

# Cyber-Physical Systems

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Lecture: Examples

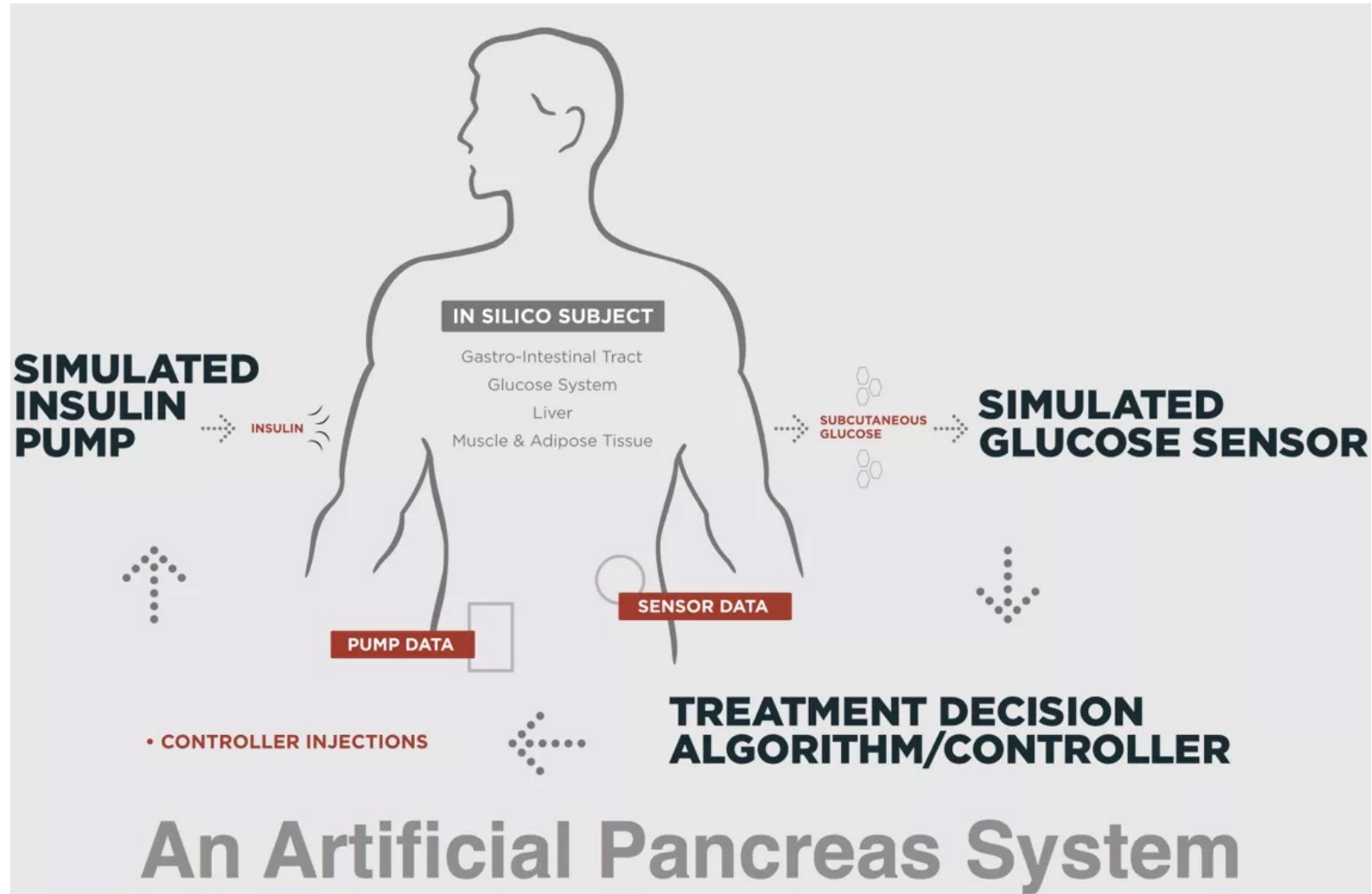
# Artificial Pancreas

Type 1 diabetes occurs when the pancreas produces little or none of the insulin needed to regulate blood glucose

They rely on external administration of insulin to manage their blood glucose levels.



# Artificial Pancreas



# Stochastic Hybrid Systems Of Glucose

$$\frac{d}{dt} \mathbf{x}(t) = F(\mathbf{x}(t); u(t); \Theta);$$

$$y(t) = x_1(t)$$

glucose concentration

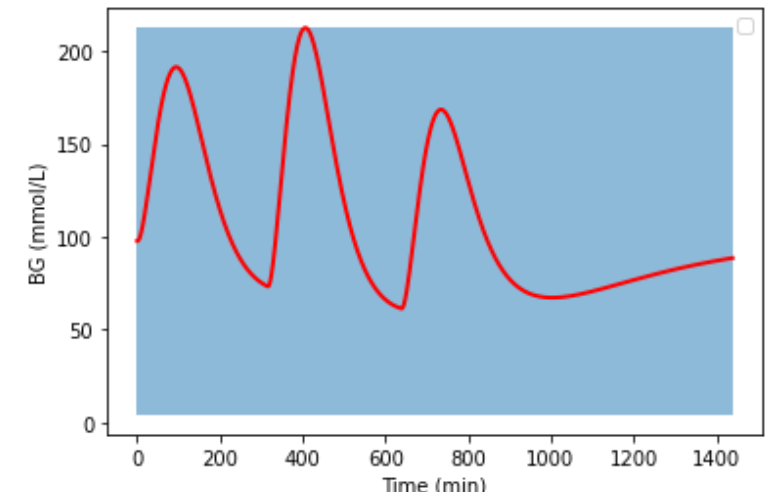
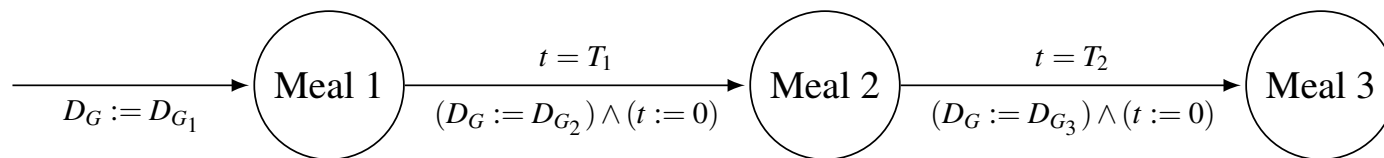
the control parameters

Infusion rate of bolus insulin

$\Theta = (D_{G_1}; D_{G_2}; D_{G_3}; T_1; T_2)$  are the control parameter

$(D_{G_1}; D_{G_2}; D_{G_3}) \in (N(40; 10); N(90; 10); N(60; 10))$  are the three daily meals

$(T_1; T_2) \in \sim N(300, 10)$  and  $T_2 \sim N(300, 10)$  are the inter-times between each of them



# Stochastic Hybrid Systems Of Glucose

$$\frac{d}{dt} Q_1(t) = -F_{01} - x_1 Q_1 + k_{12} Q_2 - F_R + EGP_0(1 - x_3) + \frac{D_G A_G}{t_{maxG}^2} t e^{-\frac{t}{t_{maxG}}}$$

$$\frac{d}{dt} Q_2(t) = x_1 Q_1 - (k_{12} + x_2) Q_2;$$

$$\frac{d}{dt} S_1(t) = u(t) + u_b - \frac{S_1}{t_{maxI}};$$

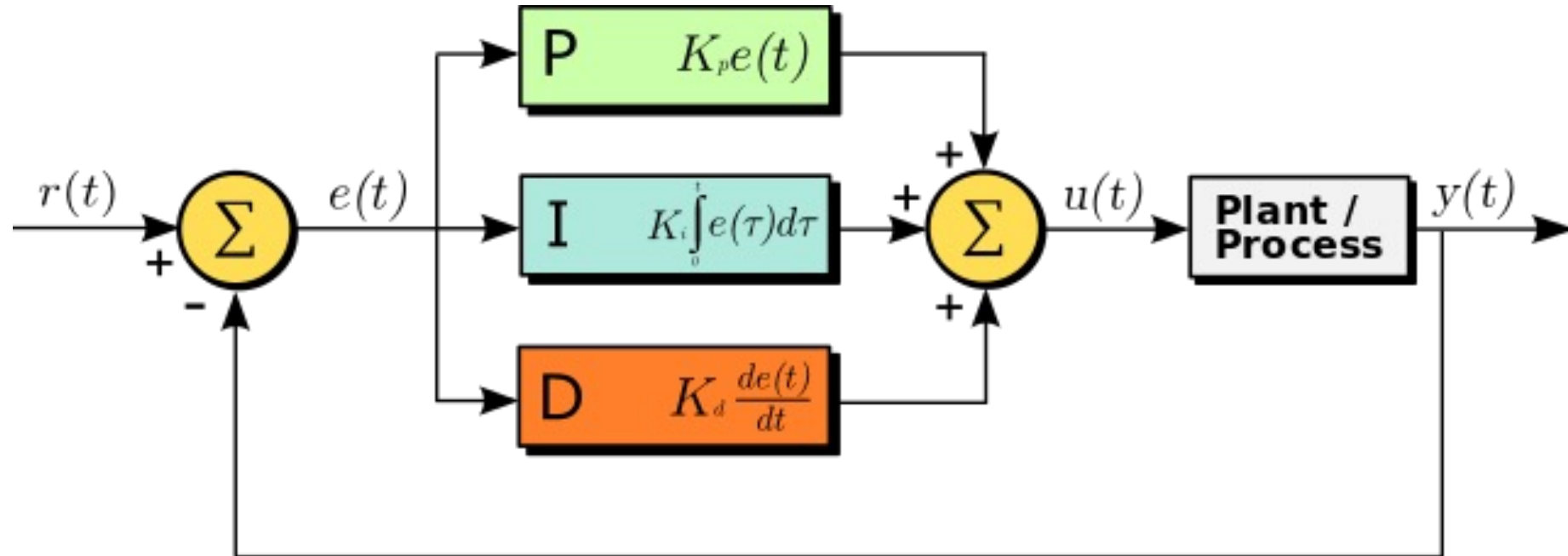
$$\frac{d}{dt} S_2(t) = S_1 - \frac{S_2}{t_{maxI}};$$

$$\frac{d}{dt} I(t) = \frac{S_2}{t_{maxI} V_I} - k_e I;$$

$$\frac{d}{dt} x_i(t) = -k_{a_i} x_i + k_{b_i} I; \quad (i = 1, 2, 3)$$

$$u(t) = K_p e(t) + K_i \int_0^t e(\tau) d\tau + K_d \frac{d}{dt} e(t), \quad e(t) = r(t) - y(t)$$

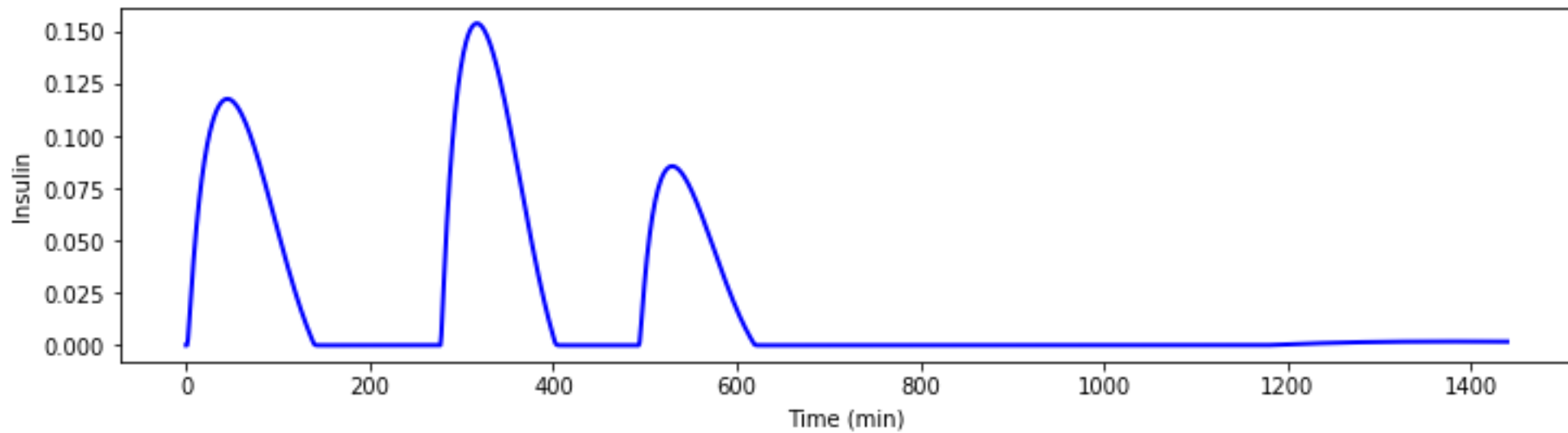
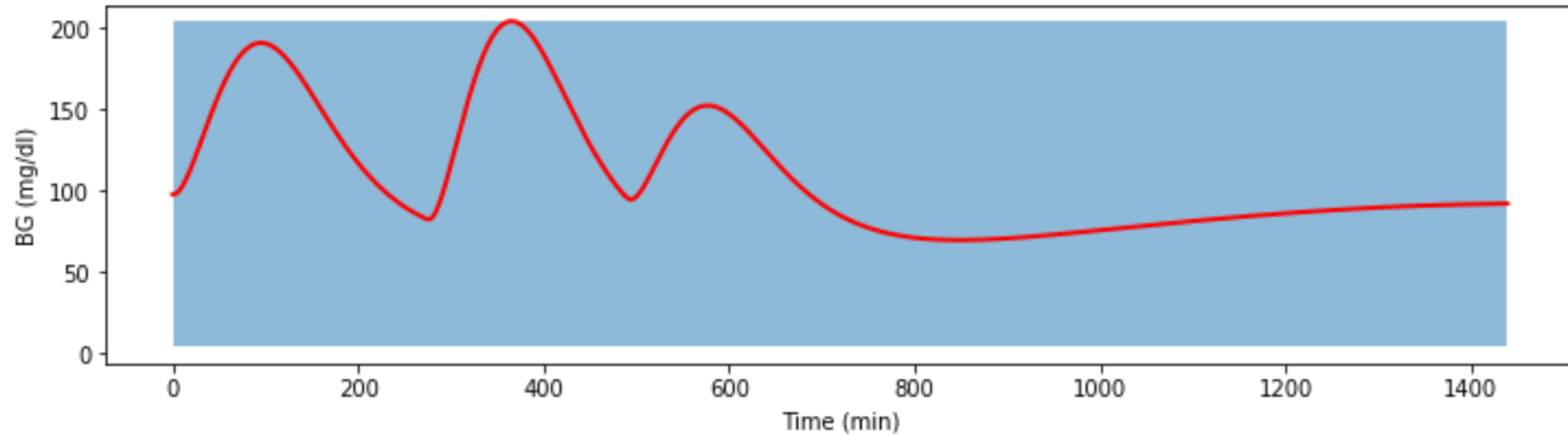
# PID Control



$$u(t) = K_p e(t) + K_i \int_0^t e(\tau) d\tau + K_d \frac{d}{dt} e(t),$$

$$e(t) = r(t) - y(t)$$

# Artificial Pancreas Simulation



# STL Properties for the Artificial Pancreas

## ▶ Hyperglycemia

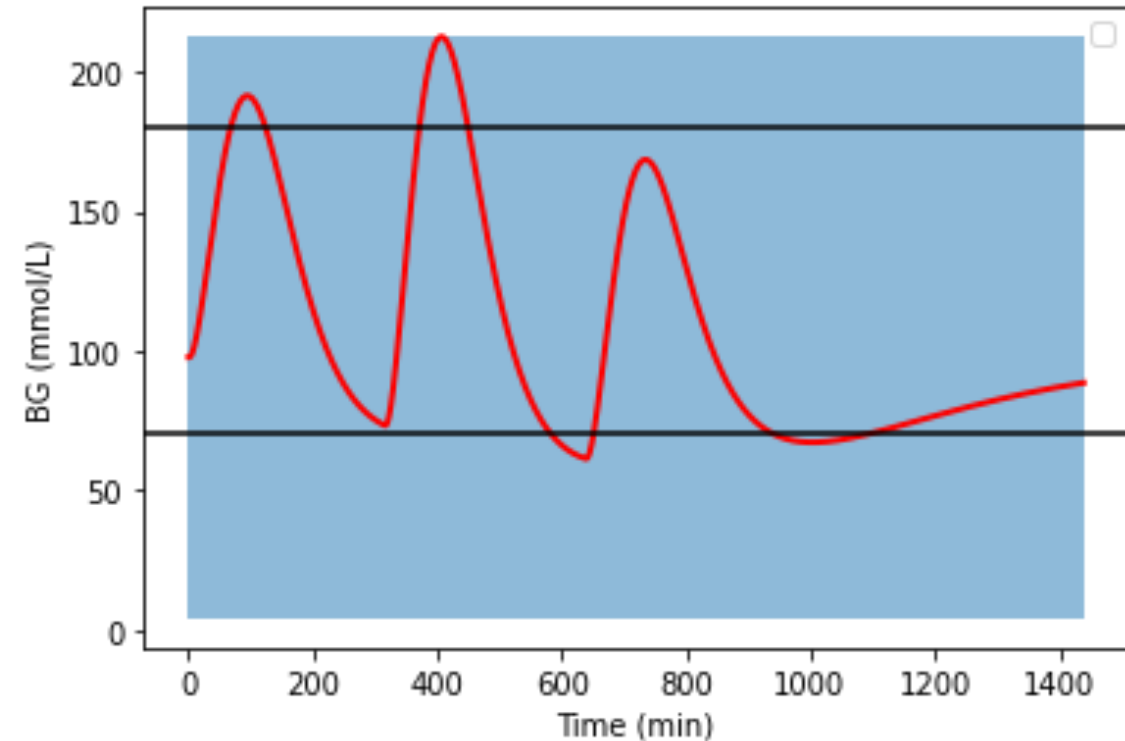
- ▶ “during the day the level of glucose goes above 180mg/dl”

$$\neg G_{[0,24h]}(BG(t) < 180)$$

## ▶ Hypoglycemia

- ▶ “during the day the level of glucose goes below 70mg/dl”

$$\neg G_{[0,24h]}(BG(t) > 70)$$





# STL Properties for the Artificial Pancreas

## ▶ Prolonged Hyperglycemia

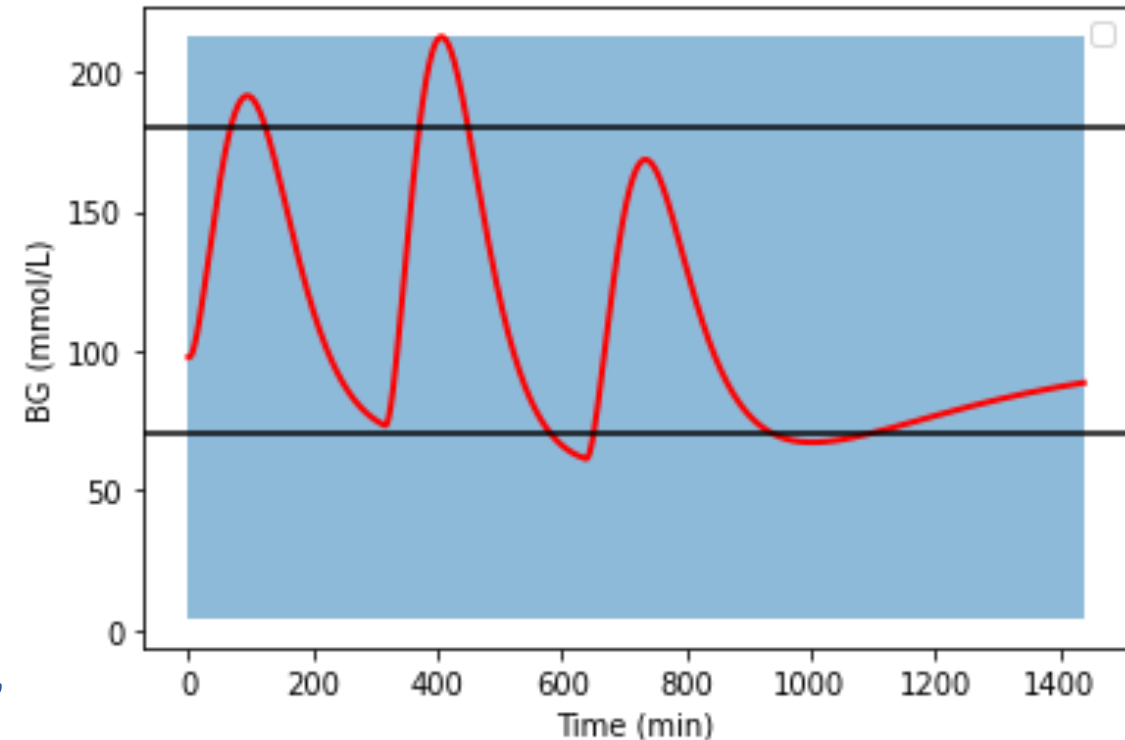
- ▶ “during the day the level of glucose goes above 180mg/dl for 3 hours”

$$F_{[0,21h]}(G_{[0,3]}(BG(t) \geq 180))$$

## ▶ Prolonged Hypoglycemia

- ▶ “during the day the level of glucose goes below 70mg/dl for 30 minutes”

$$F_{[0,21h]}(G_{[0,0.5]}(BG(t) < 70))$$



# Falsification

The most simple way to do falsification with respect a property  $\phi$  is minimizing the robustness over N iterations considering random samples on control parameters, i.e:

minSTL = 'inf'

For  $i = 1, \dots, N$ :

$\Theta = \text{sampling}(D_{G_1}, D_{G_2}, D_{G_3}, T_1, T_2)$

$t, y = \text{simulation}(\Theta)$

$\text{stl} = \text{computeRobustness}(y, \phi)$

if ( $\text{stl} < \text{minSTL}$ ):

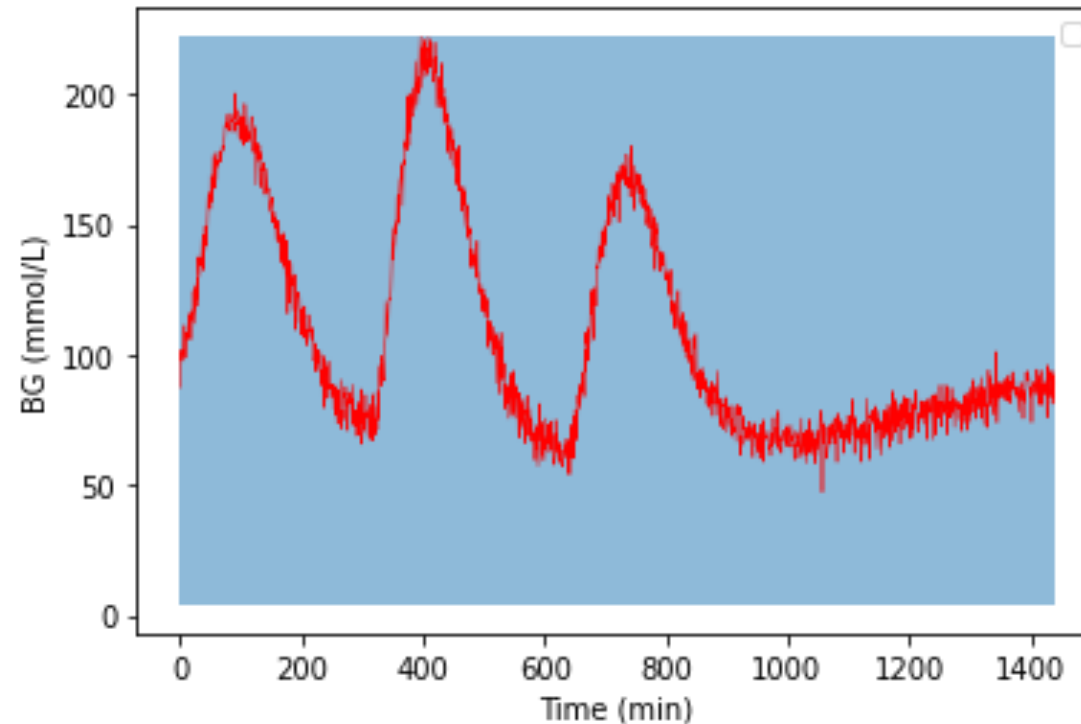
$\text{minSTL} = \text{stl}$

$\text{vSTL} = [D_{G_1}, D_{G_2}, D_{G_3}, T_1, T_2]$

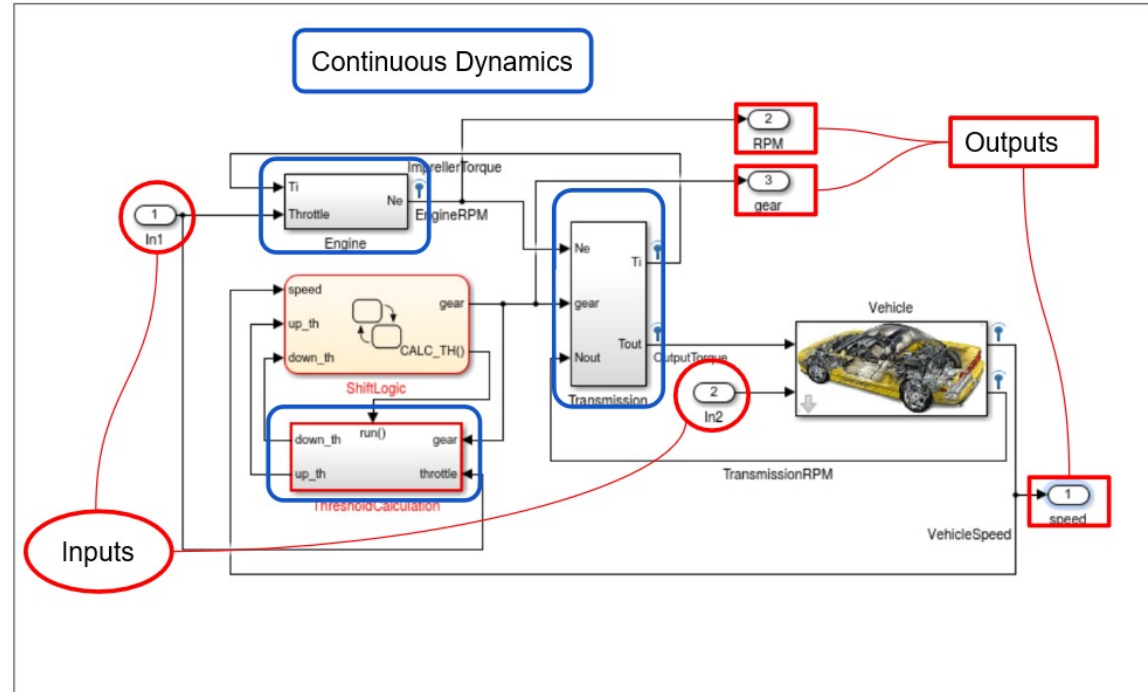
For fixed control parameter spaces you can consider to sample with respect to the grids over it.

# Noise Robustness

- ▶ To consider noisy sensor we can add a Gaussian noise to the generated glucose trajectory, i.e.  $GB(t) + \gamma$  with  $\gamma \in N(0; 5)$



# Automatic Transmission

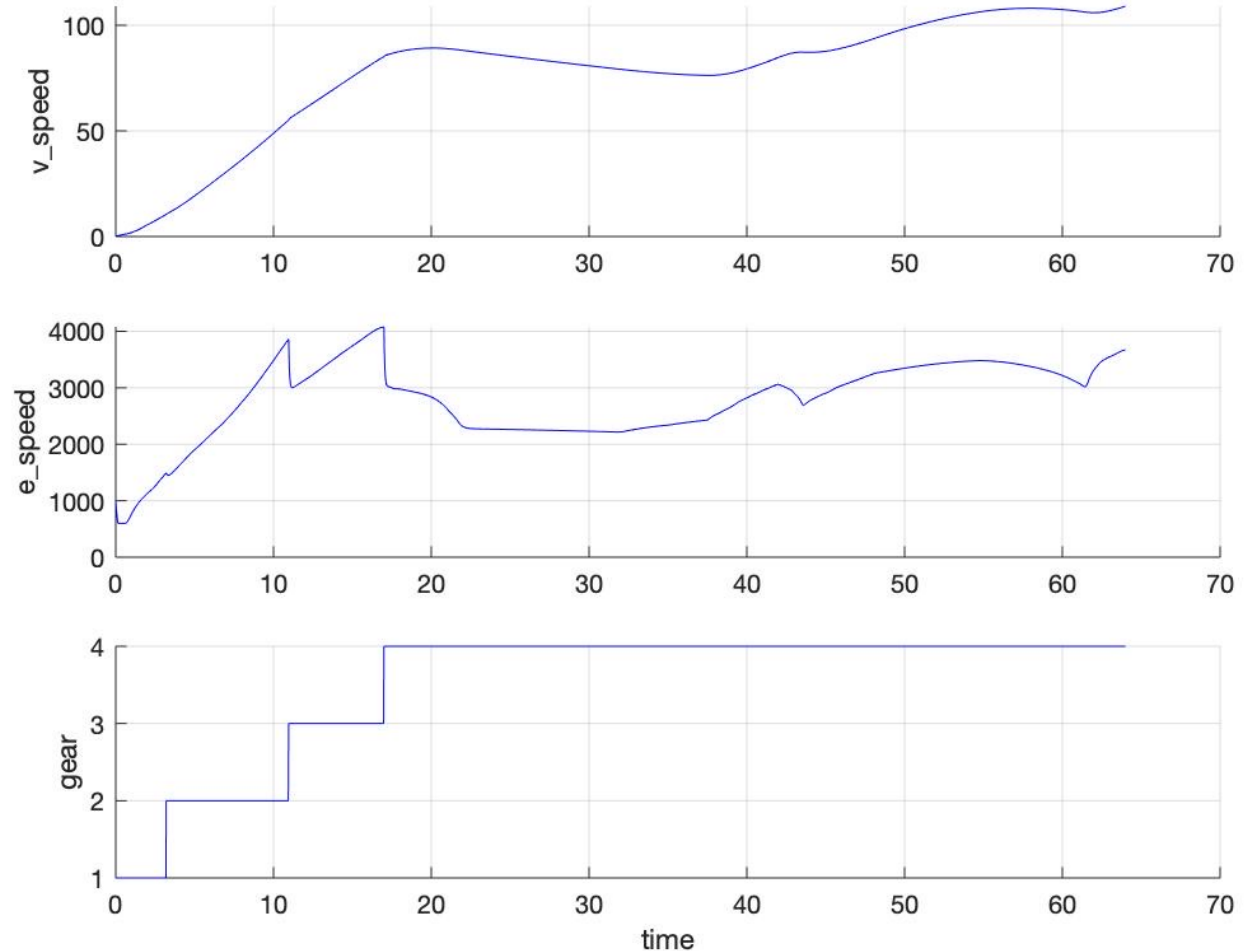


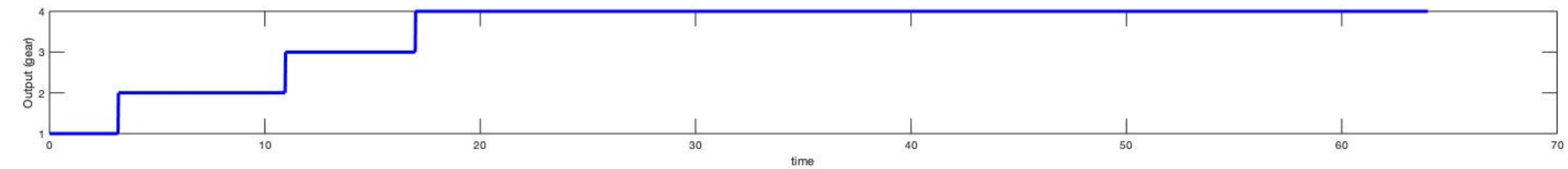
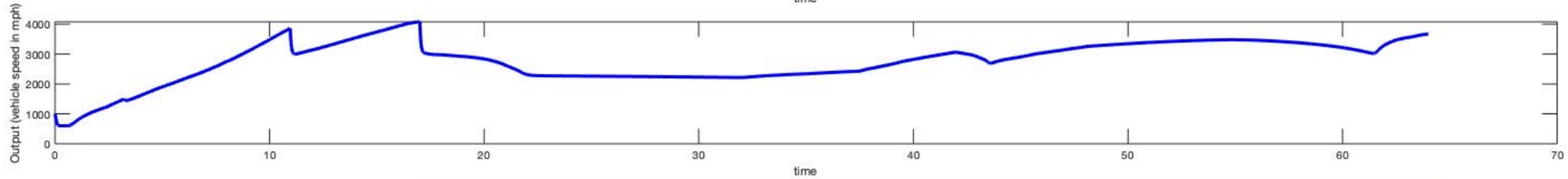
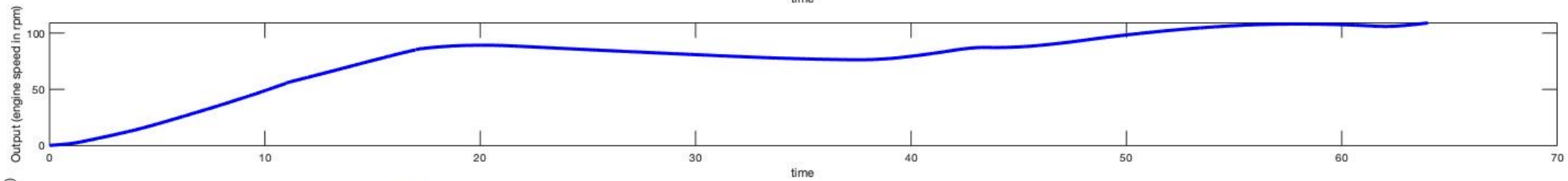
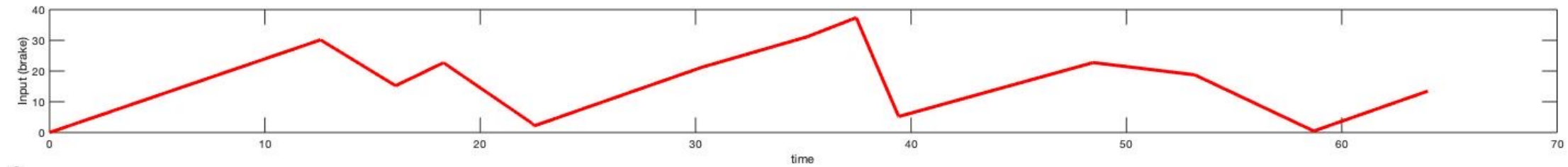
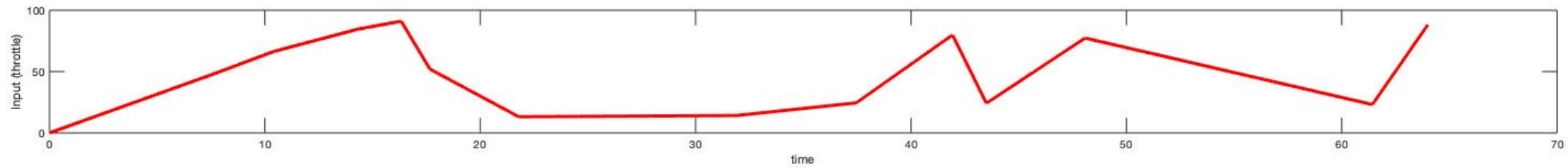
Most material that follows is from this paper:

- ▶ Bardh Hoxha, Houssam Abbas, Georgios E. Fainekos: Benchmarks for Temporal Logic Requirements for Automotive Systems. ARCH@CPSWeek 2014: 25-30

# Automatic Transmission

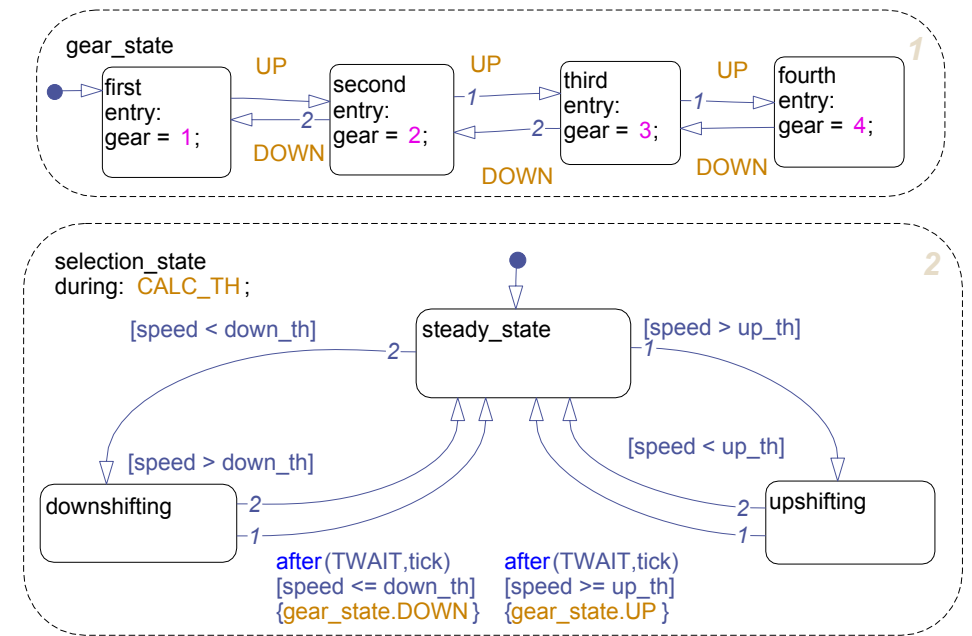
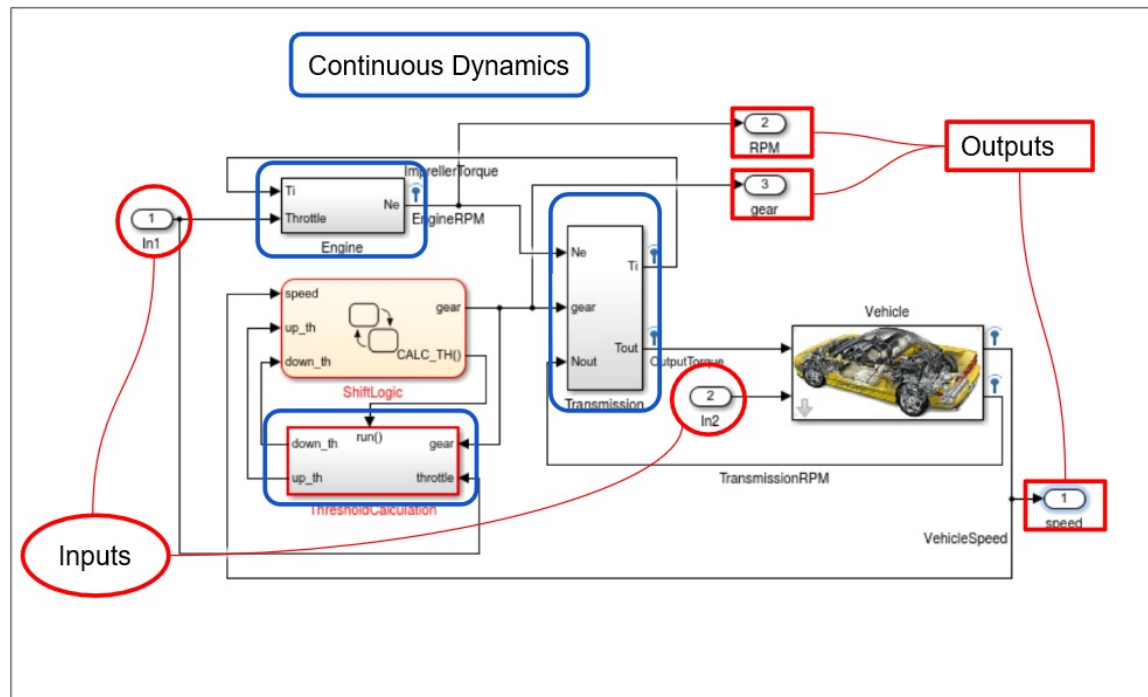
- ▶ Inputs: the throttle and break
- ▶ Outputs: the speed of the engine  $\omega$  (RPM), the speed of the vehicle  $v$  (mph) and the gear.
- ▶ Initially, the vehicle is at rest at time 0, i.e. the speed  $v = 0$  and engine speed  $\omega = 0$
- ▶ Therefore, the output trajectories depend only on the input signals  $u_t$  and  $u_b$  which model the throttle and break inputs.
- ▶ The throttle and break, at each point in time, can take any value between 0 (fully closed) to 100 (fully open).





# Automatic Transmission

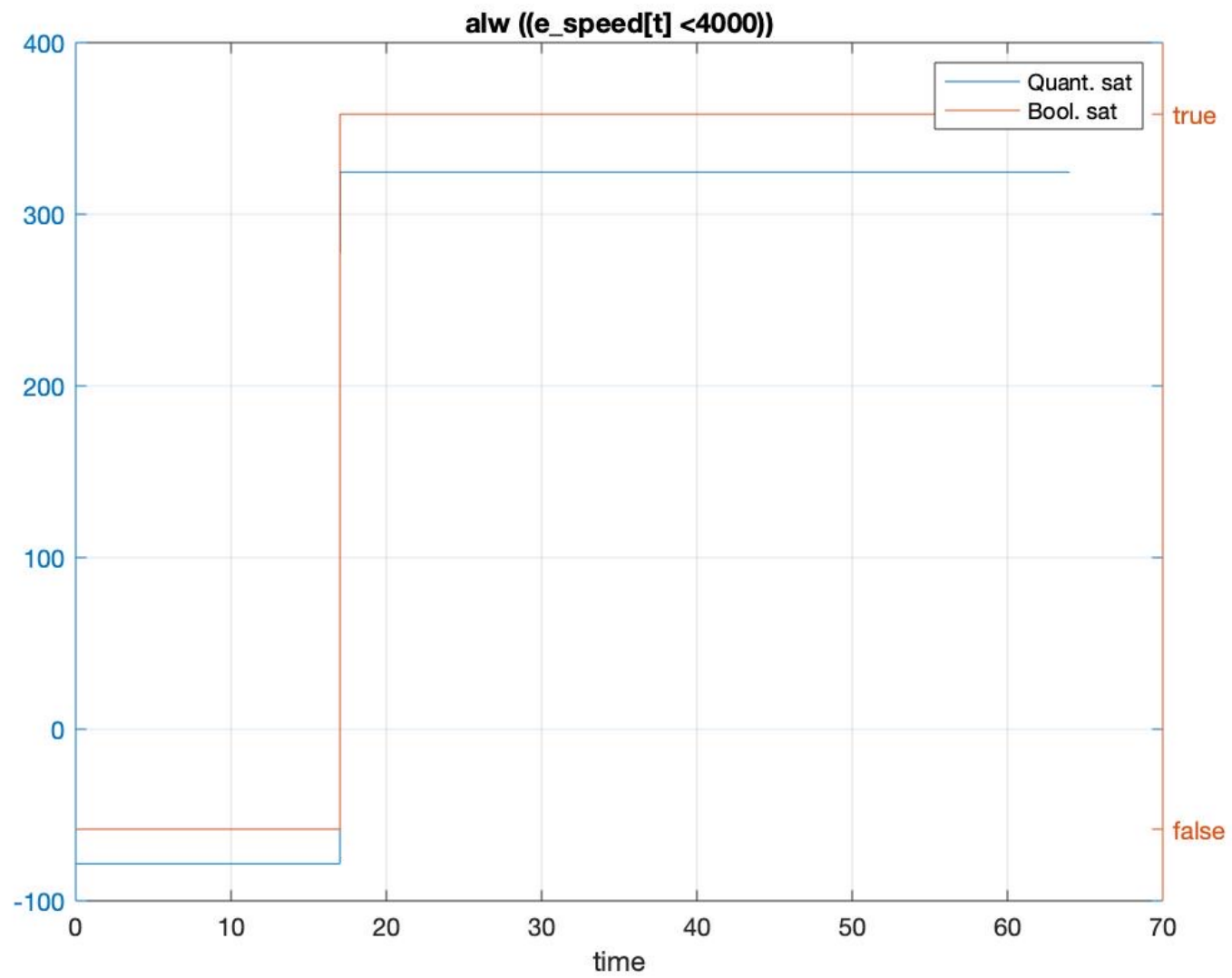
- ▶ The model contains 69 blocks among which there are 2 integrators (i.e., 2 continuous state variables), and a Stateflow chart. The Stateflow chart contains two concurrently executing Finite State Machines with 4 and 3 states, respectively.



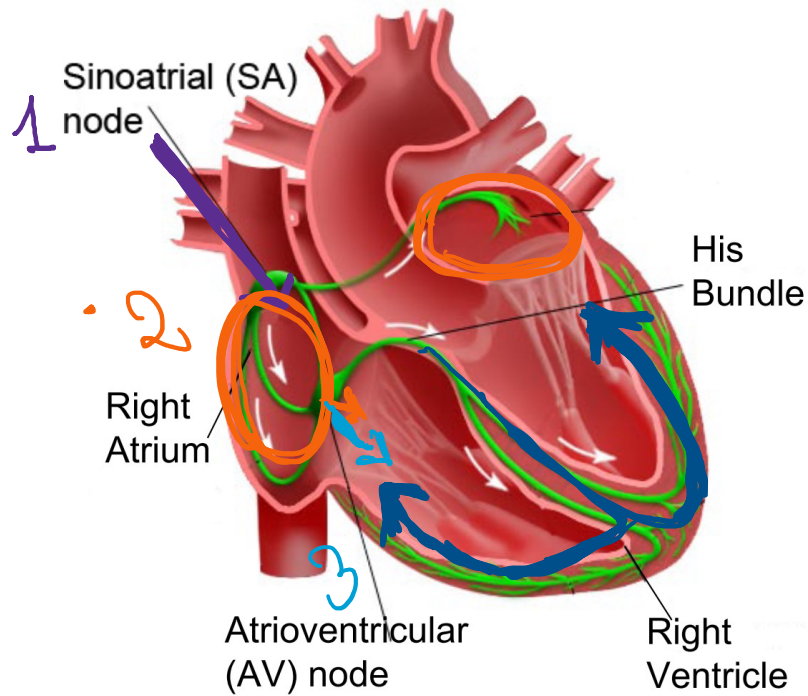
# Properties

Automatic Transmission		
	Natural Language	MTL
$\phi_1^{AT}$	The engine speed never reaches $\bar{\omega}$ .	$\Box(\omega < \bar{\omega})$
$\phi_2^{AT}$	The engine and the vehicle speed never reach $\bar{\omega}$ and $\bar{v}$ , resp.	$\Box((\omega < \bar{\omega}) \wedge (v < \bar{v}))$
$\phi_3^{AT}$	There should be no transition from gear two to gear one and back to gear two in less than 2.5 sec.	$\Box((g_2 \wedge Xg_1) \rightarrow \Box_{(0,2.5]}\neg g_2)$
$\phi_4^{AT}$	After shifting into gear one, there should be no shift from gear one to any other gear within 2.5 sec.	$\Box((\neg g_1 \wedge Xg_1) \rightarrow \Box_{(0,2.5]}g_1)$
$\phi_5^{AT}$	When shifting into any gear, there should be no shift from that gear to any other gear within 2.5sec.	$\bigwedge_{i=1}^4 \Box((\neg g_i \wedge Xg_i) \rightarrow \Box_{(0,2.5]}g_i)$
$\phi_6^{AT}$	If engine speed is always less than $\bar{\omega}$ , then vehicle speed can not exceed $\bar{v}$ in less than $T$ sec.	$\neg(\Diamond_{[0,T]}(v > \bar{v}) \wedge \Box(\omega < \bar{\omega}))$
$\phi_7^{AT}$	Within $T$ sec the vehicle speed is above $\bar{v}$ and from that point on the engine speed is always less than $\bar{\omega}$ .	$\Diamond_{[0,T]}((v \geq \bar{v}) \wedge \Box(\omega < \bar{\omega}))$
$\phi_8^{AT}$	A gear increase from first to fourth in under 10secs, ending in an RPM above $\bar{\omega}$ within 2 seconds of that, should result in a vehicle speed above $\bar{v}$ .	$((g_1 \mathcal{U} g_2 \mathcal{U} g_3 \mathcal{U} g_4) \wedge \Diamond_{[0,10]}(g_4 \wedge \Diamond_{[0,2]}(\omega \geq \bar{\omega}))) \rightarrow \Diamond_{[0,10]}(g_4 \rightarrow X(g_4 \mathcal{U}_{[0,1]}(v \geq \bar{v})))$





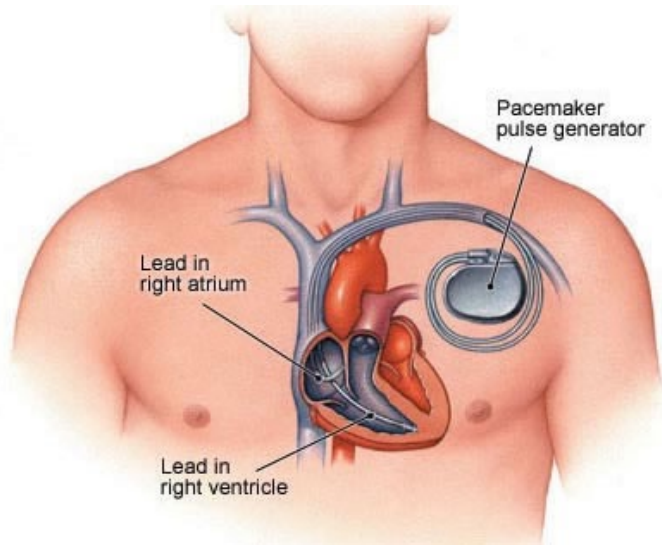
# Pacemaker



- 1 ▶ SA node (controlled by nervous system) periodically generates an electric pulse
- 2 ▶ This pulse causes both atria to contract pushing blood into the ventricles
- 3 ▶ Conduction is delayed at the AV node allowing ventricles to full fill
- 4 ▶ Finally the His-Purkinje system spreads electric activation through ventricles causing them both to contract, pumping blood out of the heart

**Electrical Conduction System of the Heart**

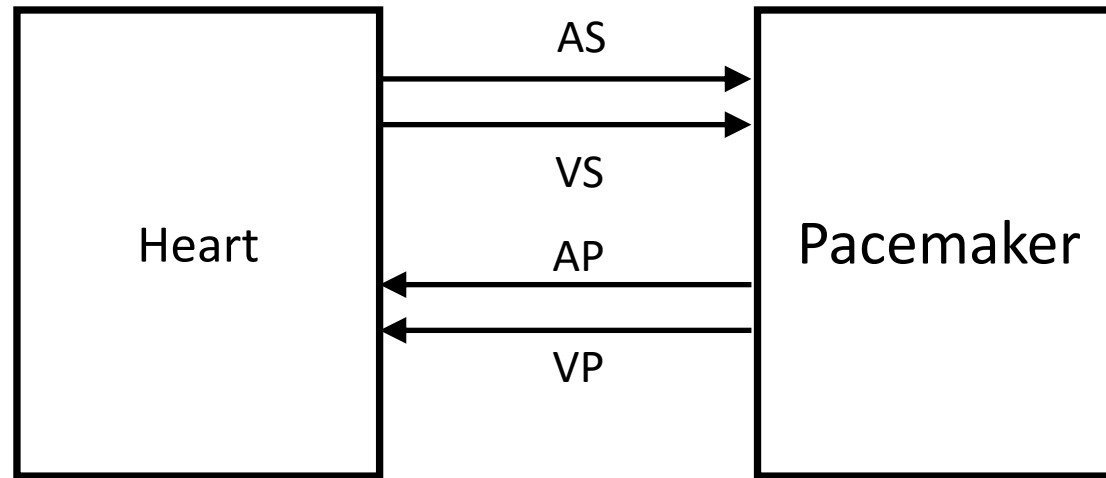
# What do pacemakers do?



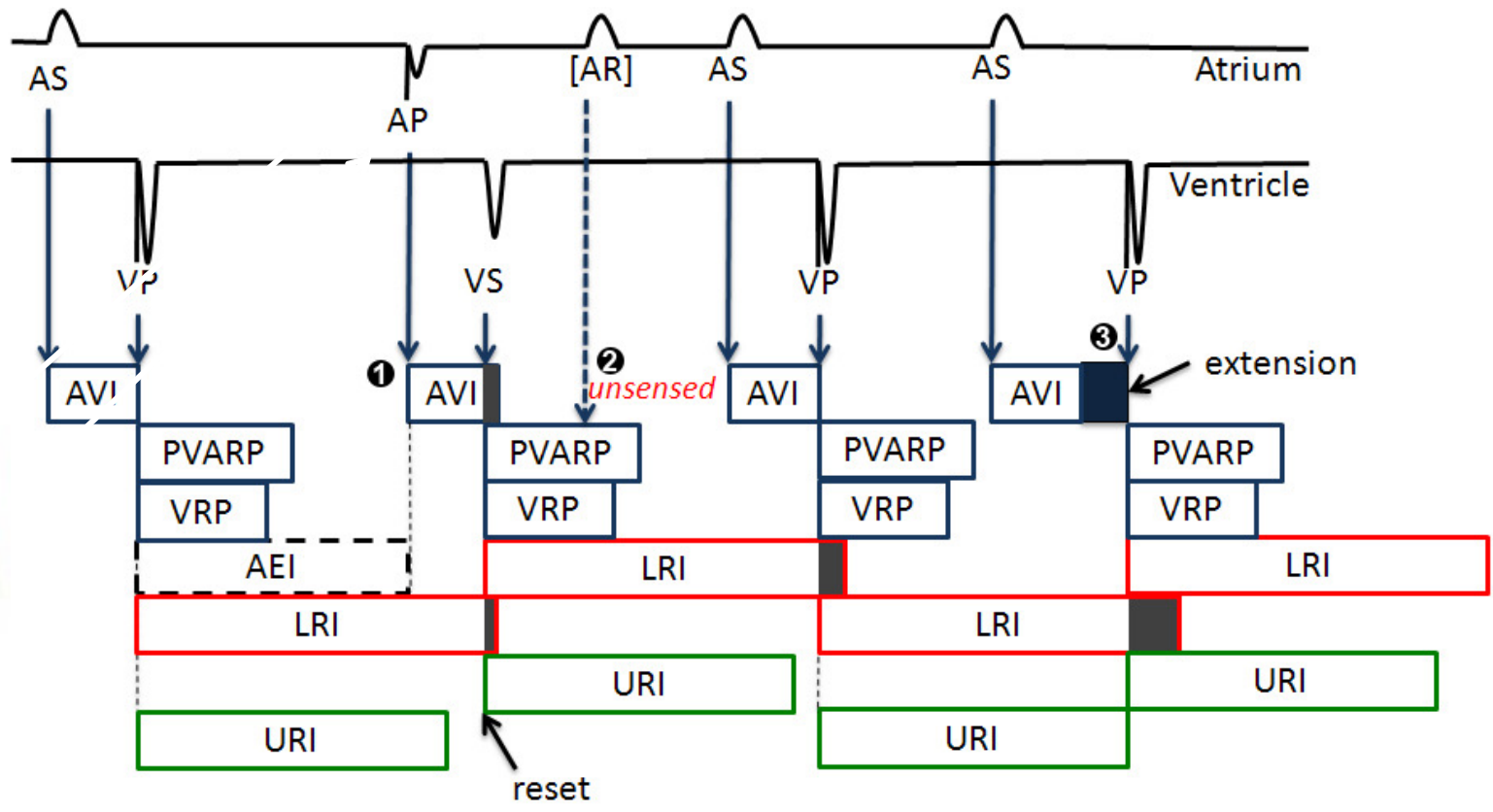
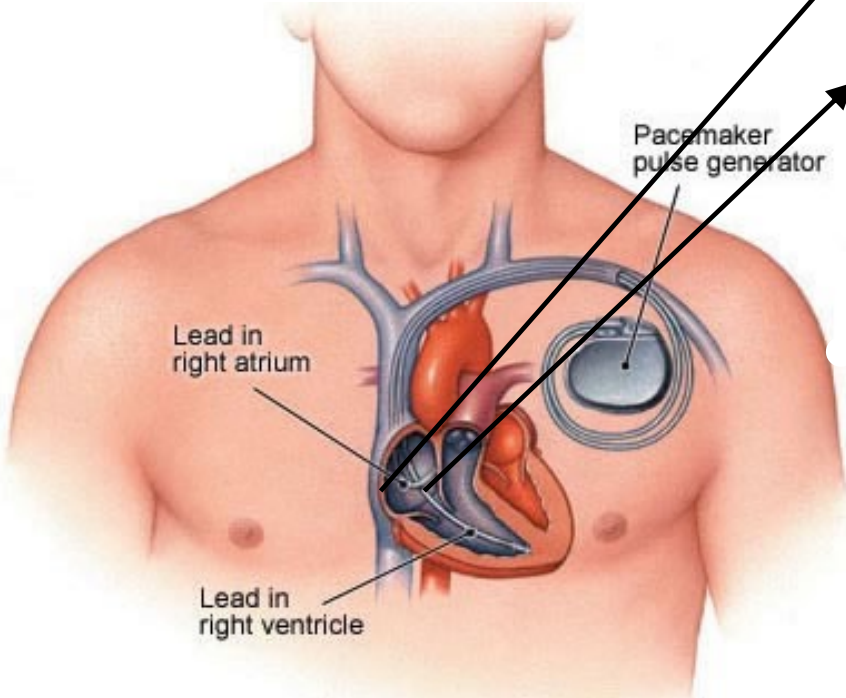
- ▶ Aging and/or diseases cause conduction properties of heart tissue to change leading to timing anomalies in heart rhythm (arrhythmias )
- ▶ Tachycardia: faster than desirable heart rate impairing hemo-dynamics (blood flow dynamics)
- ▶ Bradycardia: slower heart rate leading to insufficient blood supply
- ▶ Pacemakers can be used to treat bradycardia by providing pulses when heart rate is low

# How dual-chamber pacemakers work

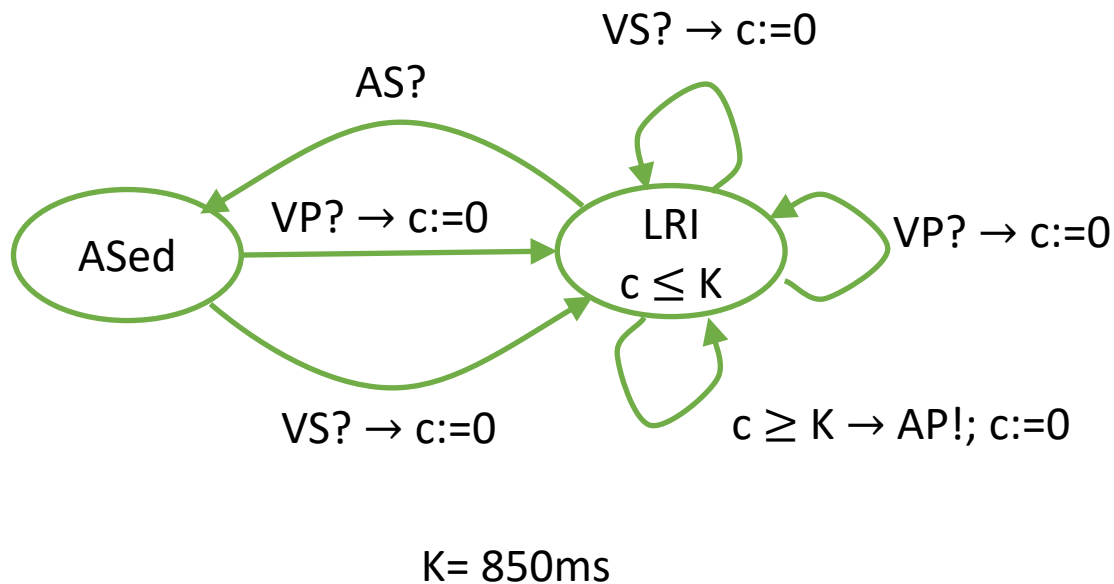
- ▶ Two fixed leads on wall of right atrium and ventricle respectively
- ▶ Activation of local tissue sensed by the leads (giving rise to events Atrial Sense (AS) and Ventricular Sense (VS))
- ▶ Atrial Pacing (AP) or Ventricular Pacing (VP) are delivered if no sensed events occur within deadlines



# Implantable Pacemaker modeling

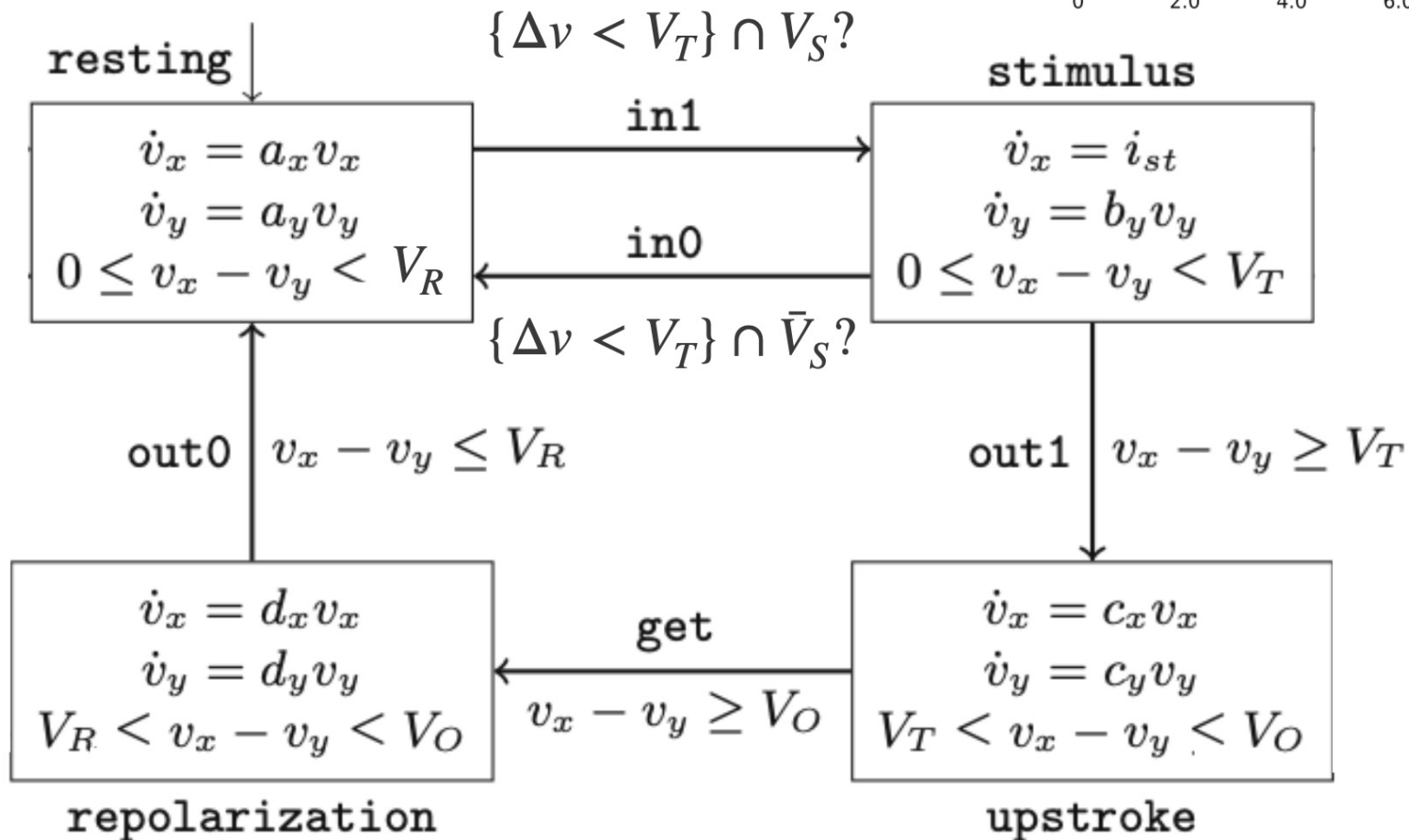
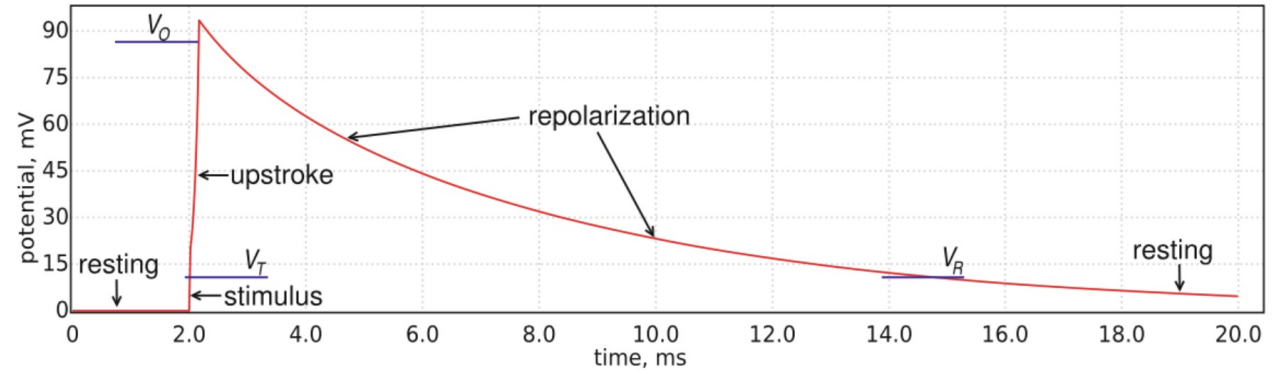


# The LRI mode of operation explained



- ▶ LRI (Low Rate Interval) component keeps heart rate above minimum level
- ▶ One of the pacemaker modes of operation that models the basic timing cycle
- ▶ Measures the longest interval between ventricular events
- ▶ Clock reset when VS or VP received
- ▶ No AS received  $\Rightarrow$  LRI outputs AP after K (TLRI-TAVI) time units

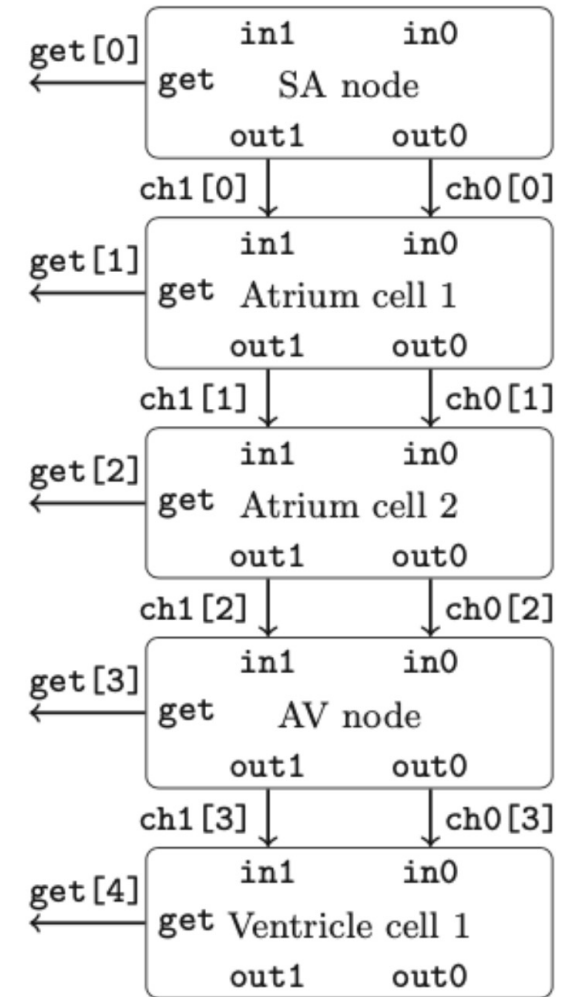
# Hodgkin - Huxley model



# Hodgkin - Huxley model

The whole heart model consists of a linear composition of cell models, which synchronize according to their output and input stimuli

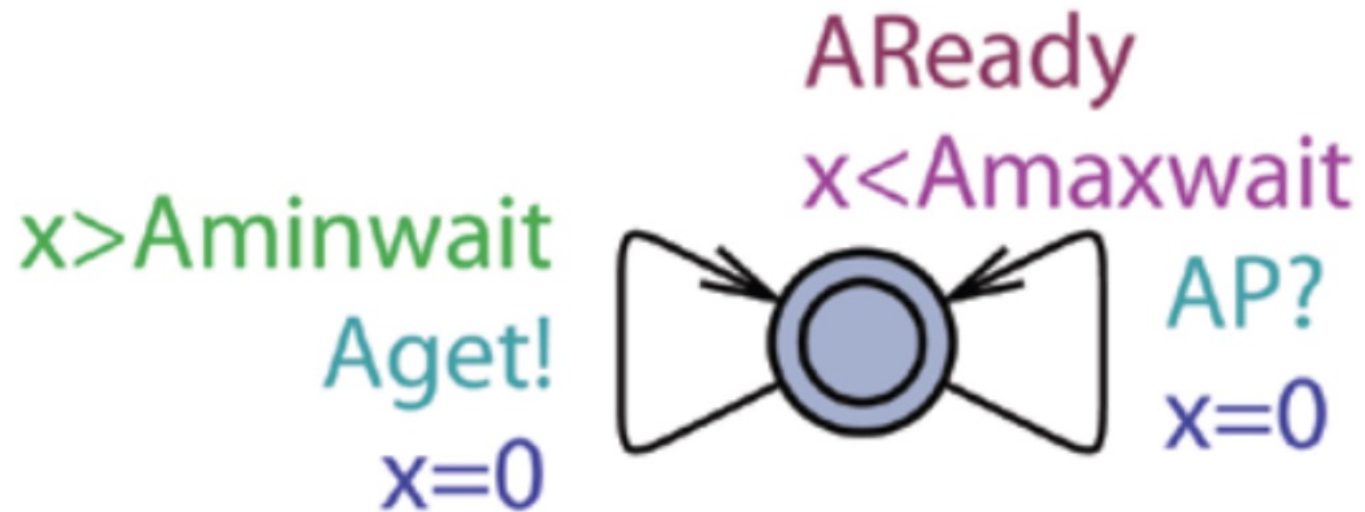
At the top of the network, we have the sinoatrial (SA) node: it's input stimulus can come from the natural pacing of the heart or from pacemaker's actuator.





# Random Heart Model (RHM)

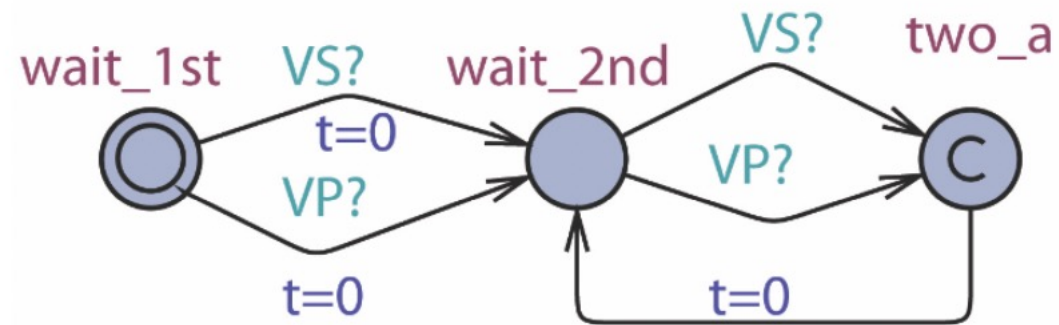
- ▶ RHM is designed to cover open-loop heart behaviors For the atrial region for instance, the interval between each action (*Aget!*) is a random value from the interval (*Aminwait*, *Amaxwait*).



# Property

TCTL formula :  $A \Box ((VS! V VP!) \rightarrow A \Box_{\leq TLRI} (VS! V VP!))$

The interval between two ventricular events should be less than TLRI



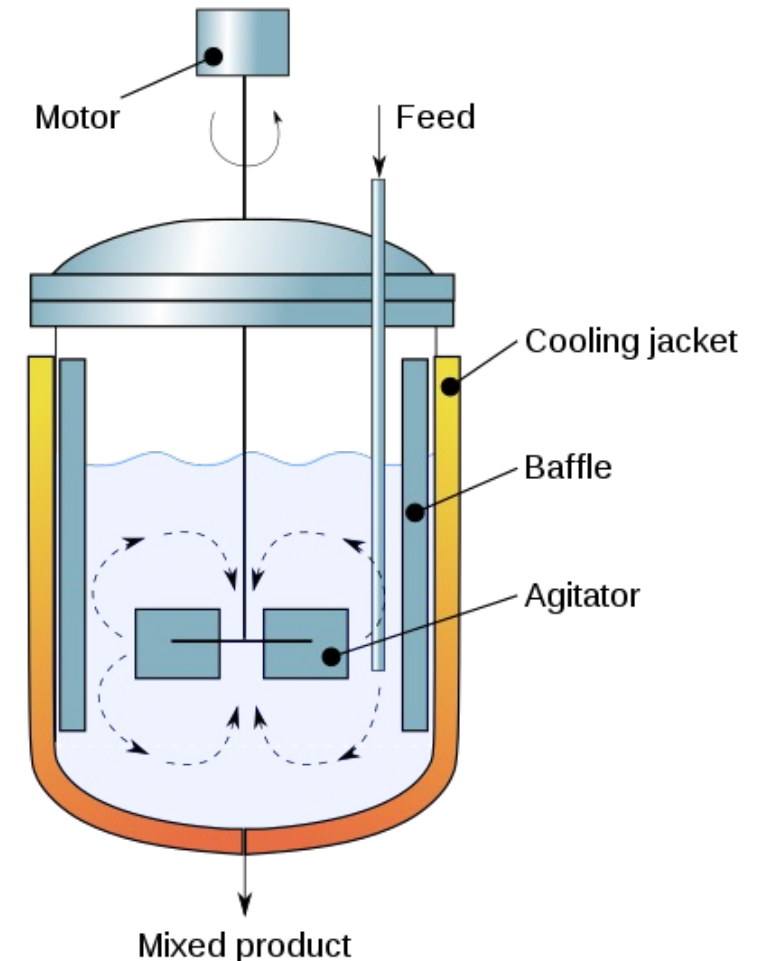
# Property

TCTL formula :  $A \square ( \text{ch1}[0] ! \rightarrow A \diamond \text{ch1}[N] ! )$

Given an initial input, the signal should propagate all the way from SA node to atrium and then ventricle, and eventually be visible at the end of the N cells chain described in the previous section.

# Temperature Control of a Continuous Stirred Tank Reactor

- Control (PID and MPC) the temperature of an exothermic CSTR so that it follows a constant set point;
- Requirement specification and checking using STL;
- Falsification of the requirements;



# Plant Model

First Order Reaction:  $A \rightarrow_{k \cdot C_A} B$

Reaction rate per unit volume (Arrhenius law):

$$k(T) = k_0 e^{-E_a/R \cdot T}$$

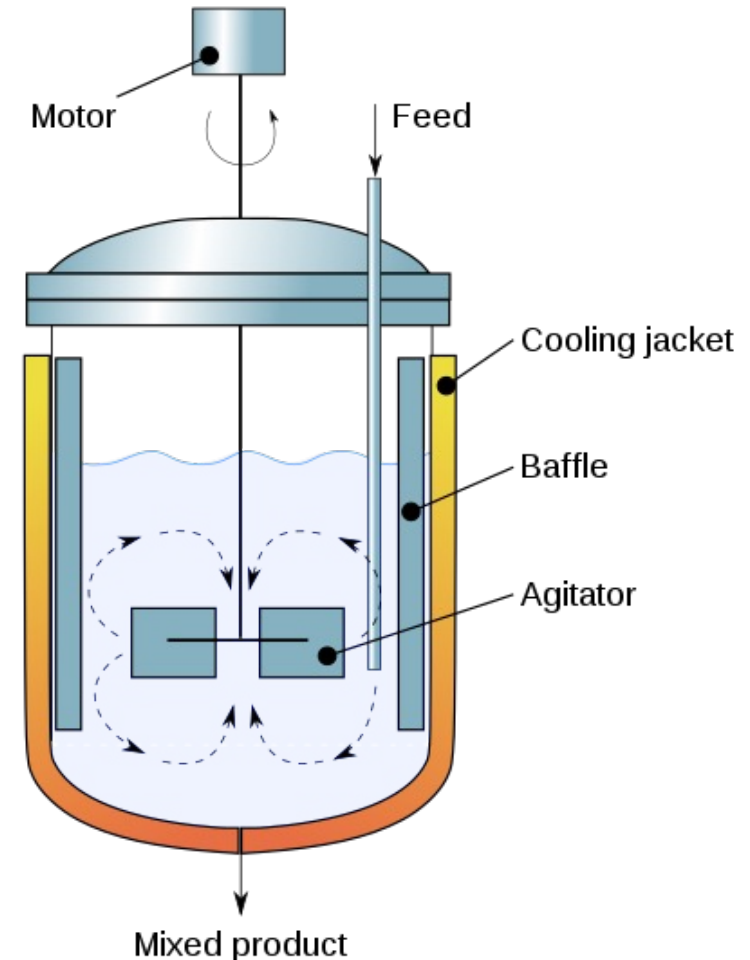
Mole balance equation:

$$\frac{dC_A}{dt} = \frac{q}{V} (C_{Af} - C_A) - k(T)C_A$$

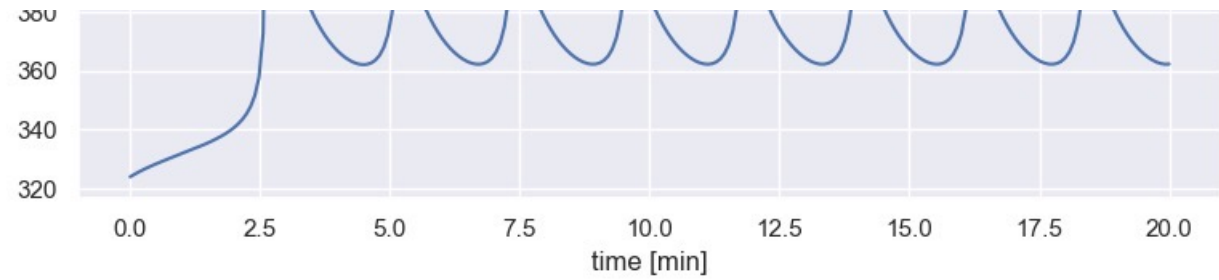
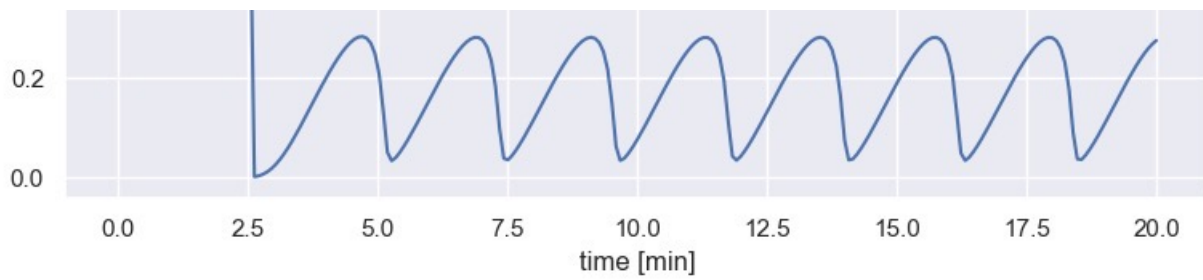
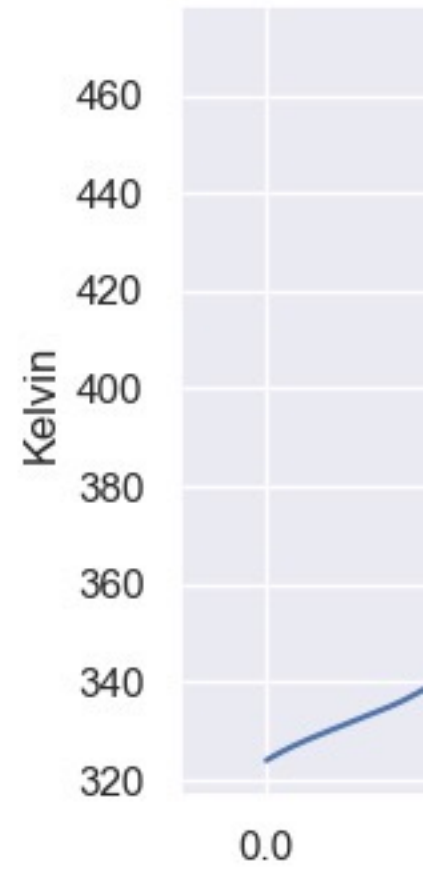
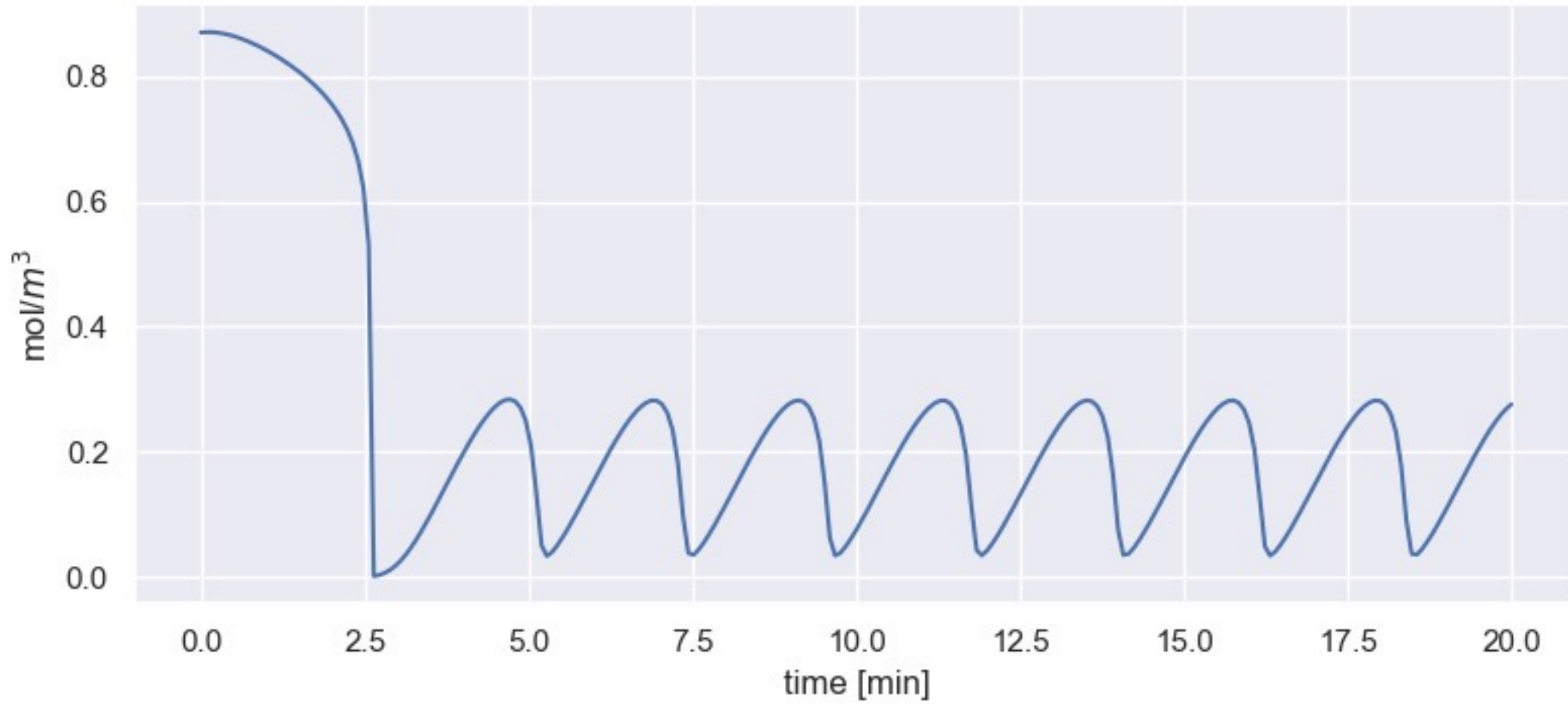
Energy balance equation:

$$\frac{dT}{dt} = \frac{q}{V} (T_f - T) + \frac{-\Delta H_R}{\rho C_p} k(T)C_A + \frac{UA}{\rho C_p V} (T - T_c)$$

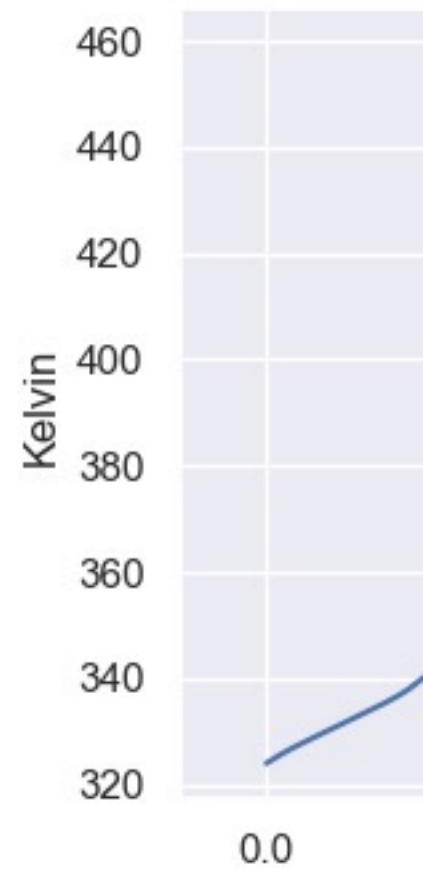
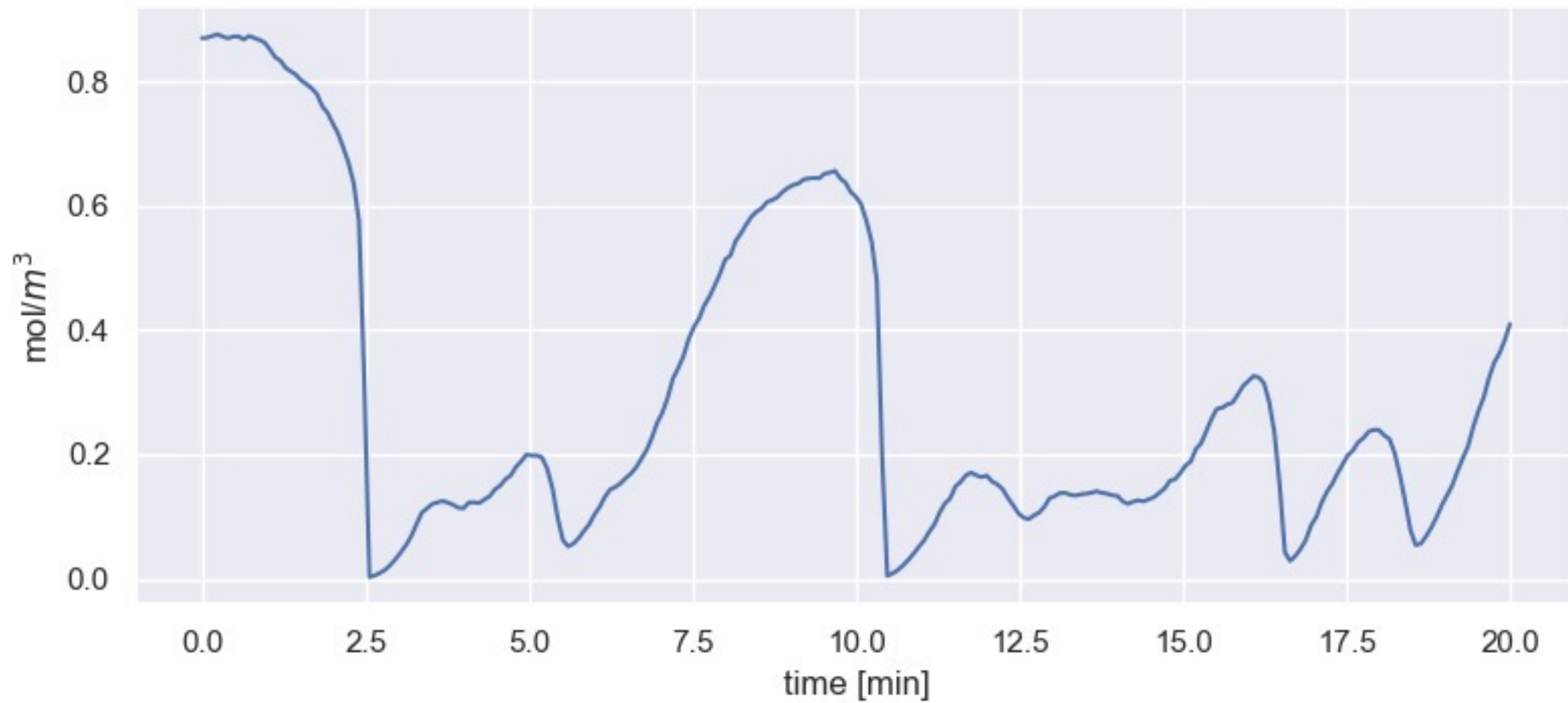
Input constraint:  $T_c \in [250, 350]$



Concentration



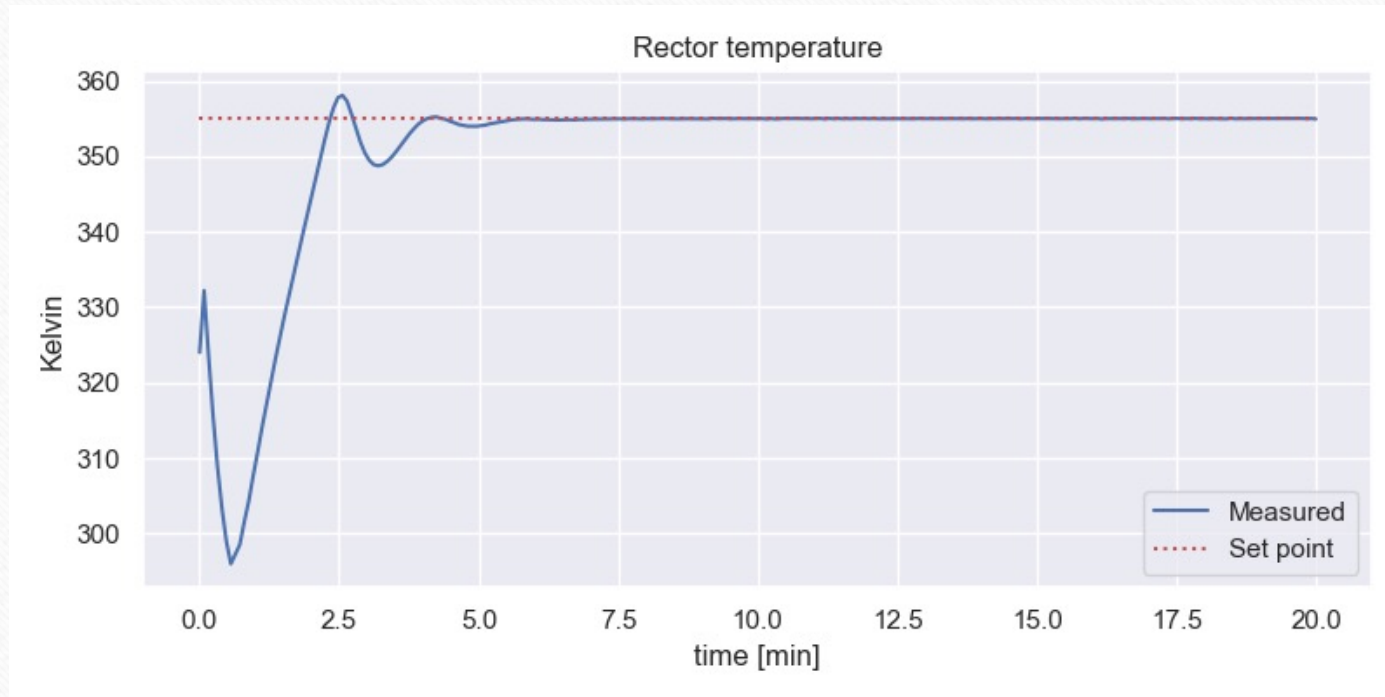
Concentration





# PID Control Cont'd

Performance of PID controller when tracking a temperature of 355K



PID parameters:

$$K_p = 1.7$$

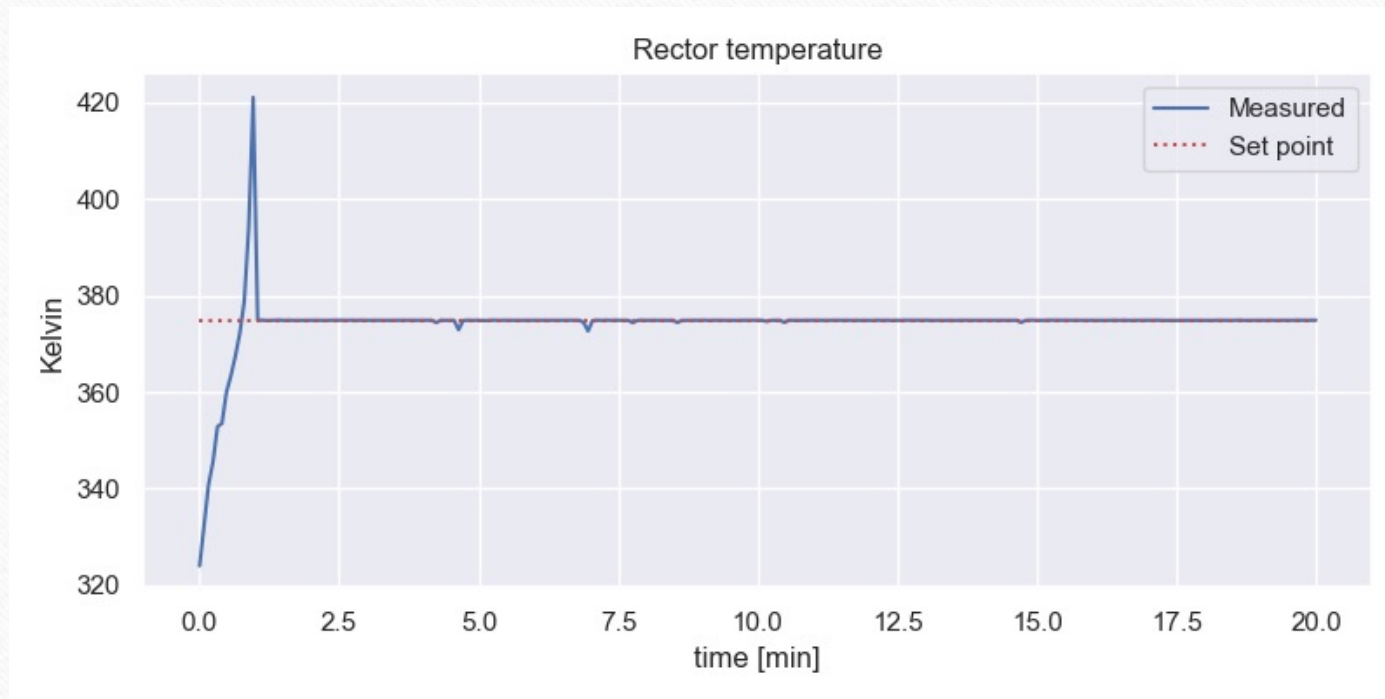
$$\tau_i = 0.8$$

$$\tau_d = 0.2$$



# Non-linear MPC Cont'd

Performance of MPC when tracking a temperature of 375K



MPC parameters:

$$Q = 2.0$$

$$R = 0.01$$

$$H = 10.0$$

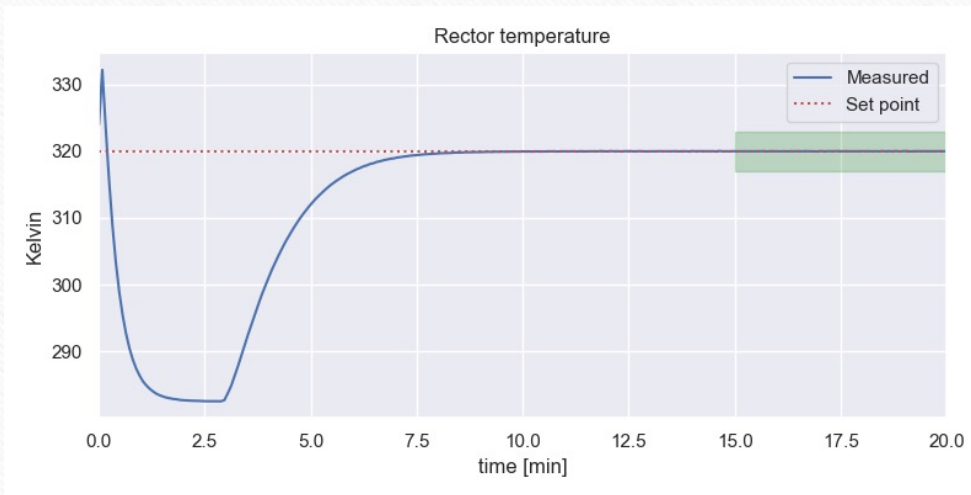
# STL Requirements 3

Goal: CSTR should closely follow reference temperature

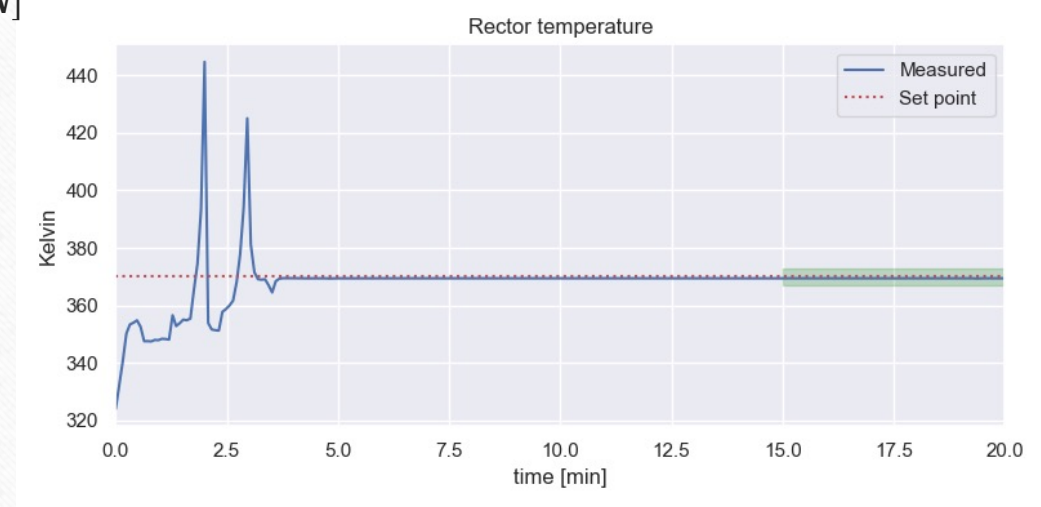
Difference from reference:  $d(t) = |T(t) - ref(t)| \forall t$

1. In the last part of the simulation, difference from reference should not exceed  $3K$

$$\phi_3 = G_{[\frac{2N}{3}, N]}(d(t) < 3.0)$$



PID

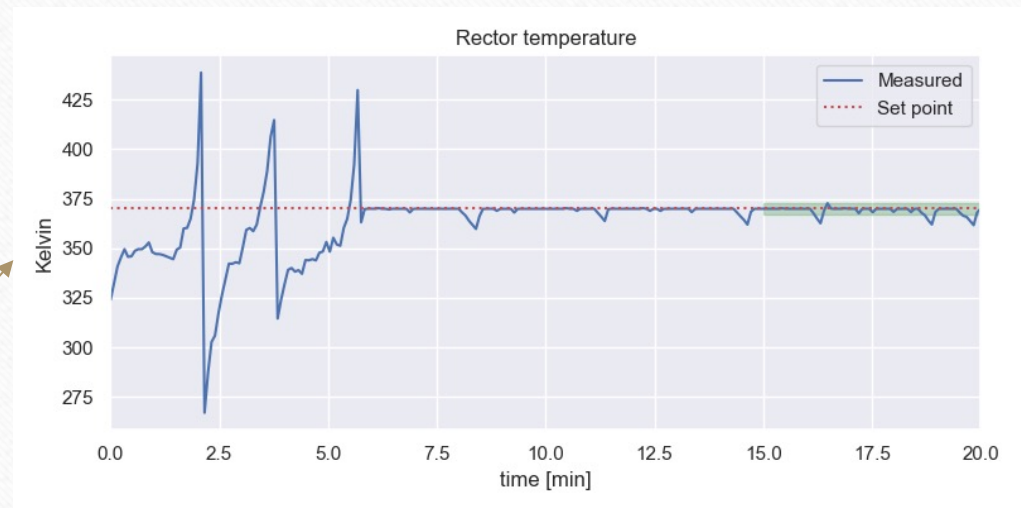


MPC

# Falsification Cont'd

MPC parameters found in falsification analysis

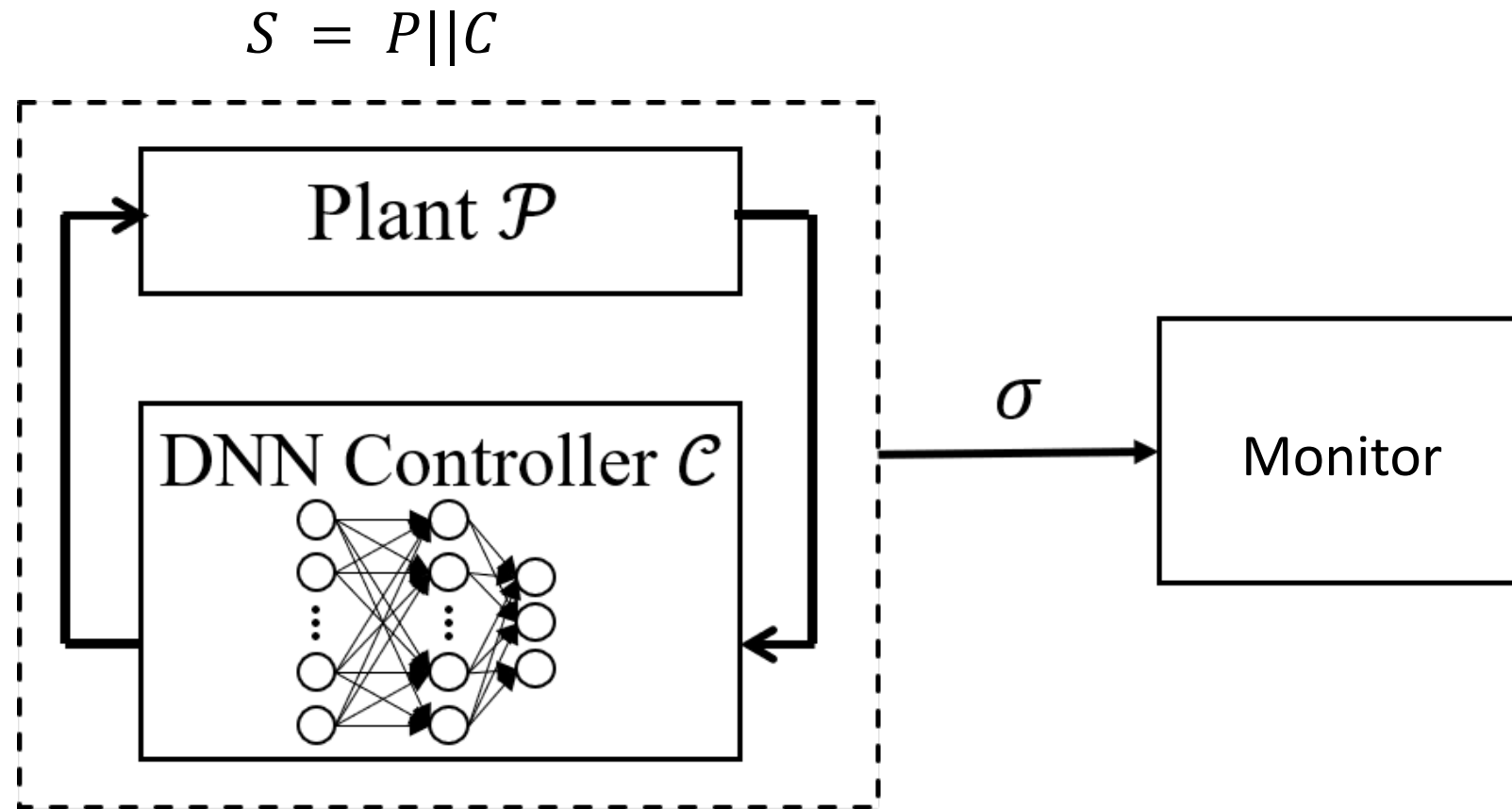
Reference	Q	R	Robustness
320	1.33663	0.020416	-1.28741
325	0.376885	0.024445	-20.7467
330	0.210134	0.0191757	-31.3692
335	1.60591	0.0040131	-0.423672
340	1.63118	0.00144311	-0.0405561
345	2.45878	0.0092065	-0.10704
350	2.67307	0.0045229	-2.28309
355	1.57202	0.00161315	-3.23189
360	1.67468	0.0150942	-8.42903
365	2.70502	0.00979266	-58.8853
370	2.59014	0.00121103	-5.30934
375	1.73716	0.0150608	-0.0113018
380	1.48972	0.018182	-2.94381
385	0.226472	0.0107259	-8.14433



Falsification for reference temperature 370K



# A Deep Neural Network controller



# Bibliography

**Nice survey on Specification-Based Monitoring of CPSs:** <http://www-verimag.imag.fr/PEOPLE/maler/Papers/monitor-RV-chapter.pdf>

## **Artificial Pancreas:**

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- ▶ Simone Silvetti, Laura Nenzi, Ezio Bartocci, Luca Bortolussi: Signal Convolution Logic. CoRR abs/1806.00238 (2018)
- ▶ Fraser Cameron, Georgios E. Fainekos, David M. Maahs, Sriram Sankaranarayanan: Towards a Verified Artificial Pancreas: Challenges and Solutions for Runtime Verification. RV 2015: 3-17
- ▶ Sriram Sankaranarayanan, Suhas Akshar Kumar, Faye Cameron, B. Wayne Bequette, Georgios E. Fainekos, David M. Maahs: Model-based falsification of an artificial pancreas control system. SIGBED Rev. 14(2): 24-33 (2017)

## **Pacemaker:**

- ▶ Z. Jiang, M. Pajic, S. Moarref, R. Alur, R. Mangharam, *Modeling and Verification of a Dual Chamber Implantable Pacemaker*, In Proceedings of Tools and Algorithms for the Construction and Analysis of Systems (TACAS), 2012.
- ▶ The textbook has detailed descriptions of some other pacemaker components