

MEDICAL PHYSICS LAB

LECTURE 1 - INTRODUCTION

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About me (contact information)

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About me (as a Researcher)

- Phase-contrast X-ray imaging
 - Mammography and Breast Computed Tomography
- X-ray imaging with Synchrotron Radiation (Elettra)
- Detectors for X-ray imaging
 - Single-photon-counting
 - Silicon microstrip detectors
- Collaborating with other lecturers
 - R. Longo, F. Arfelli
- Conferenza divulgativa (Frascati, 2015)
 - <http://www.inf.infn.it/edu/openlabs/2015/raggi-x.php>

About me (as a Lecturer)

- **Dipartim. Clin. di Scienze med., chirurgiche e della salute**
 - Radiology technicians
 - Physics of X-ray Imaging
 - Physics of Nuclear Medicine
 - Physics of Magnetic Resonance Imaging
 - Laboratory technicians
 - Basic and Applied Physics
- **Dipartimento di Scienze della Vita**
 - Students of Biology
 - Basic and Applied Physics
- **Dipartimento di Fisica**
 - Units/ICTP Master of Advanced Studies in Medical Physics
 - Medical Imaging Fundamentals
 - Units/Uniud Corso di Laurea Magistrale Interateneo in Fisica
 - Medical Physics Laboratory

Course Topics



- Medical Imaging Fundamentals
 - Mathematical Methods
 - Linear Systems
 - Fourier Analysis
 - Acquisition, formation, processing and display of medical images
 - Evaluation of Image Quality

Some useful books

Author	Title	Year
Jerrold T. Bushberg, J. Anthony Seibert, Edwin M. Leidholdt, John M. Boone, editors.	The essential physics of medical imaging	2012
Richard Van Metter, Jacob Beutel, Harold Kundel, editors.	Handbook of medical imaging. Volume 1, Physics and psychophysics	2000
Webb, S.	The Physics of medical imaging	1988
Bracewell, R.N.	The Fourier transform and its applications	1986
Hasegawa, B. H.	The physics of medical X-ray imaging (or the photon and me: how I saw the light)	1990

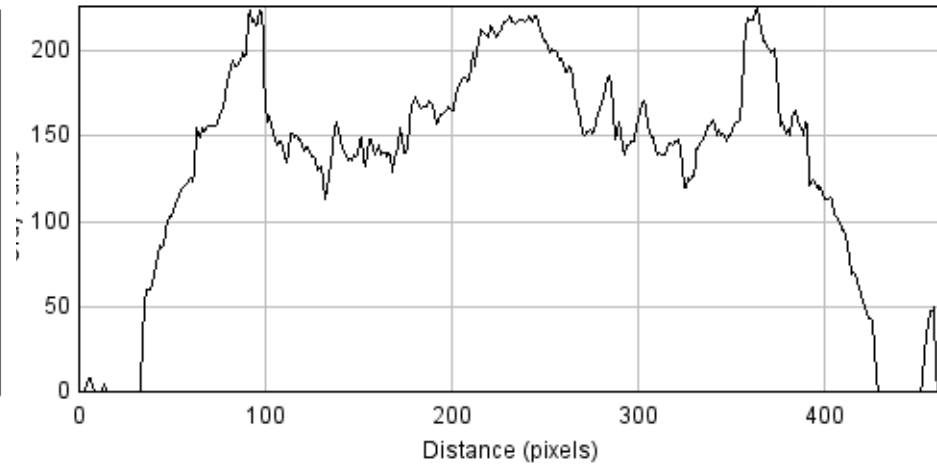
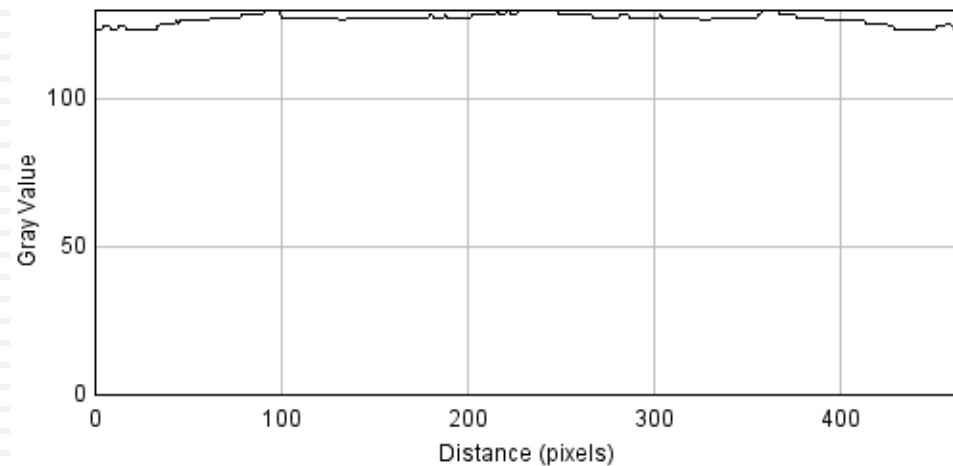
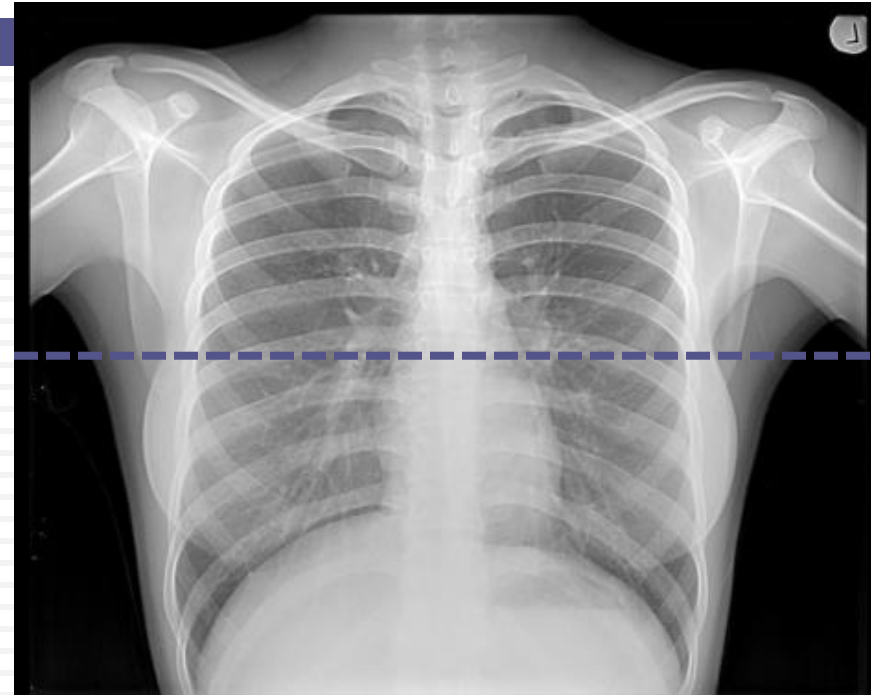
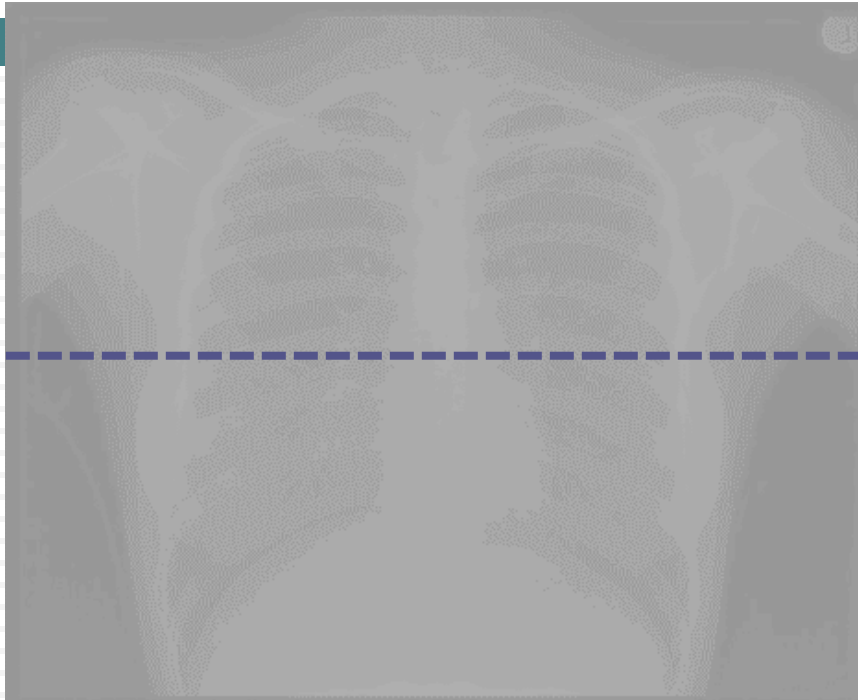
An invitation to Medical Imaging

An introduction inspired by the lectures of
prof. P. Sprawls (<http://www.sprawls.org/>)

Image quality

- In our simplified scheme, image quality depends from 5 factors:
 - Contrast
 - Blur (detail visibility - spatial resolution)
 - Background Noise
 - Artifacts
 - Distortions
- We will now briefly review these points, which will be studied in detail in the next lectures
- Our brief review will use the simplest imaging method (i.e. planar radiology) as a case study

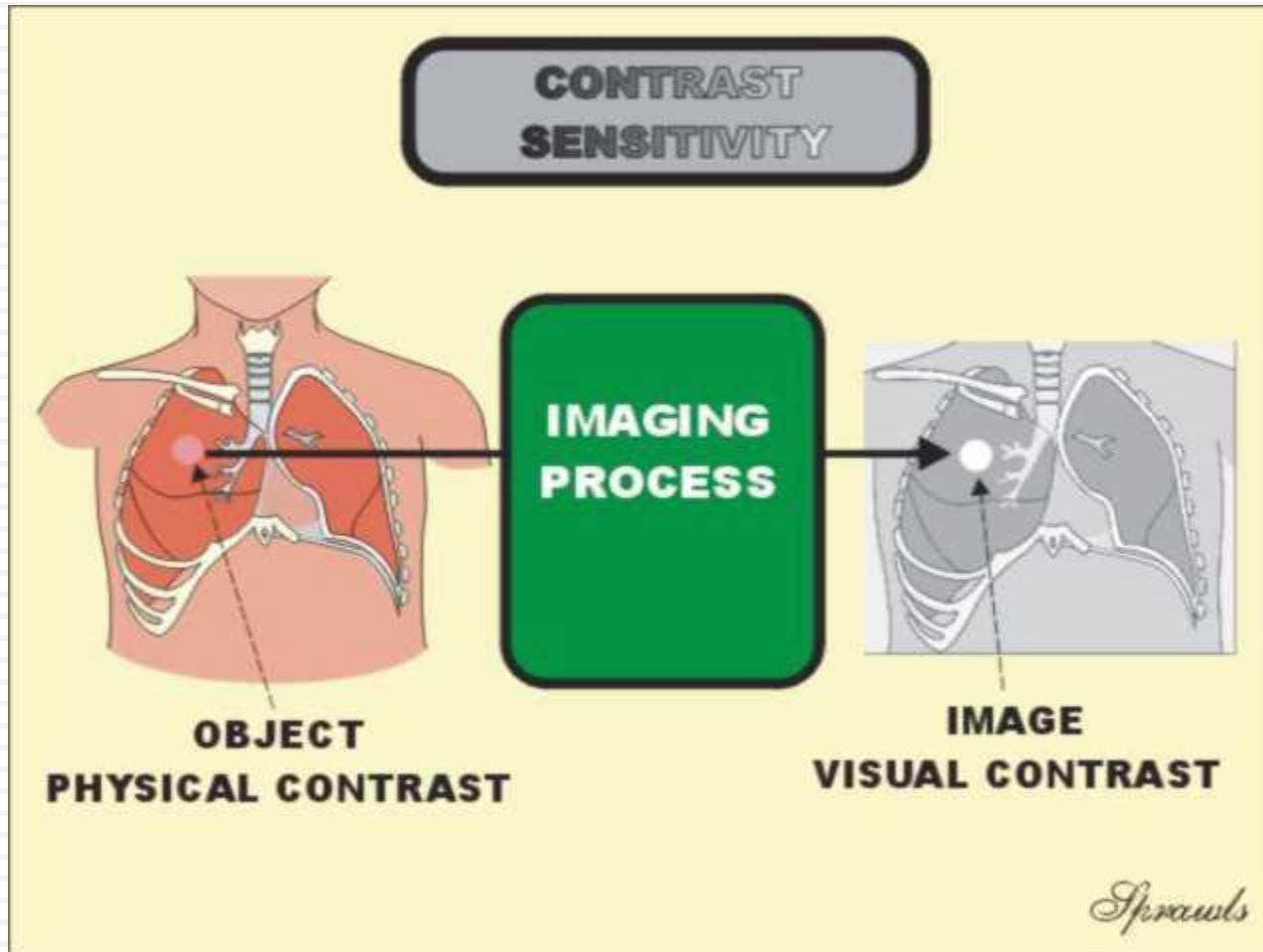
Contrast



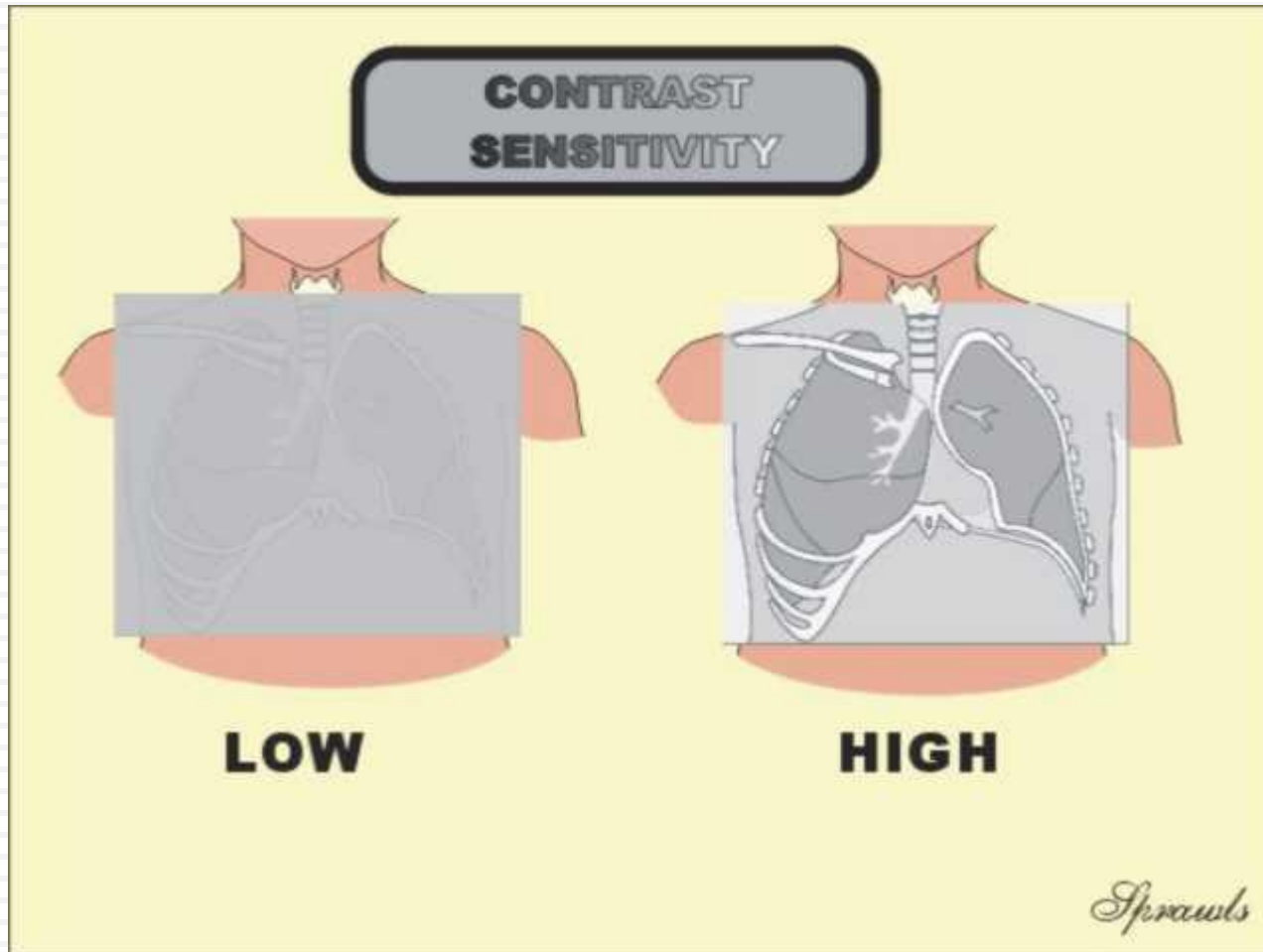
Contrast

- Contrast represents the difference in one or more characteristics of the object between two specific points in the image.
- In the (digital) image it is typically represented by various tonalities of gray (gray values or gray levels).
- The contrast required to make an object visible depends both upon the imaging method and upon the characteristics of the imaging system.
- Different imaging methods are sensitive to different contrasts.
 - For example, one method could give evidence to different densities of the tissues, another to different atomic numbers, another to different elastic properties, another to different relaxation times, another to different concentrations of radioactive substances, etc.
 - These differences represent the physical contrast.
- The fundamental characteristic of an imaging method is its contrast sensitivity, i.e. the ability to render a physical contrast as a contrast on the image (image contrast).

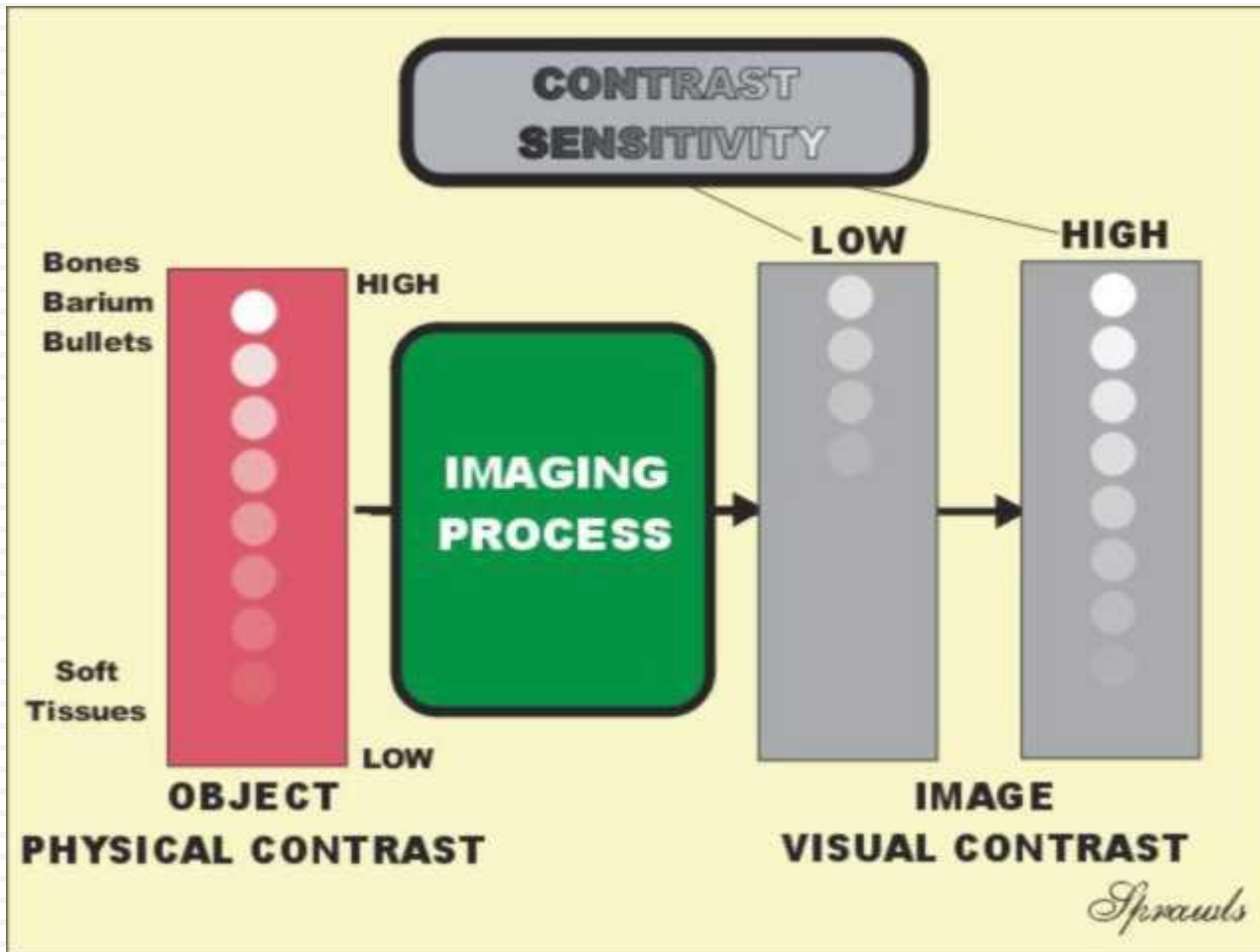
Contrast Sensitivity



Contrast Sensitivity



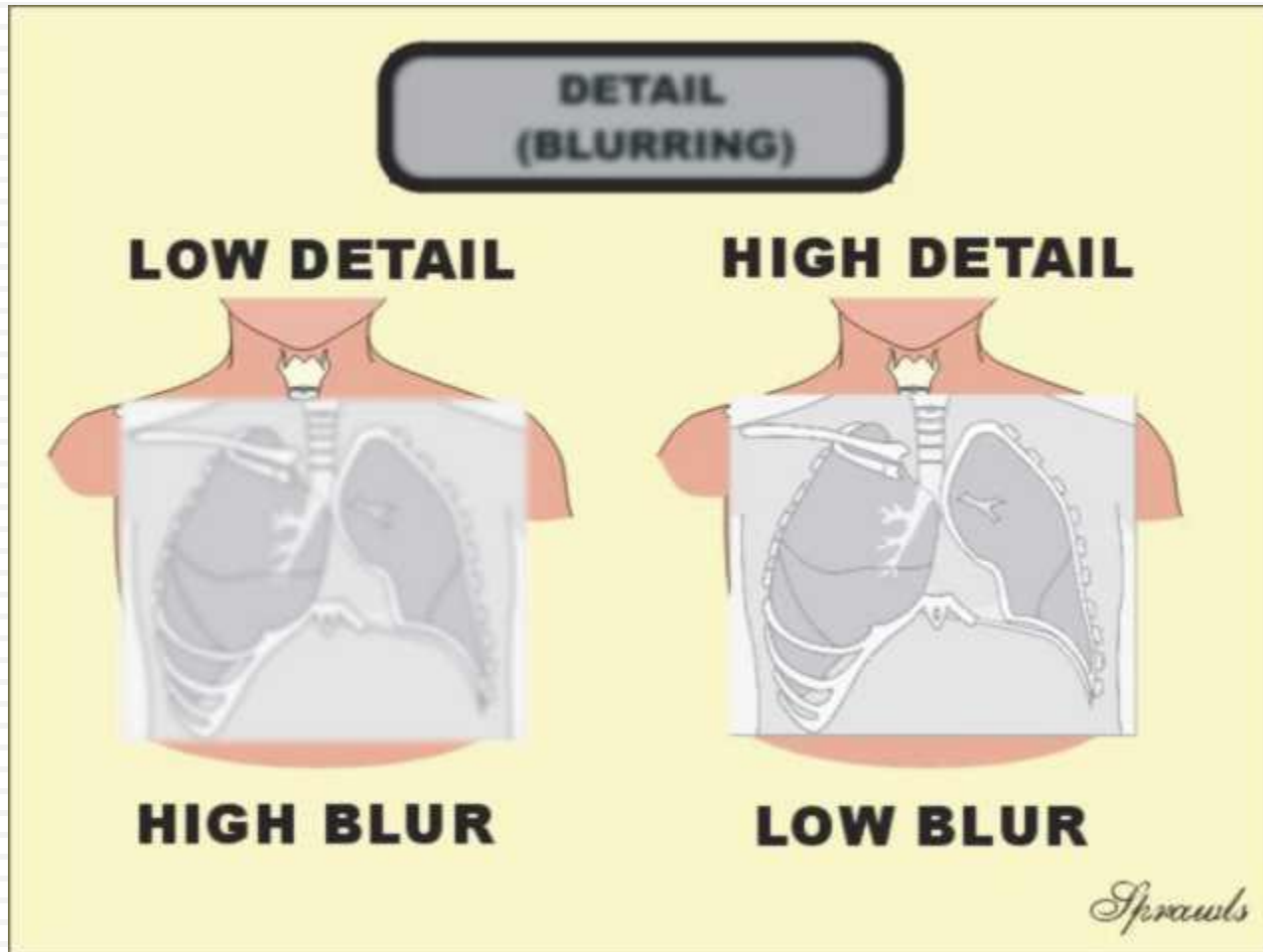
Contrast Sensitivity



Blur (detail visibility – spatial resolution)

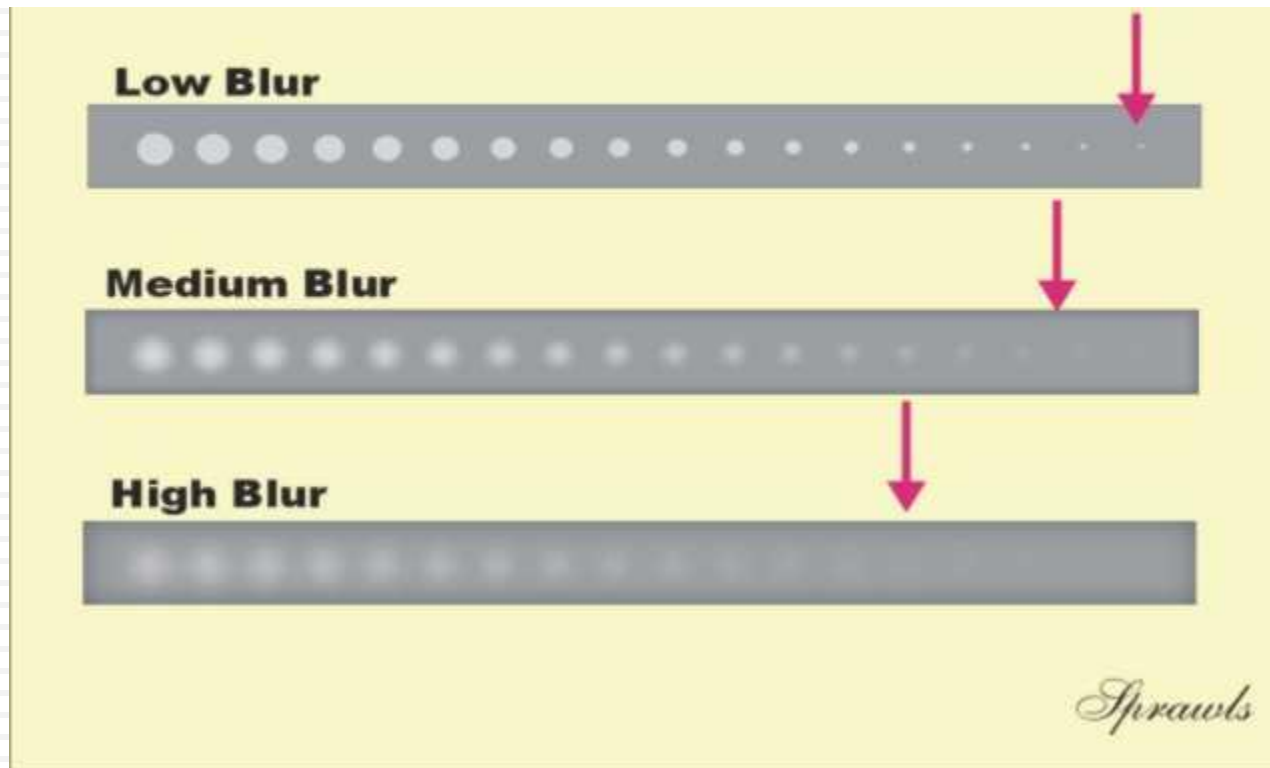
- Inside the body the objects differ not only for their characteristics but also for their dimensions, from the large organs and the bones, to the small calcifications.
- Each imaging method has a lower limit of the dimensions of the objects that can be resolved, and therefore of the details visibility.
- The visibility is limited since every imaging method introduces some "blurring" in the process.

Blur (detail visibility – spatial resolution)

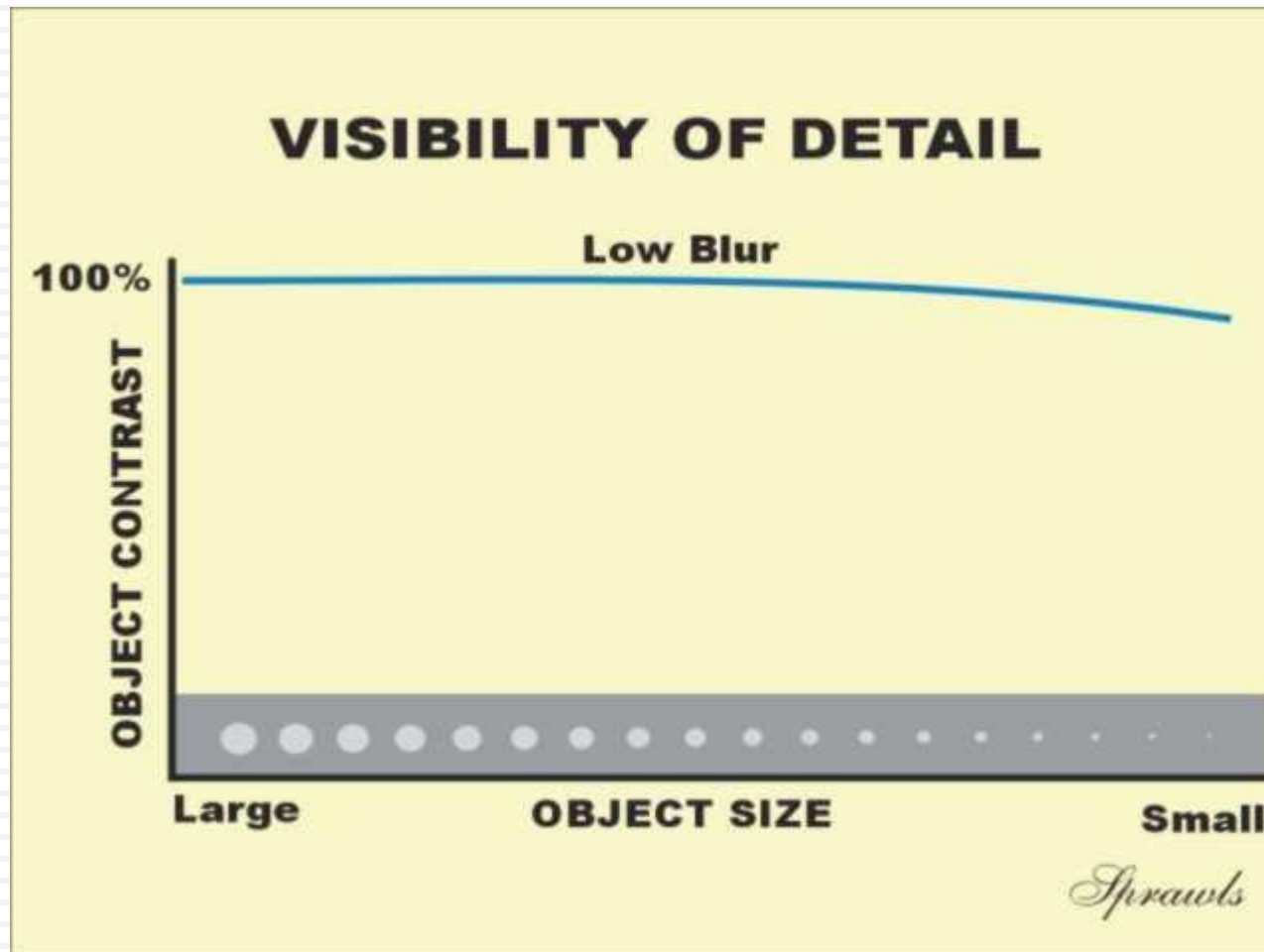


Blur (detail visibility – spatial resolution)

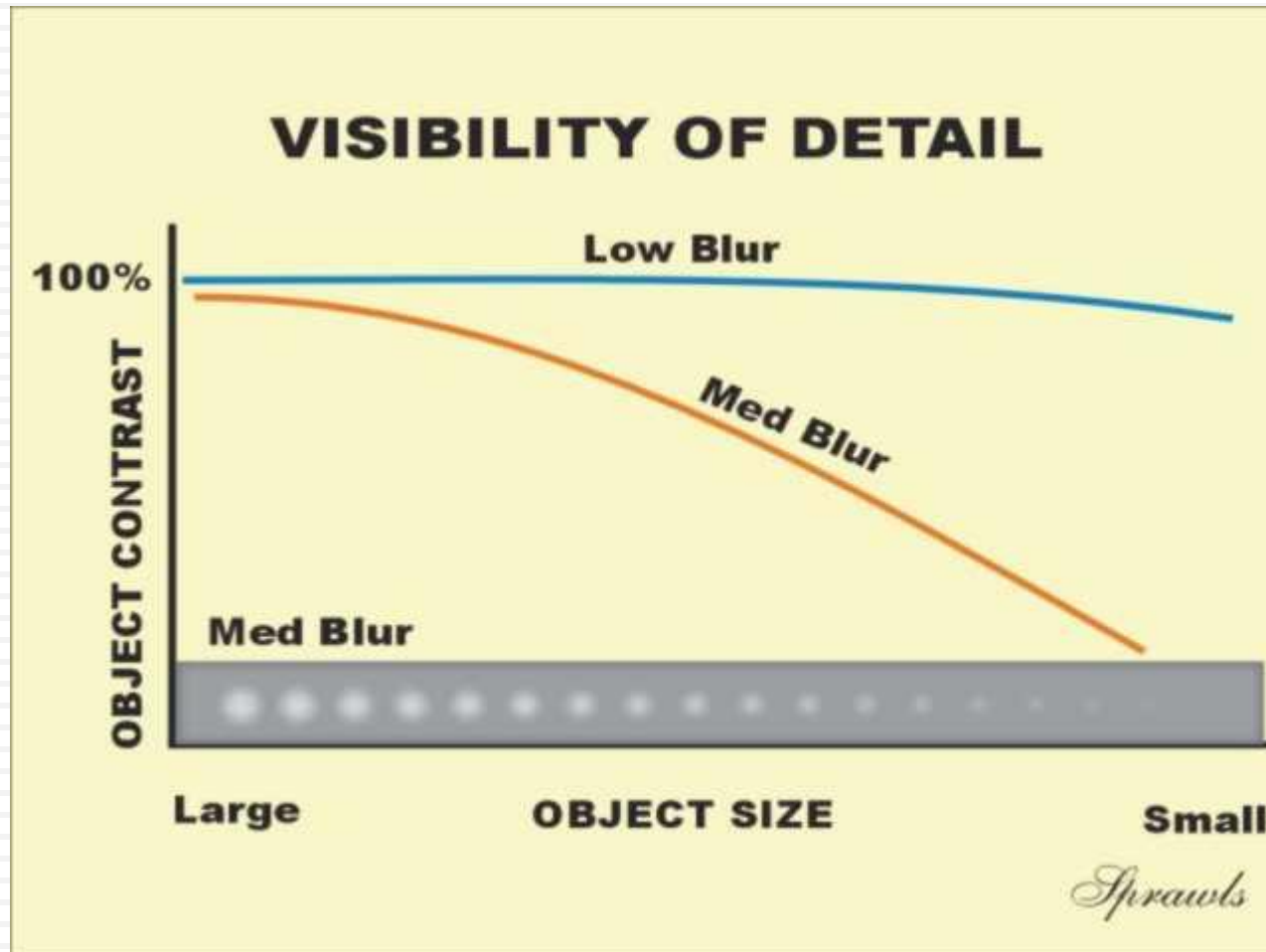
Obviously the blur has a little effect on the visibility of large objects, while it reduces the visibility and the contrast of small objects



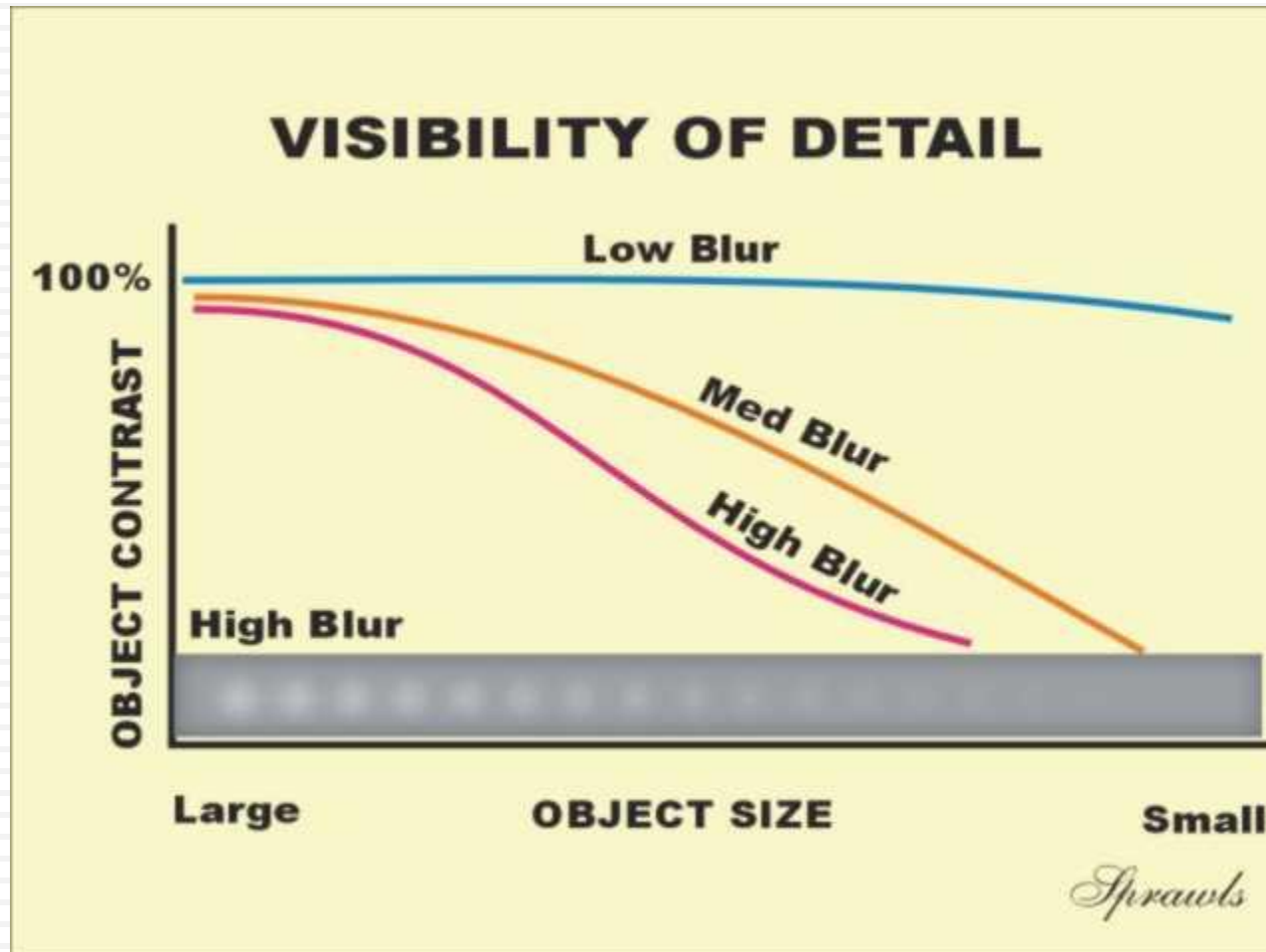
Blur (detail visibility – spatial resolution)



Blur (detail visibility – spatial resolution)

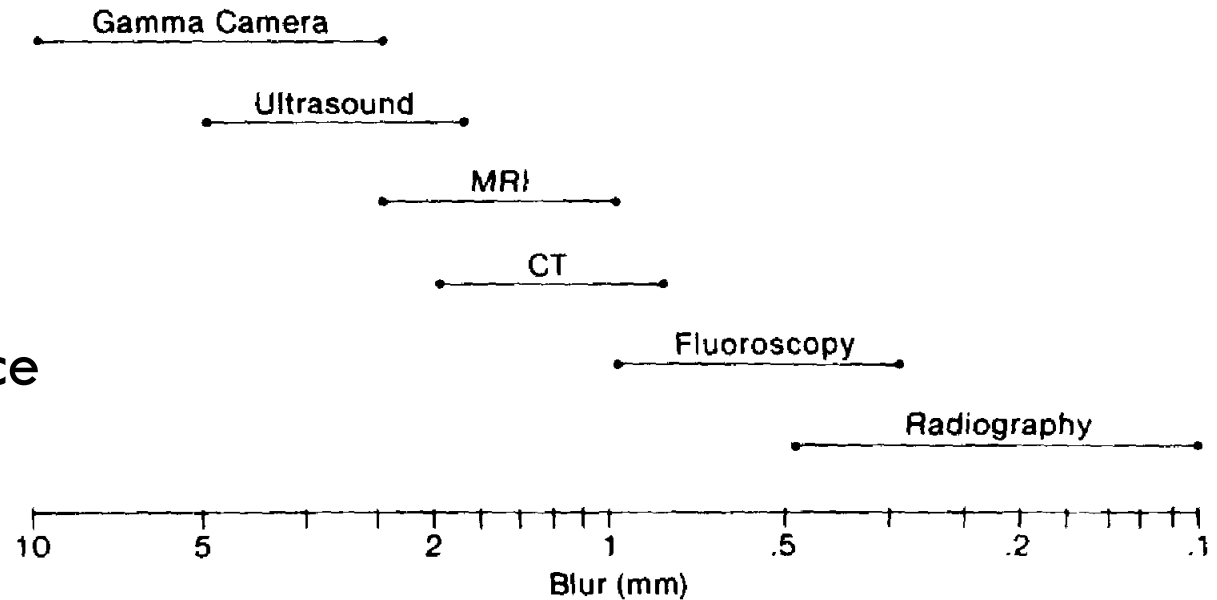


Blur (detail visibility – spatial resolution)



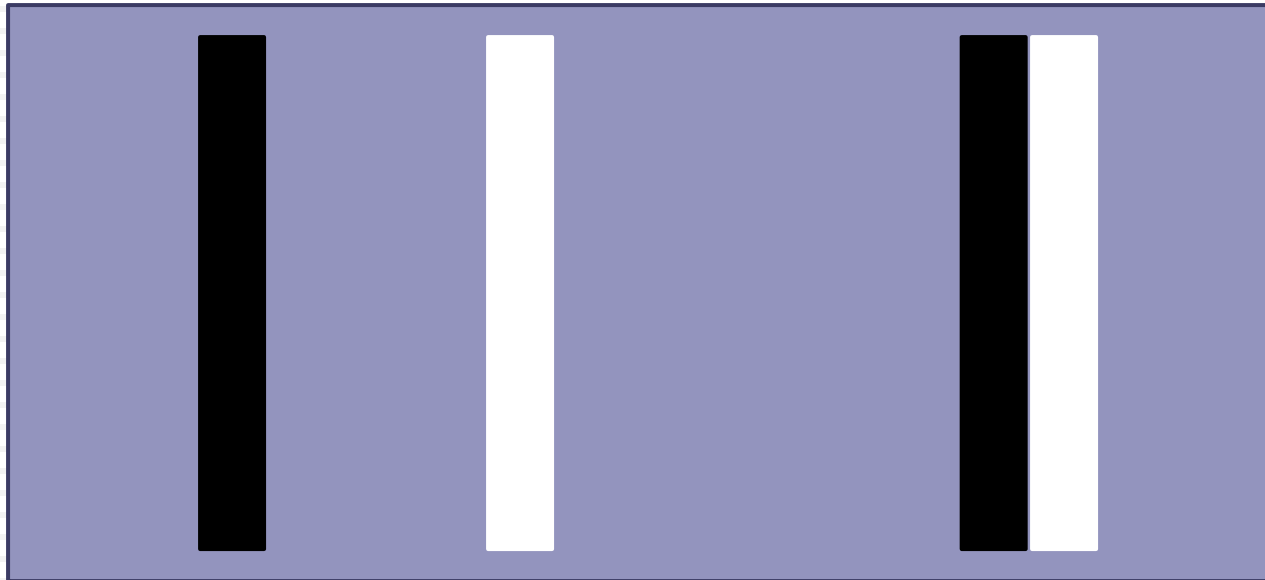
Blur (detail visibility – spatial resolution)

- gamma camera
 - ▣ from 10 to 3 mm
- ultrasounds
 - ▣ from 5 to 2 mm
- magnetic resonance
 - ▣ from 3 to 1 mm
- tomography
 - ▣ from 2 to 0.8 mm
- fluoroscopy
 - ▣ from 1 to 0.4 mm
- conventional radiography
 - ▣ from 0.5 to 0.1 mm (down to 0.05 in mammography)

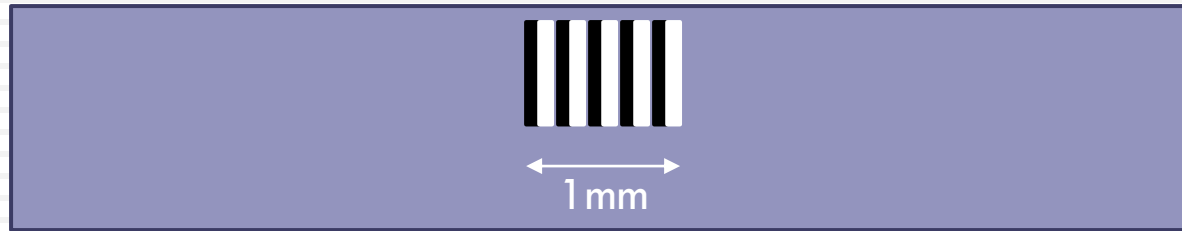


Spatial resolution (lp/mm)

- The spatial resolution of an imaging method is often defined in terms of "line pairs per millimeter", lp/mm
- A line is either a dark line or a light line; a line pair comprises a dark line and an adjacent light line.

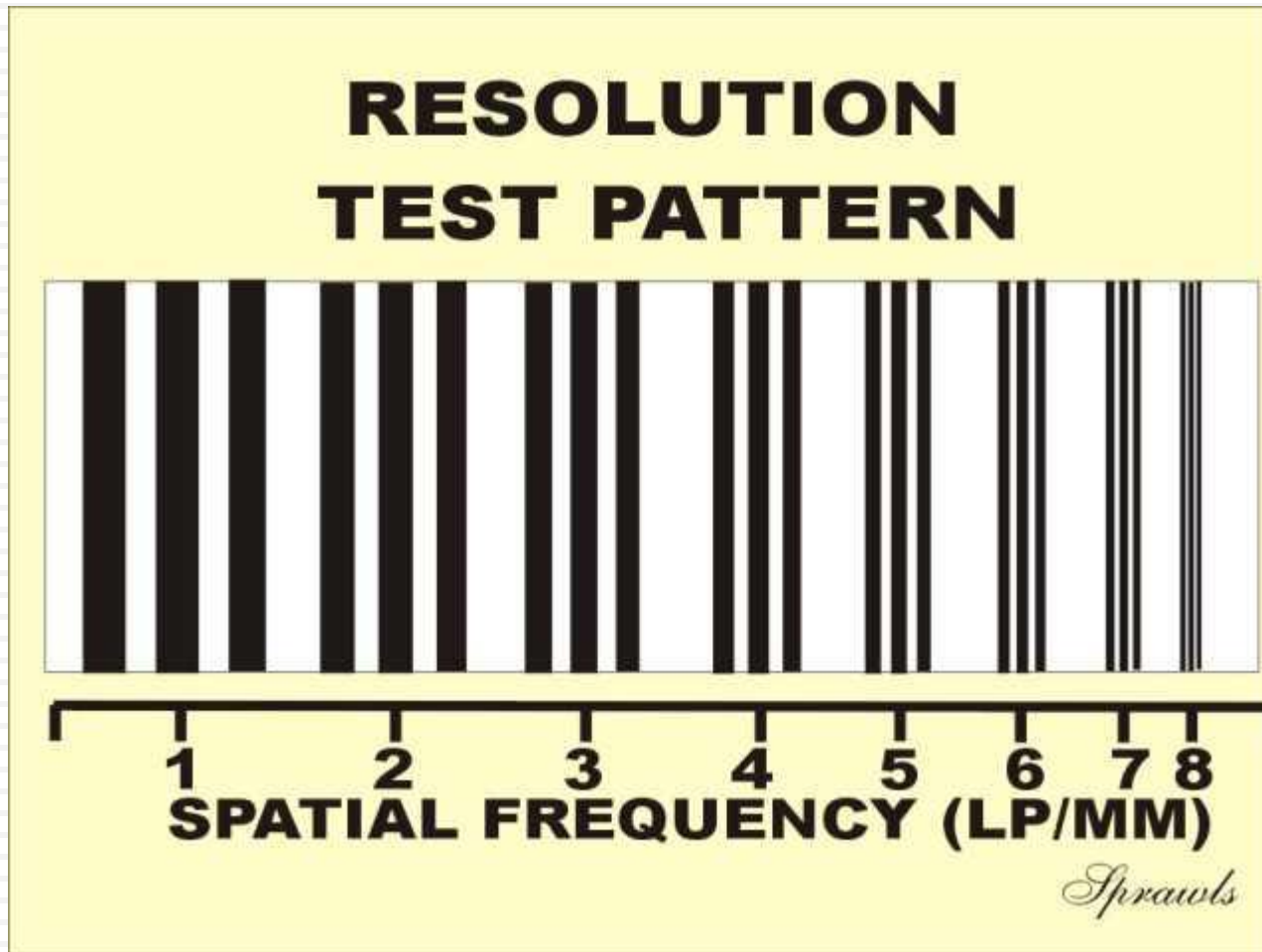


Spatial resolution (lp/mm)

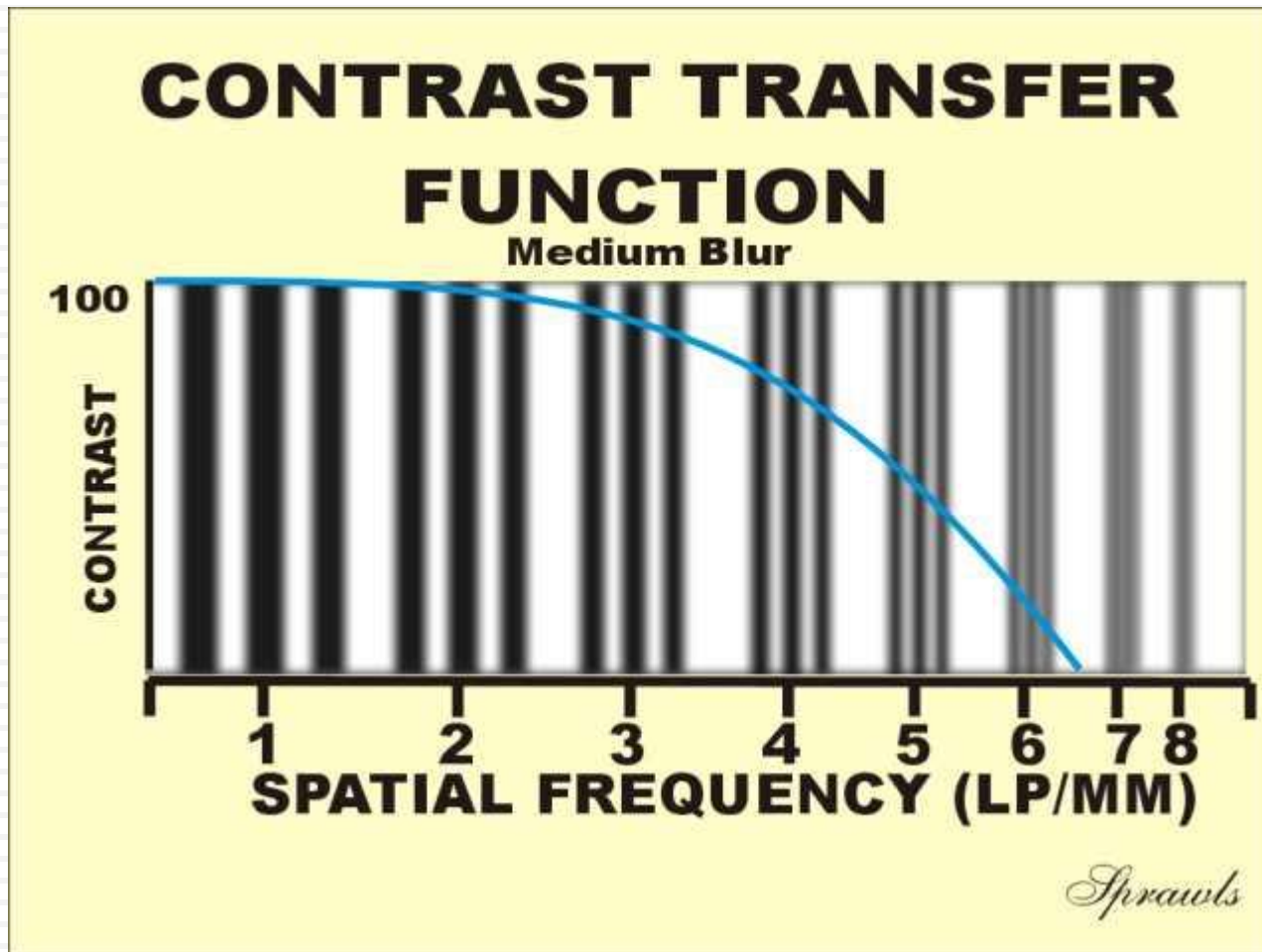


- Example: a resolution of 10 lines per millimeter means that the system can render:
 - 5 dark lines of 0.1 mm alternating with 5 light lines of 0.1 mm.
 - Overall, I have 10 lines in 1 mm, i.e. 5 line pairs per millimeter (5 lp/mm).
- The number of lp/mm defines a spatial frequency
- The higher spatial frequency that the system can render, the better its spatial resolution.

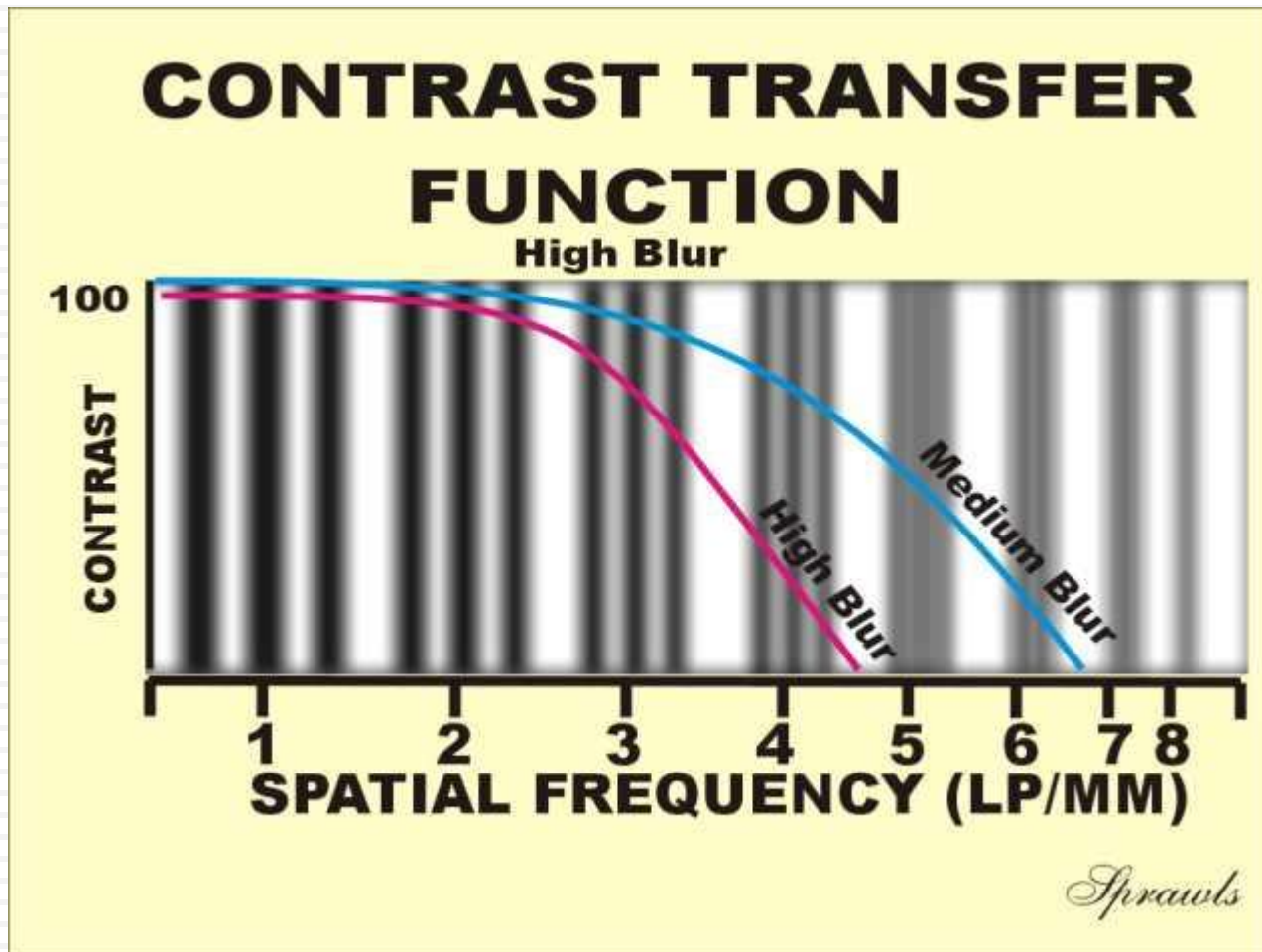
Spatial resolution (lp/mm)



Spatial resolution (lp/mm)



Spatial resolution (lp/mm)



Noise

- The background noise gives a "granular" aspect to the image, and tends therefore to diminish the visibility of small and/or low-contrast objects.



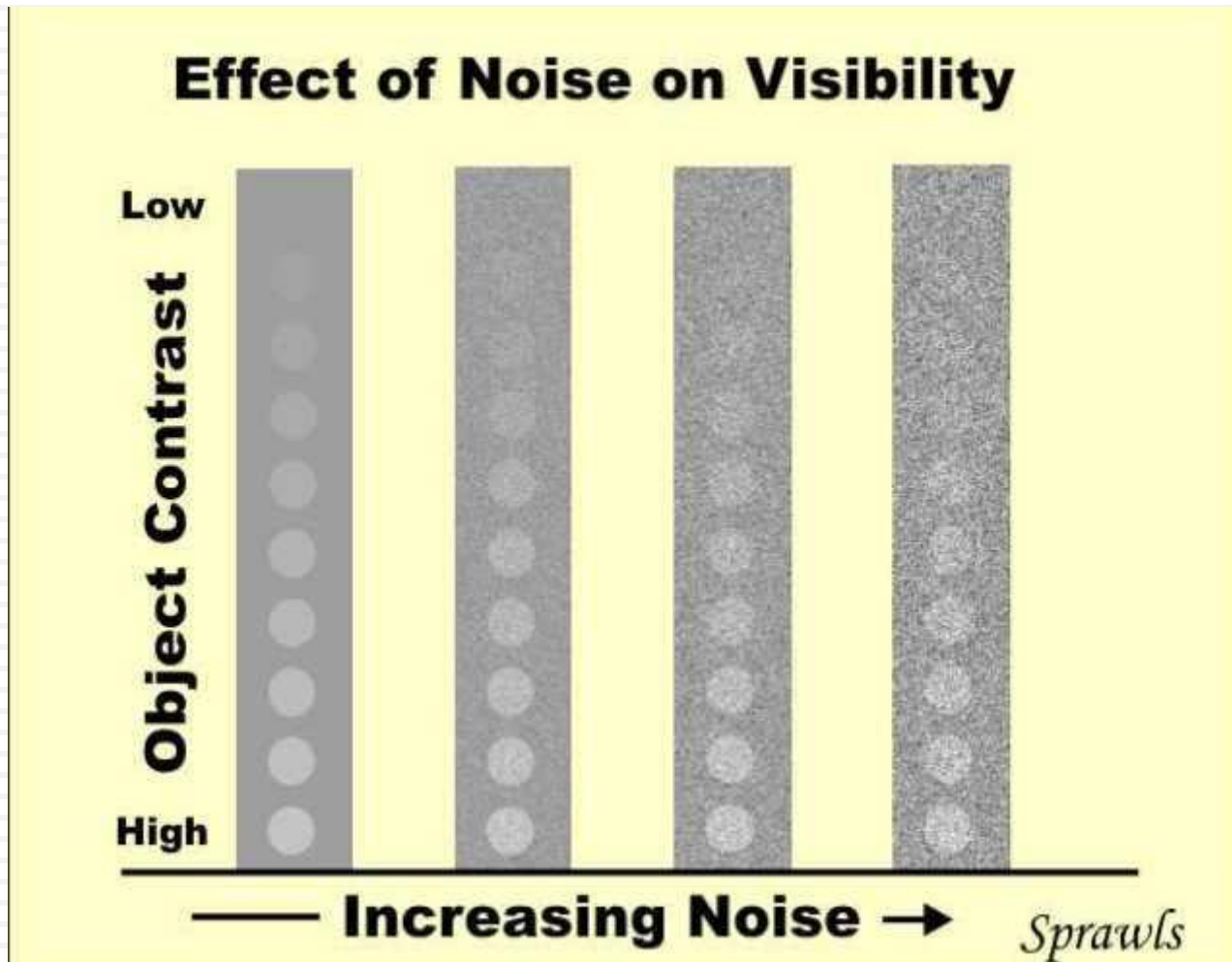
LOW



HIGH

Sprawls

Noise



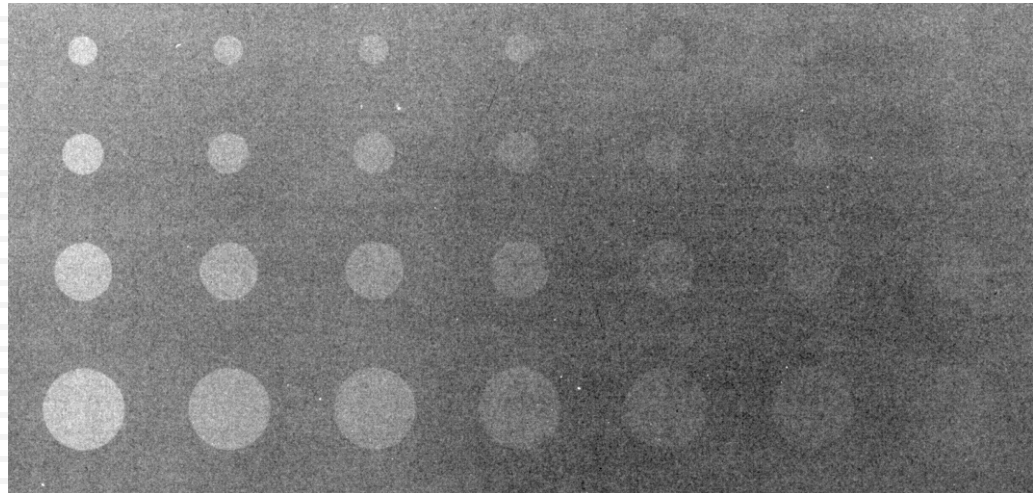
Contrast-Detail (CD) phantom

- A CD phantom allows to quickly assess the Blur and Noise characteristics of an imaging system.
- The phantom contains a matrix of details.
 - ▣ All of the details in a given row have a constant contrast.
 - ▣ All of the details in a given column have a constant size.

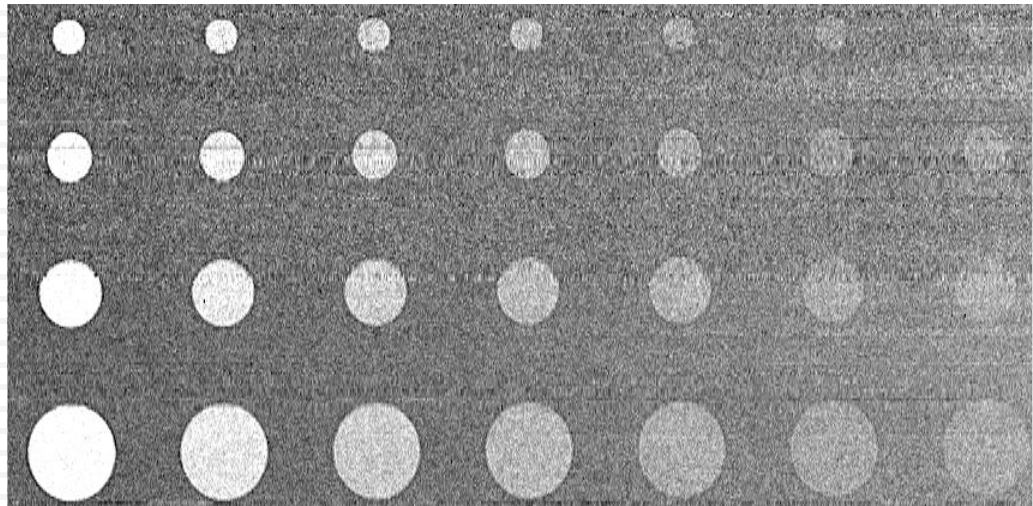


Example: system comparison with CD

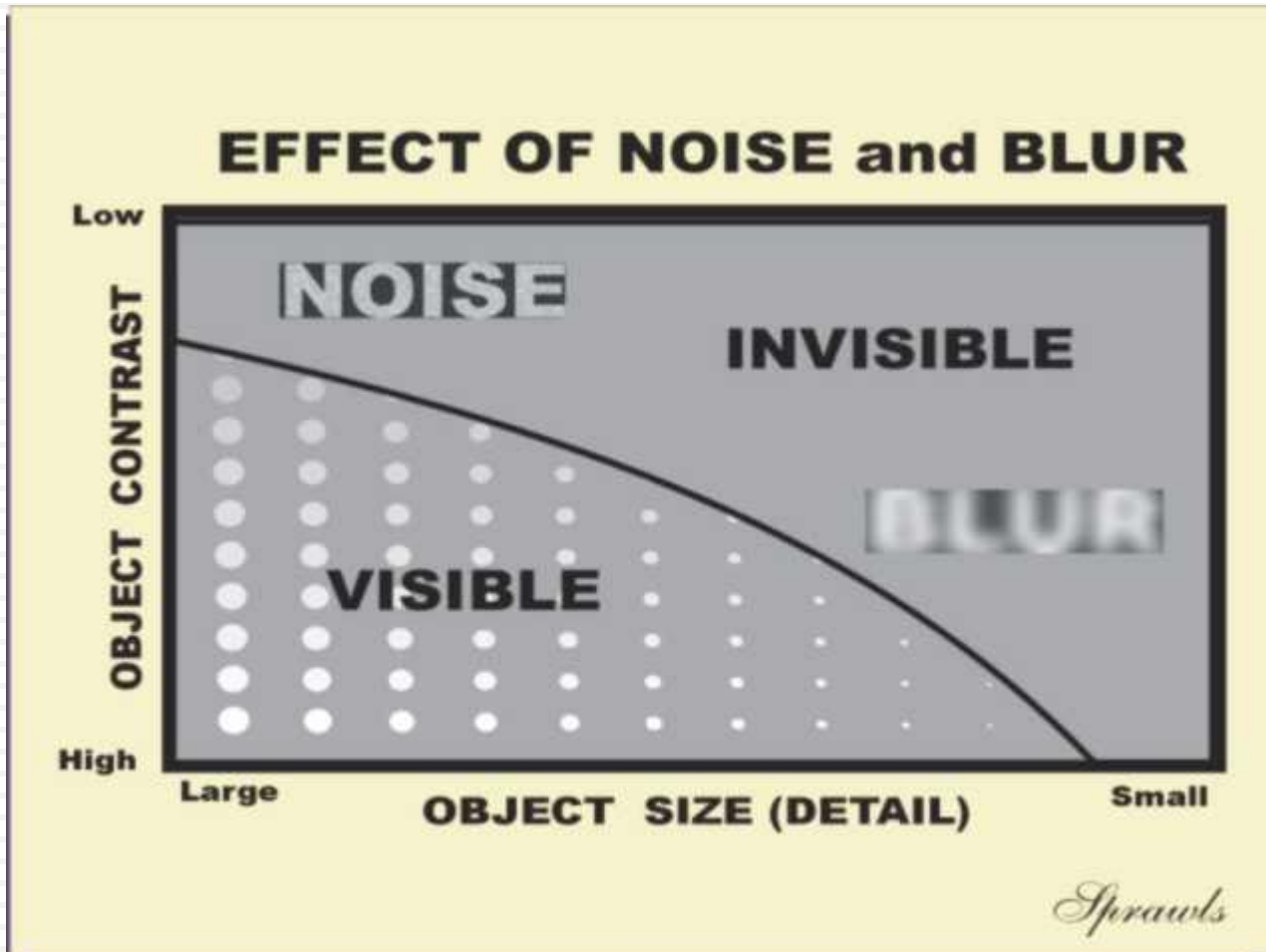
1.
Conventional Screen-Film
Mammographic system
26 kVp
Dose: 1.8 mGy



2.
"Frost" Digital detector (INFN)
Single photon counting
Synchrotron radiation
20 keV
Dose: 1.4 mGy

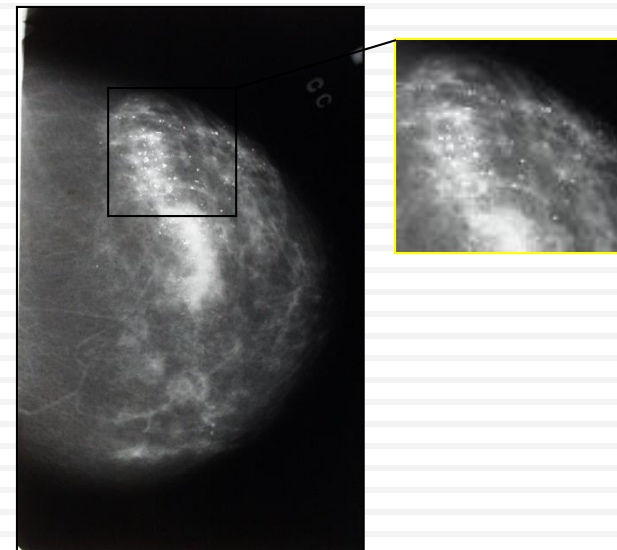
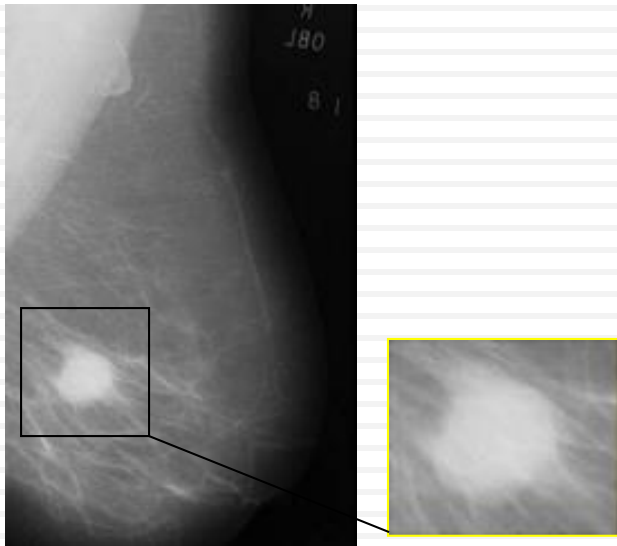


Blur Vs Noise: effect on visibility



Structural Noise

- An example from mammography
- In mammography, radiologists evaluate the presence of
 - ▣ Masses
 - ▣ Micro-calcifications



Structural noise

- But these features may be hard to find in dense breasts, due to the presence of healthy glandular tissue (structural noise)

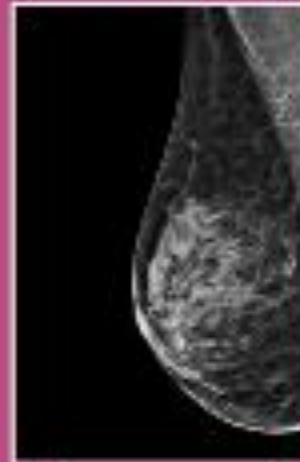
Radiologists classify breast density using a 4-level scale:



almost entirely
fatty



scattered areas
of fibroglandular
density



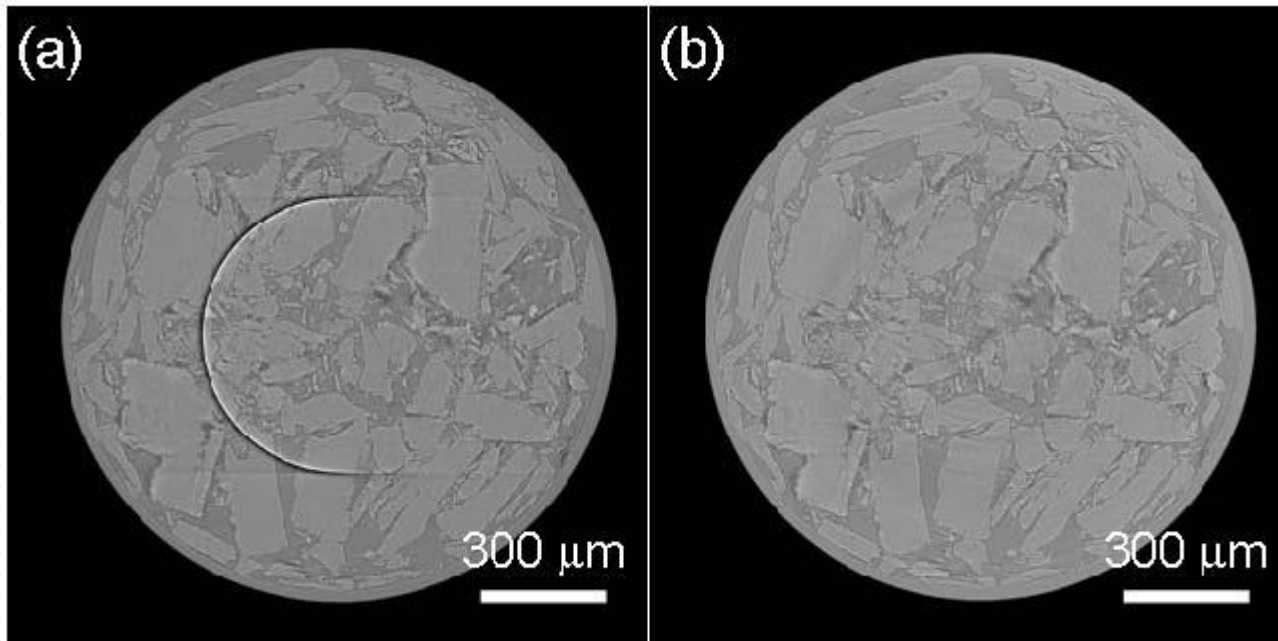
heterogeneously
dense



extremely
dense

Artifacts

- Most of the imaging techniques produce in the image characteristics that do not correspond to real structures of the object under examination. These "false" characteristics are known as "artifacts".

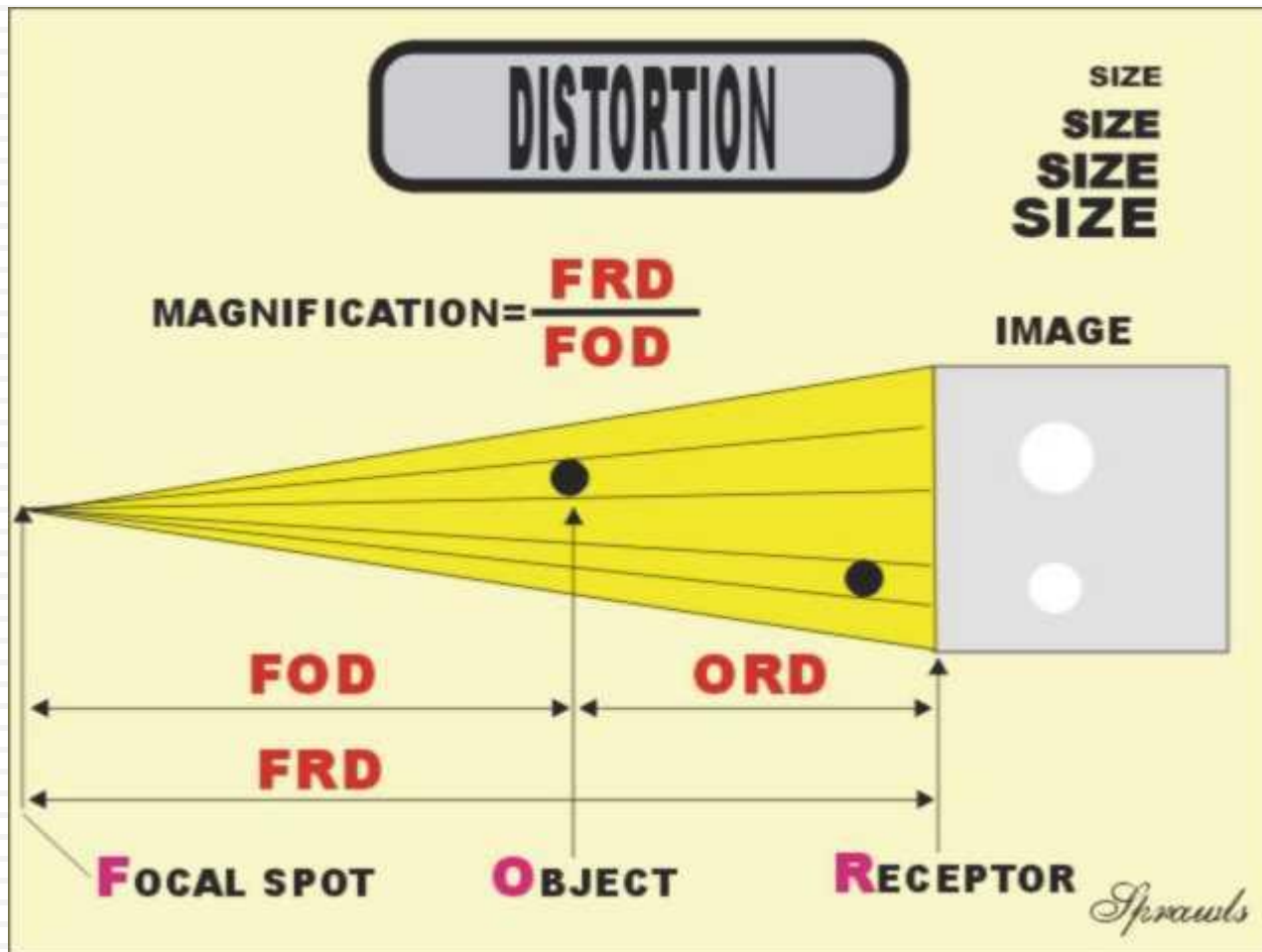


Distortions

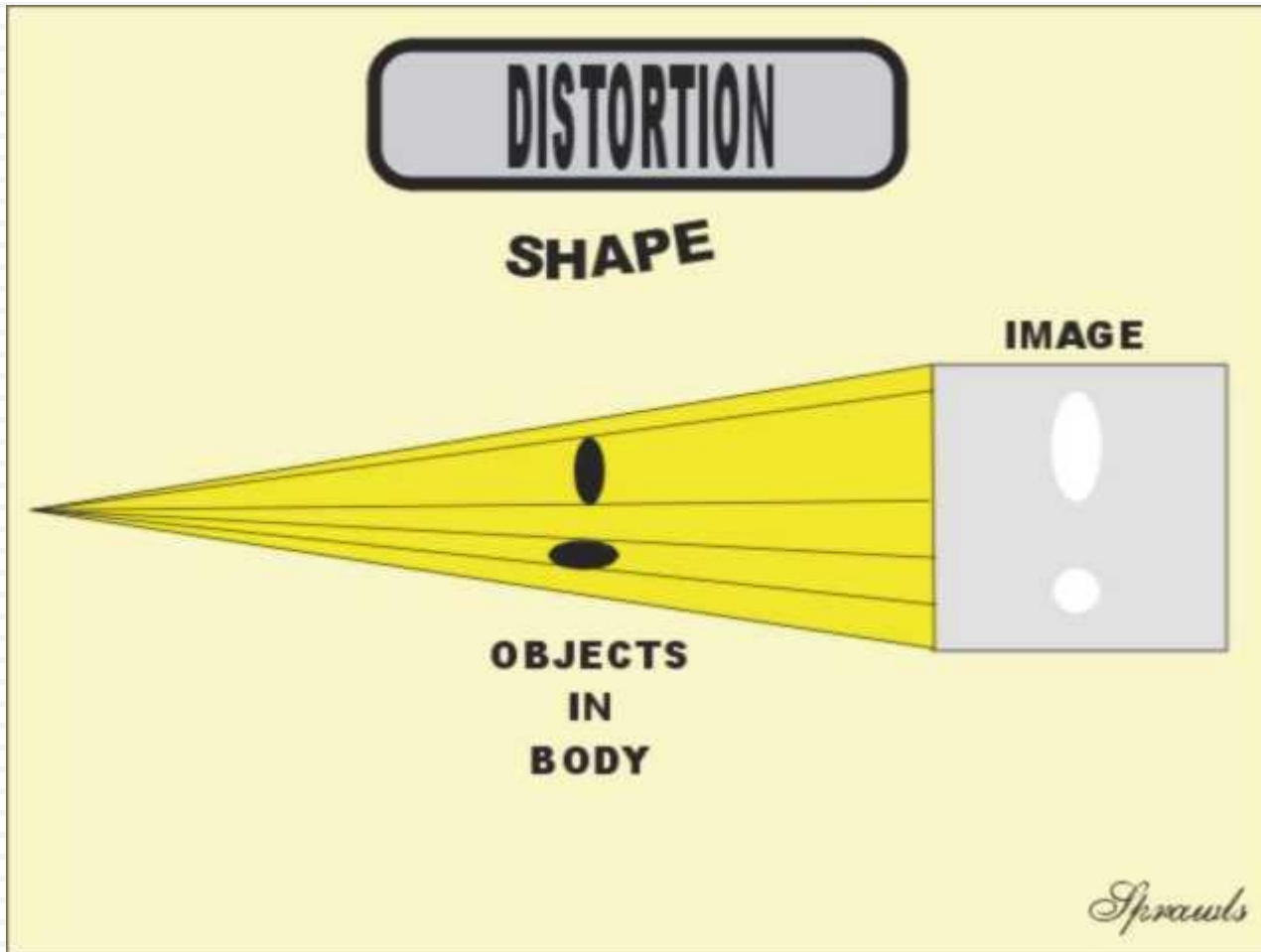
- An image should represent in an accurate way
 - ▣ Dimensions
 - ▣ Shape
 - ▣ Relative positions of the objects.

- Every imaging method can however introduce distortions in all these three factors.

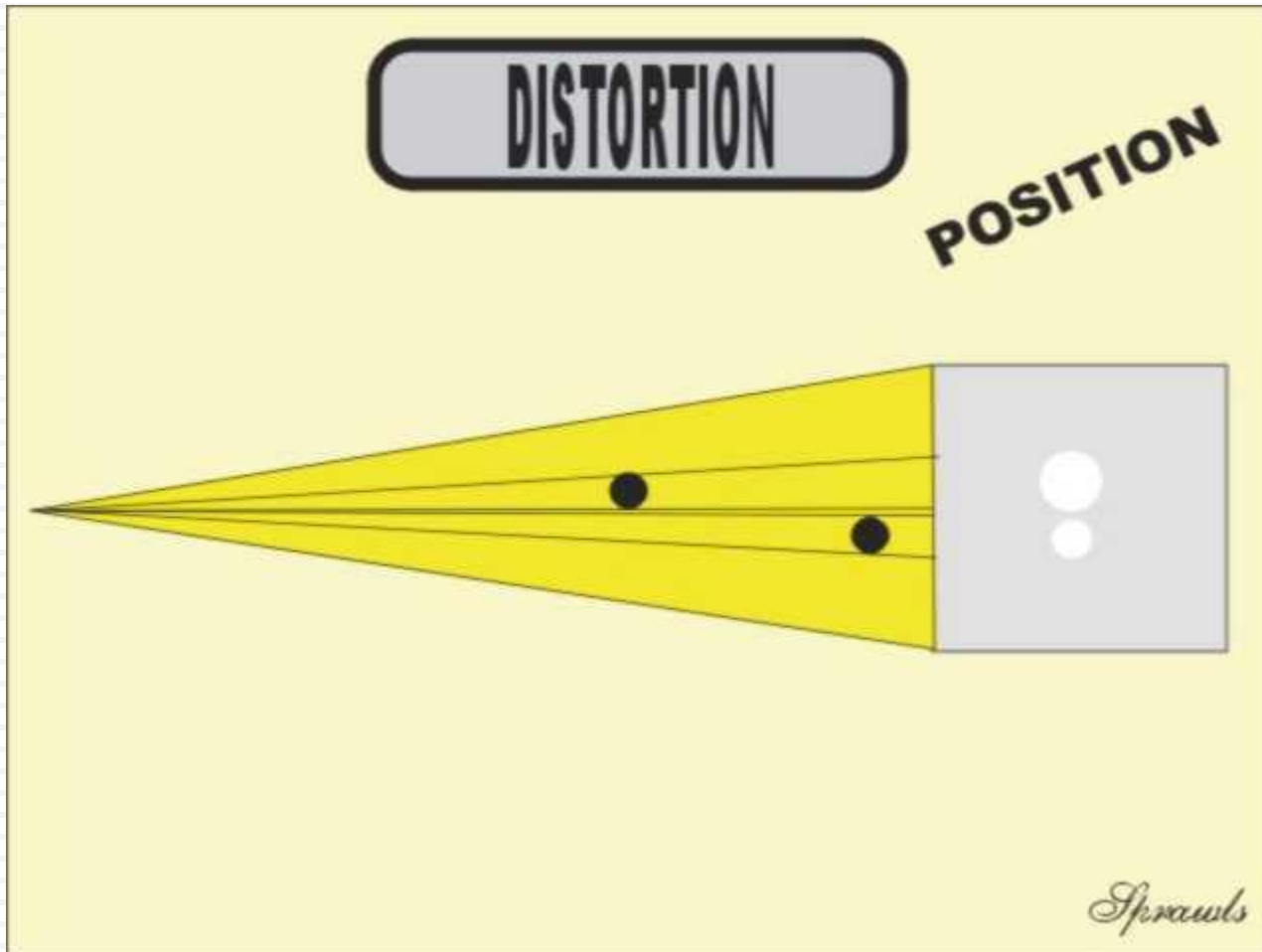
Distortions (size)



Distortions (shape)



Distortions (positions)



General concluding remarks

- In general, it would be advisable to optimize the various parameters of the measurement so that the maximal visibility is obtained.
- In many cases however changing one parameter improves one of the characteristic of the image, but other characteristics are worsened.
- Often one gets an improvement of the image to the detriment, for example, of the total time of the measurement, and this could lead to other possible inconvenients (increase of the exposure to radiations, possible movements of the patients, higher cost, etc.)
- One should therefore look for the best compromise among the different factors, according to the characteristics one desires to know best.