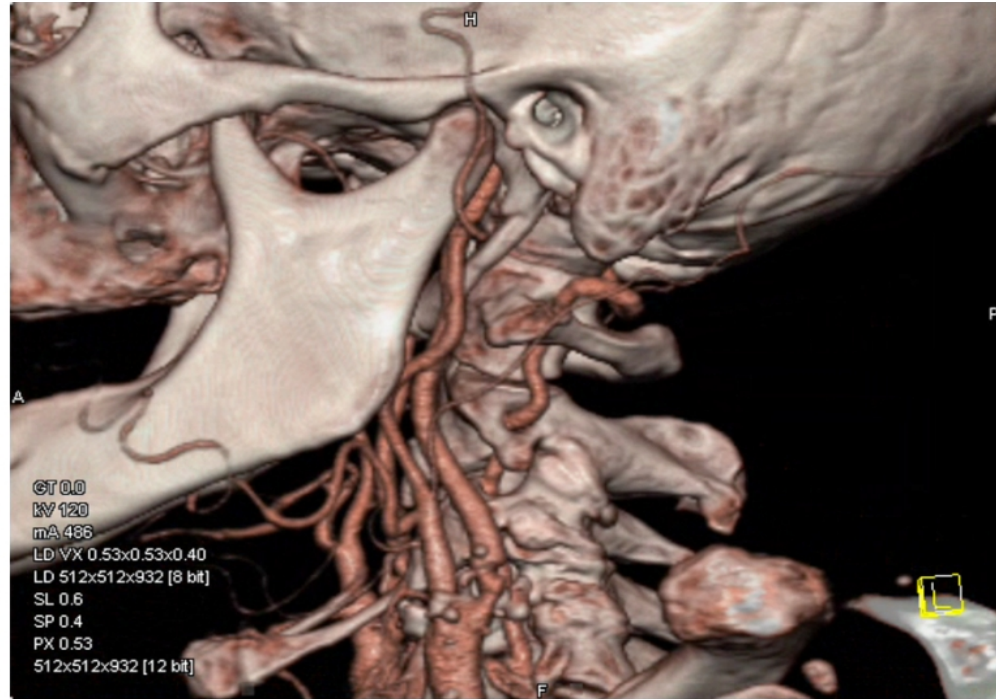
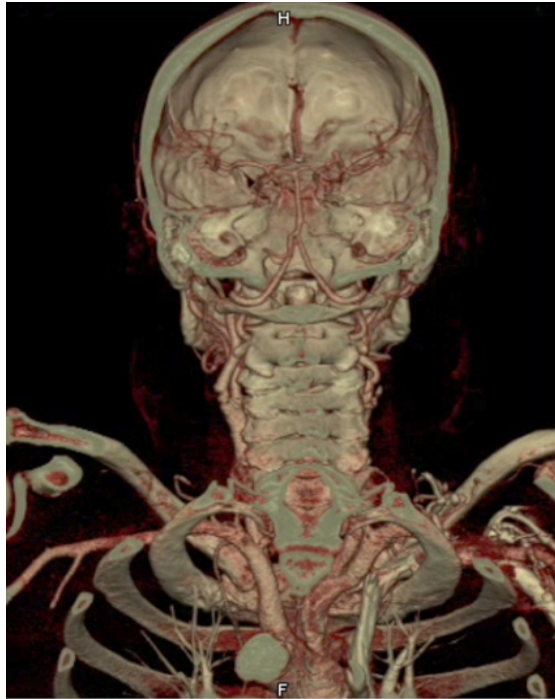
Tomographic Display



source: <http://wikipedia.org>

source: W. Kalender, Publicis, 3rd ed. 2011

Volume rendering display



Summary

- Computed tomography: reconstruction from projections
- Analytic approach:
 - Projections and tomographic slices are related by the Fourier slice theorem
 - Standard algorithm uses filtered back-projection
- Algebraic approach:
 - Tomography as a system of linear equations
 - Iterative methods are used for large matrix inversions
 - More powerful but computationally more costly
- Imperfect data leads to artifacts

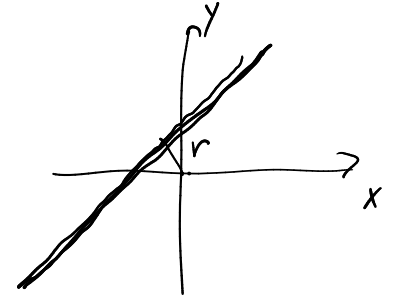
Raden transform (reminder)

w : reciprocal variable to r

$$\rho(r, \theta) = \iint f(x, y) \delta(r - (x \cos \theta + y \sin \theta)) dx dy$$

$$\mathcal{F}_r \{ \rho(r, \theta) \} = \int_{-\infty}^{\infty} \rho(r, \theta) e^{-2\pi i r w} dr$$

$$= \int_{-\infty}^{\infty} \iint f(x, y) \delta(r - (x \cos \theta + y \sin \theta)) e^{-2\pi i r w} dx dy dr$$



$$= \iint f(x, y) \exp(-2\pi i w (x \cos \theta + y \sin \theta)) dx dy$$

$$= \iint f(x, y) \exp\left[-2\pi i \left(x \cdot \underbrace{w \cos \theta}_u + y \cdot \underbrace{w \sin \theta}_v \right)\right] dx dy$$

$$= F(u = w \cos \theta, v = w \sin \theta)$$

